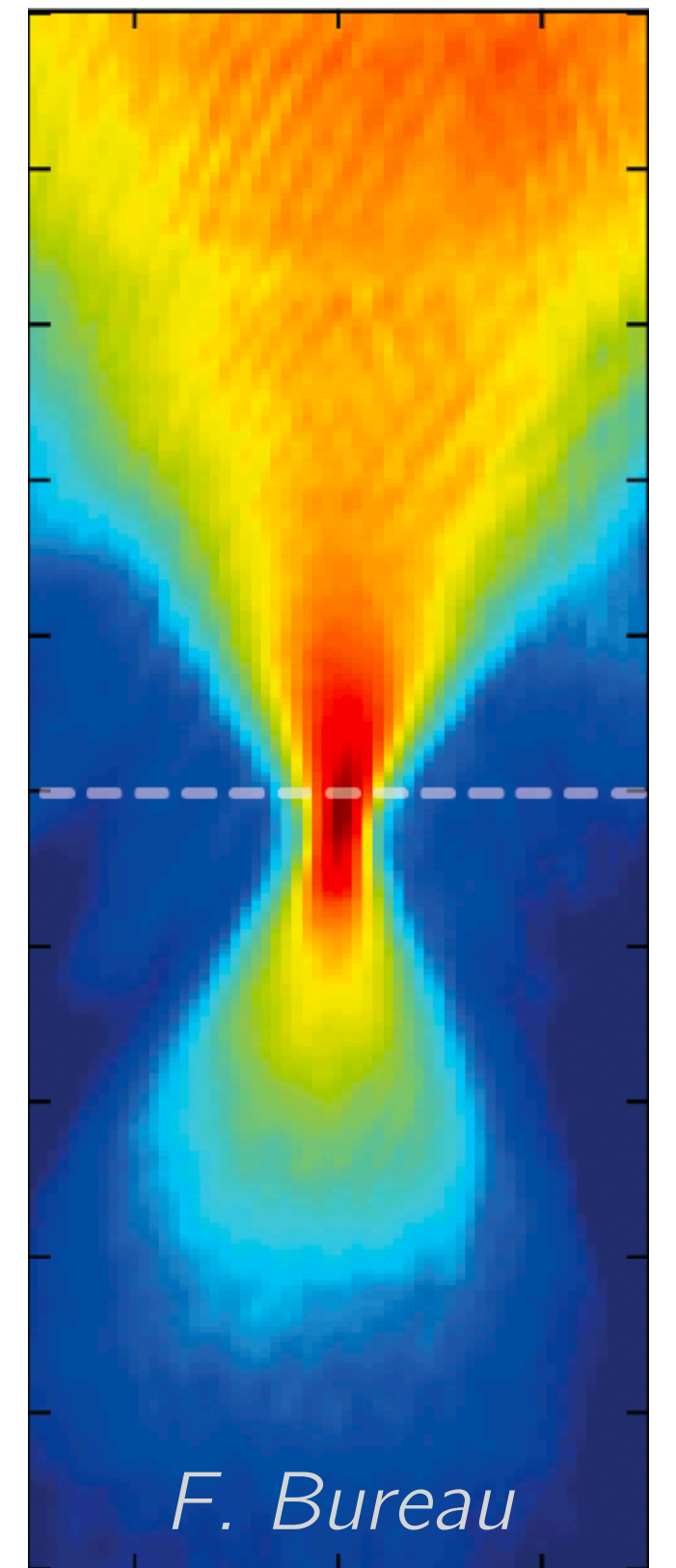
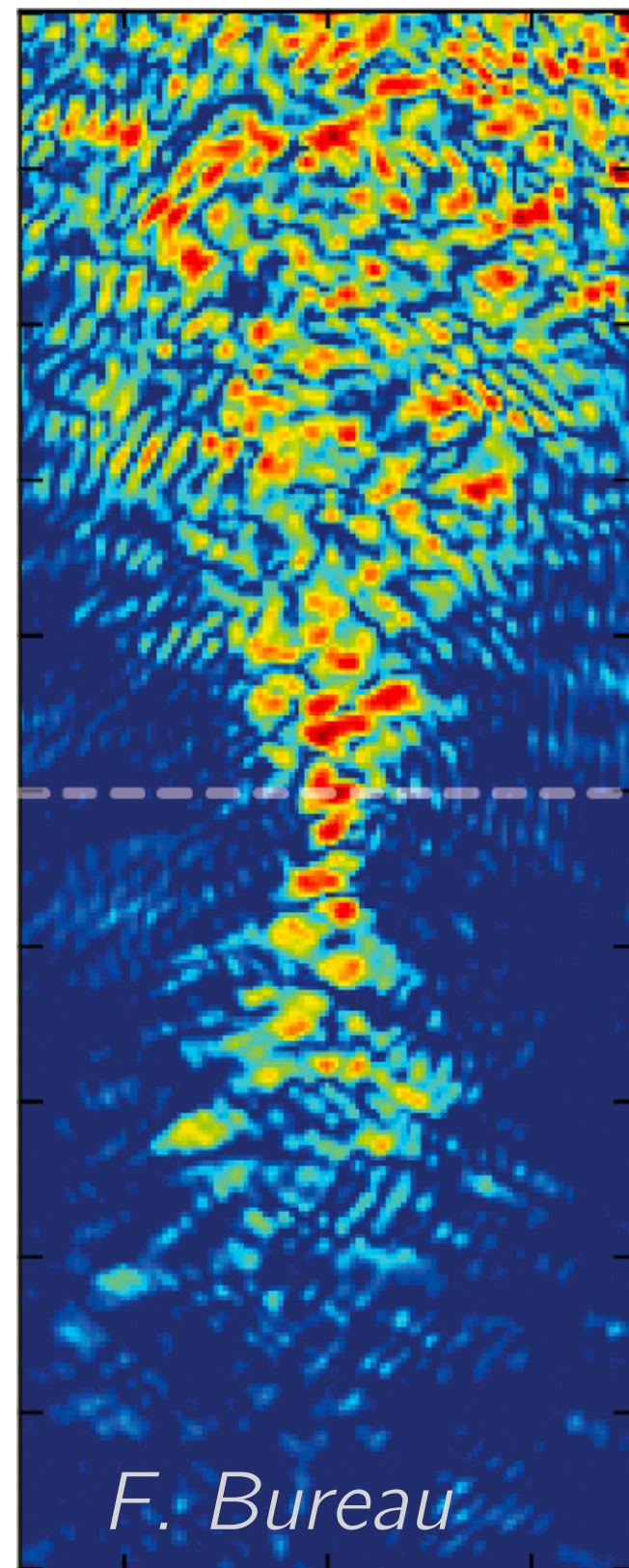


Self-Imaging Waves

Probing the speckle to estimate the effective speed of sound, a first step towards quantitative ultrasound imaging

Joint work w/ J. Garnier, L. Giovangigli, Q. Goepfert, E. Parolin



Institut **Langevin**

ONDES ET IMAGES ESPCI  PARIS | PSL 

Adaptative optics in 1 min

Theoretical model for a linear imaging system



Theoretical Point Spread Function (PSF)

Adaptative optics in 1 min

Theoretical model for a linear imaging system



Theoretical Point Spread Function (PSF)

Practical situation with point-like object in field of view

Fitting of the PSF

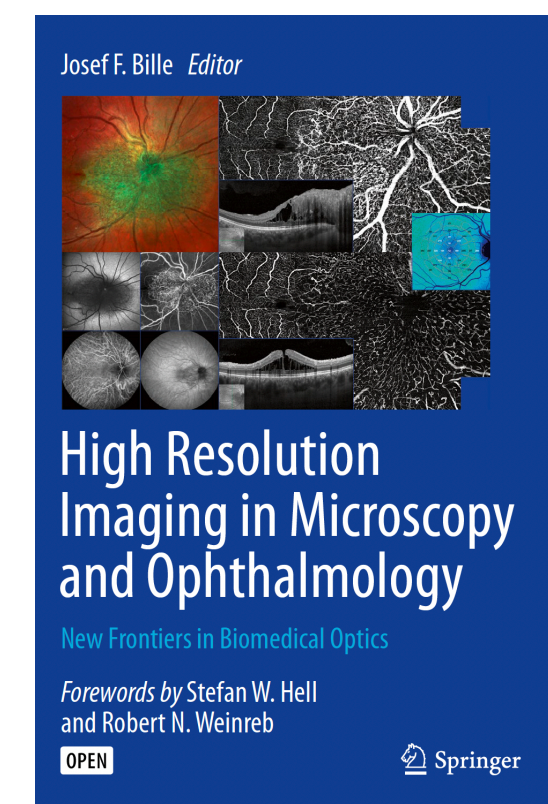
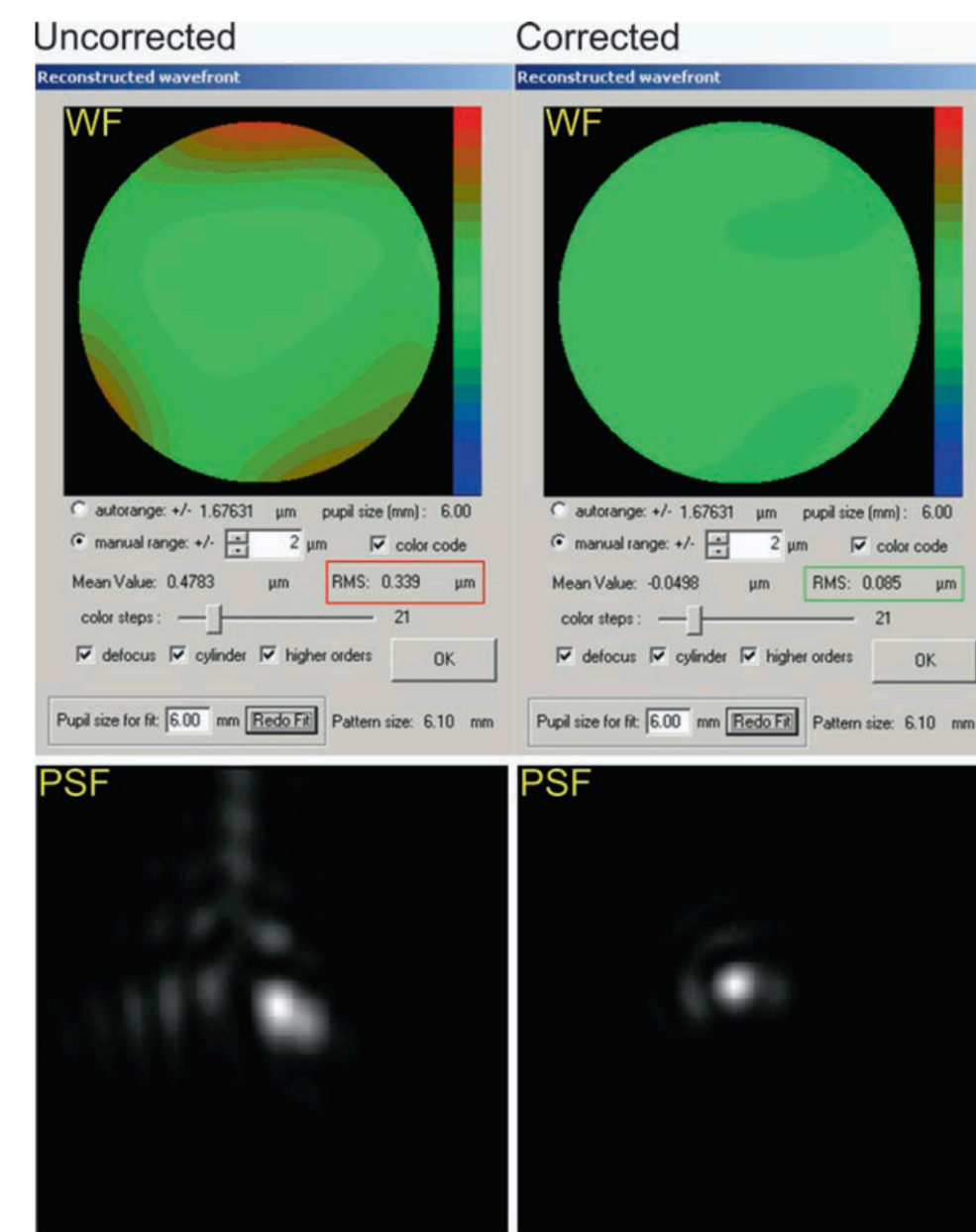
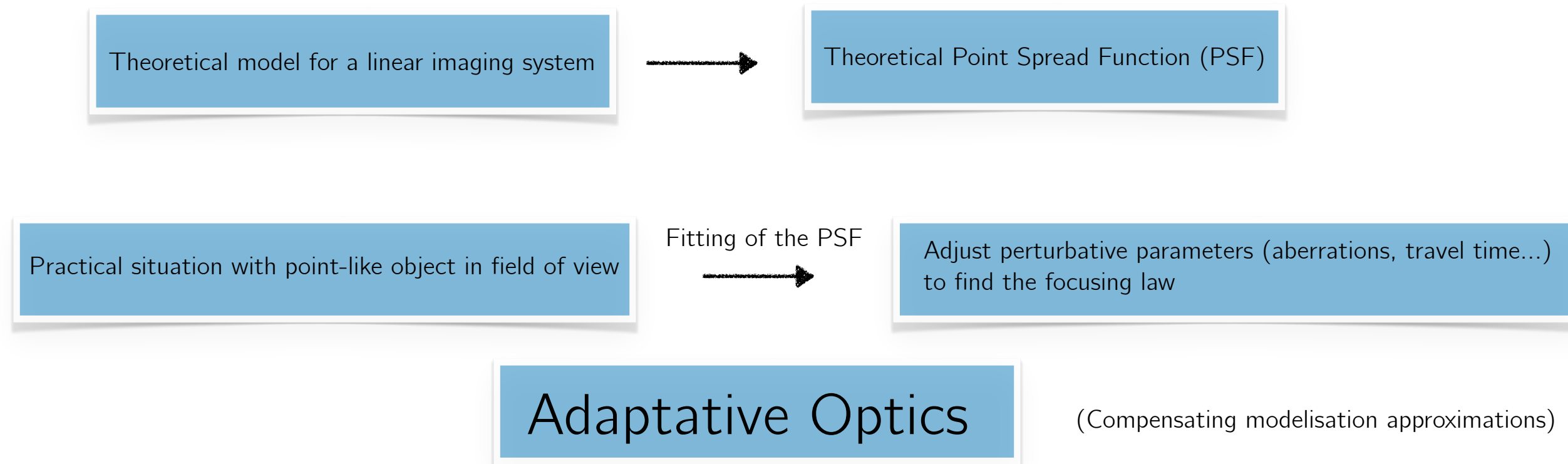


Adjust perturbative parameters (aberrations, travel time...) to find the focusing law

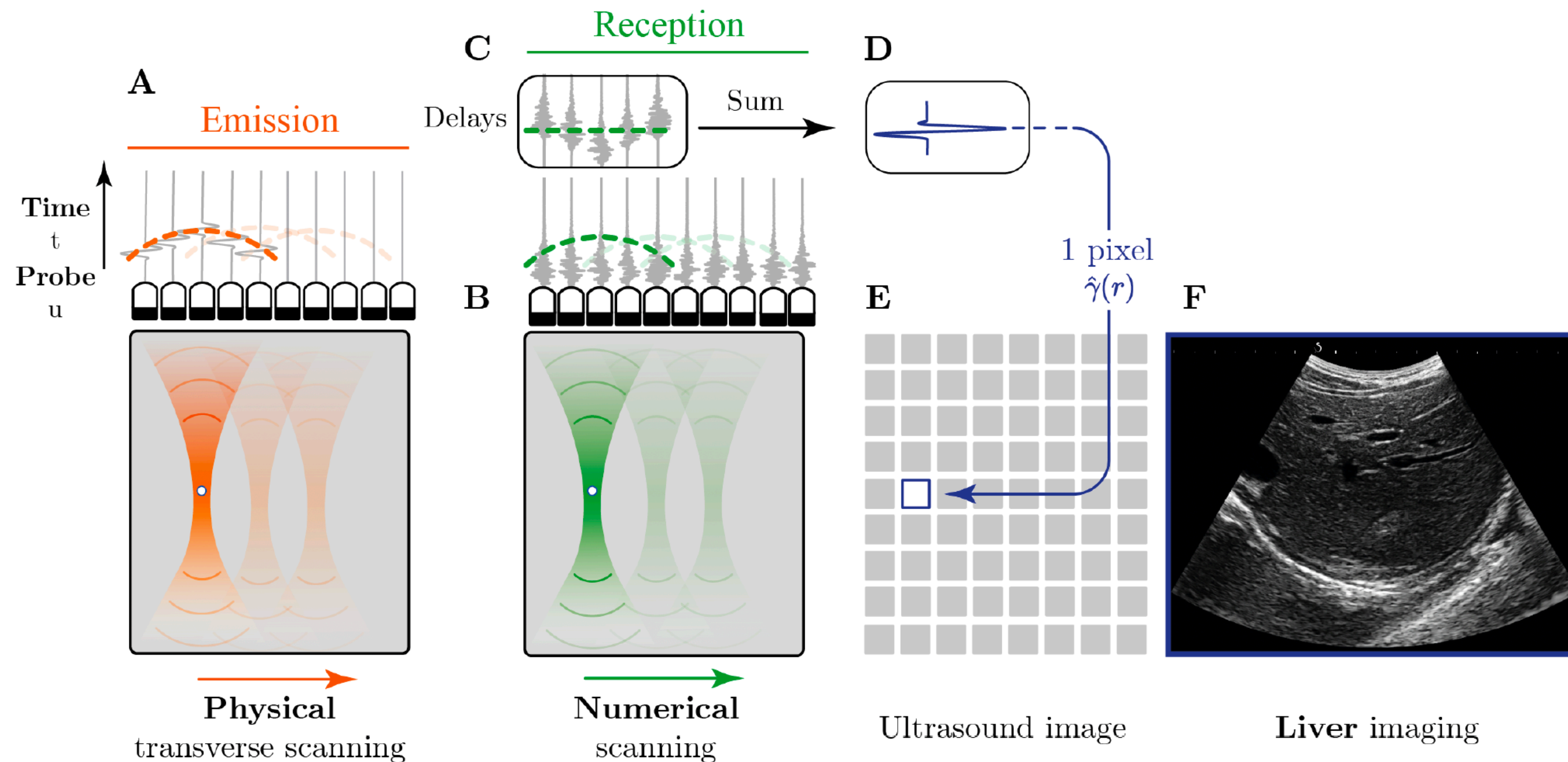
Adaptative Optics

(Compensating modelisation approximations)

Adaptative optics in 1 min

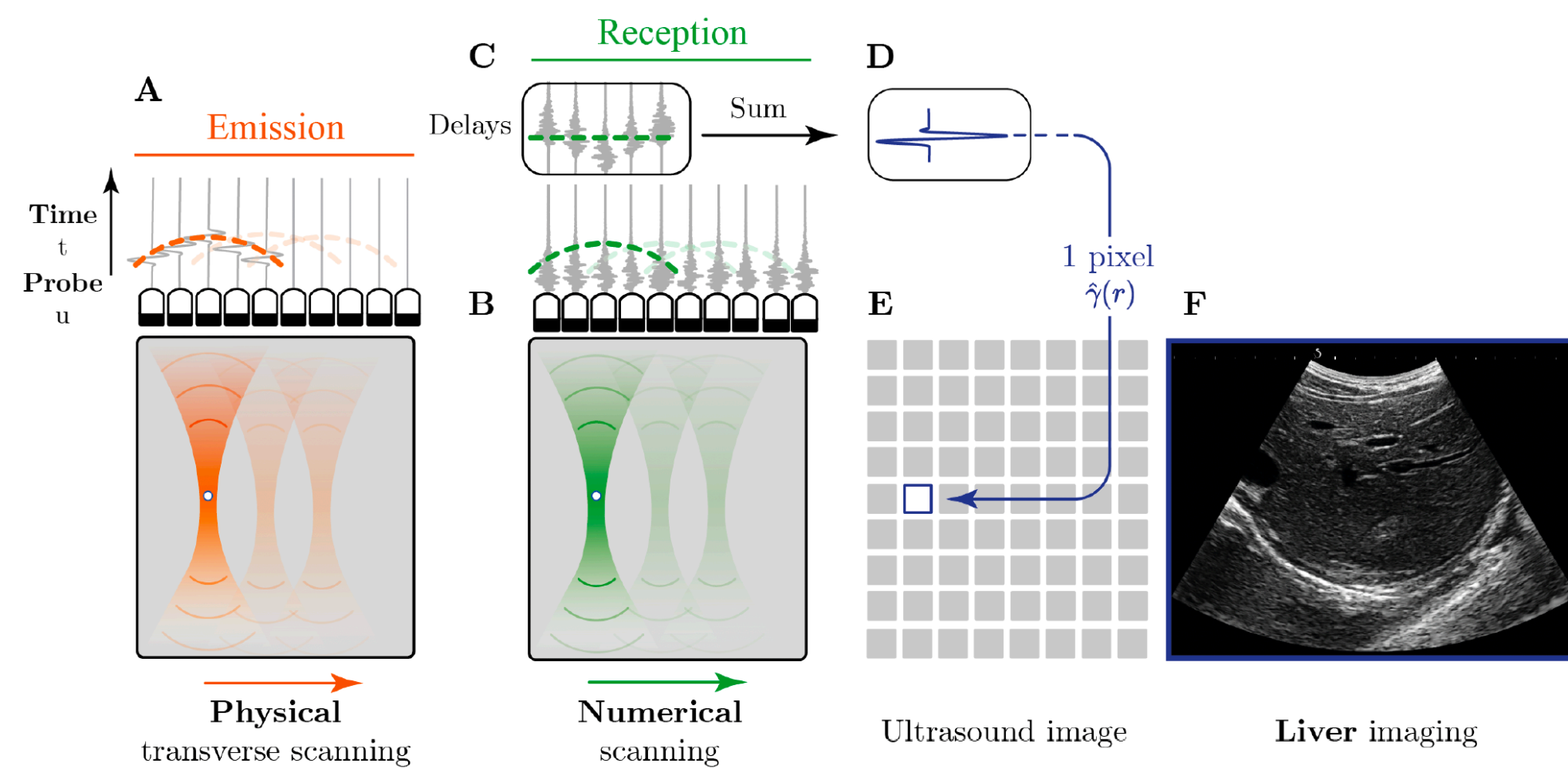


Principle of ultrasound imaging



Principle of ultrasound imaging

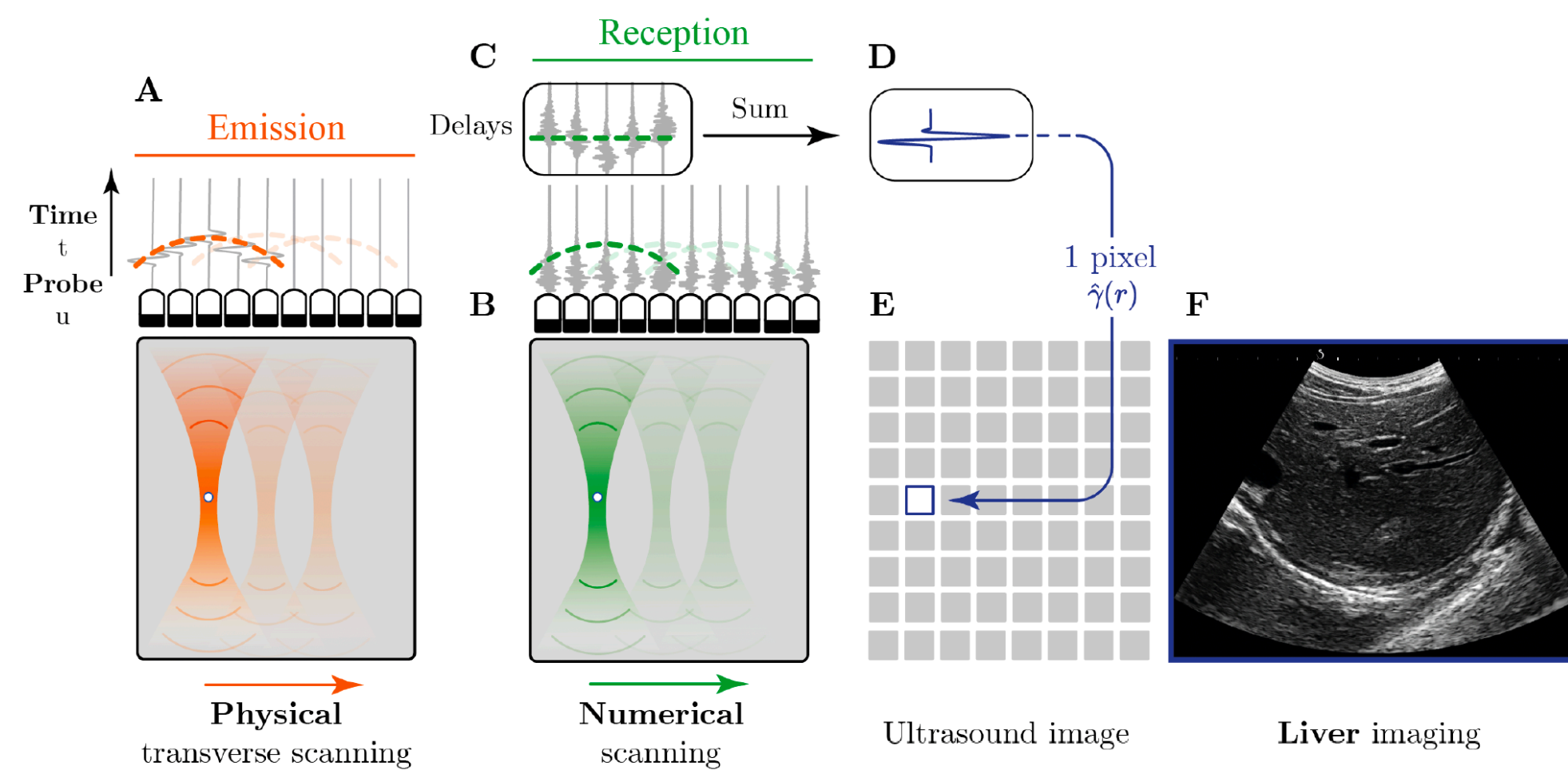
Image is computed using space time correspondance



Principle of ultrasound imaging

Image is computed using space time correspondance

In practice ?



Speed of sound in soft tissues varies ($\pm 10\%$) around a known value
Soft tissues are « weakly scattering »

Principle of ultrasound imaging

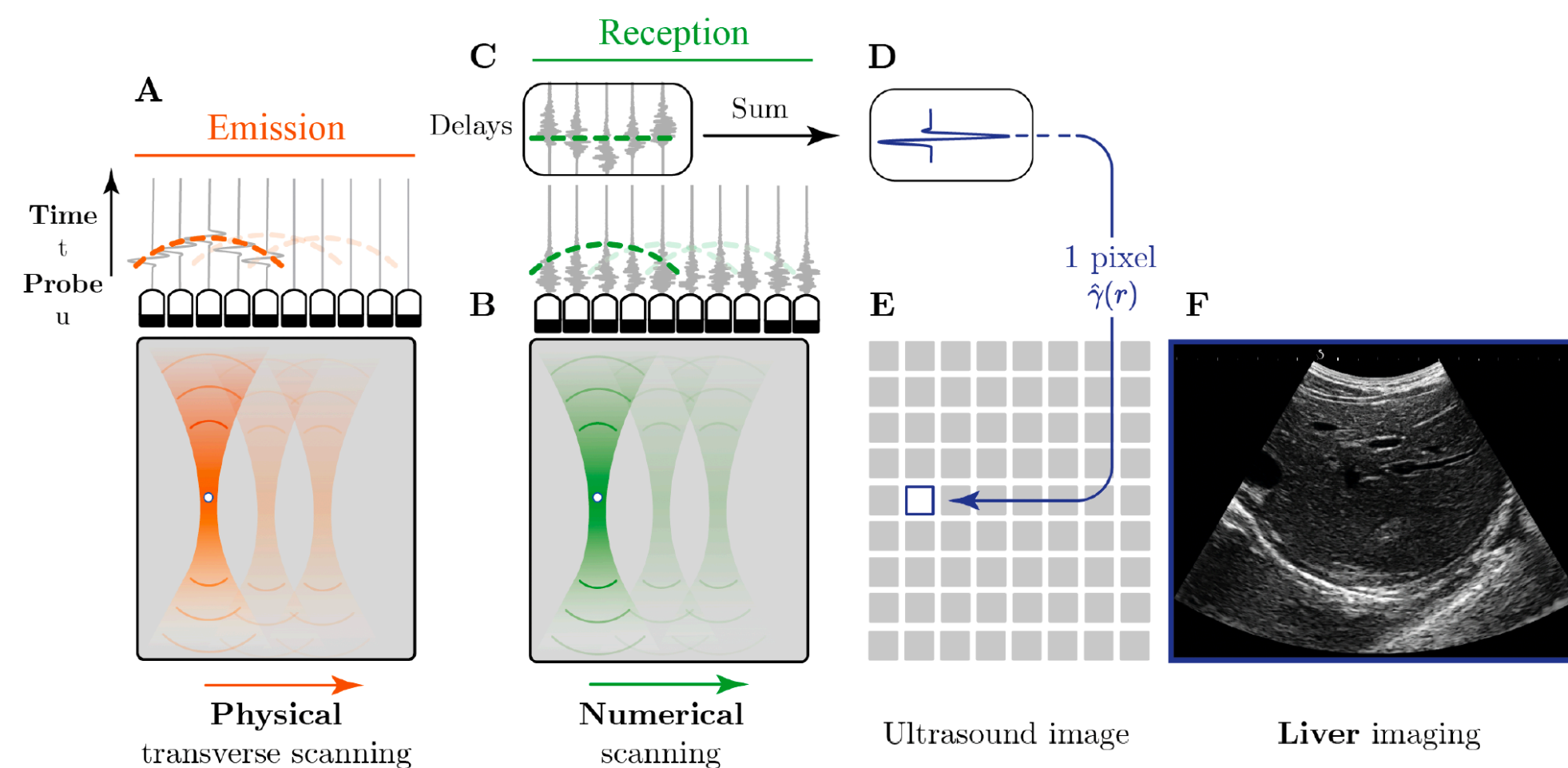
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Constant speed of sound
Single diffusion regime



Principle of ultrasound imaging

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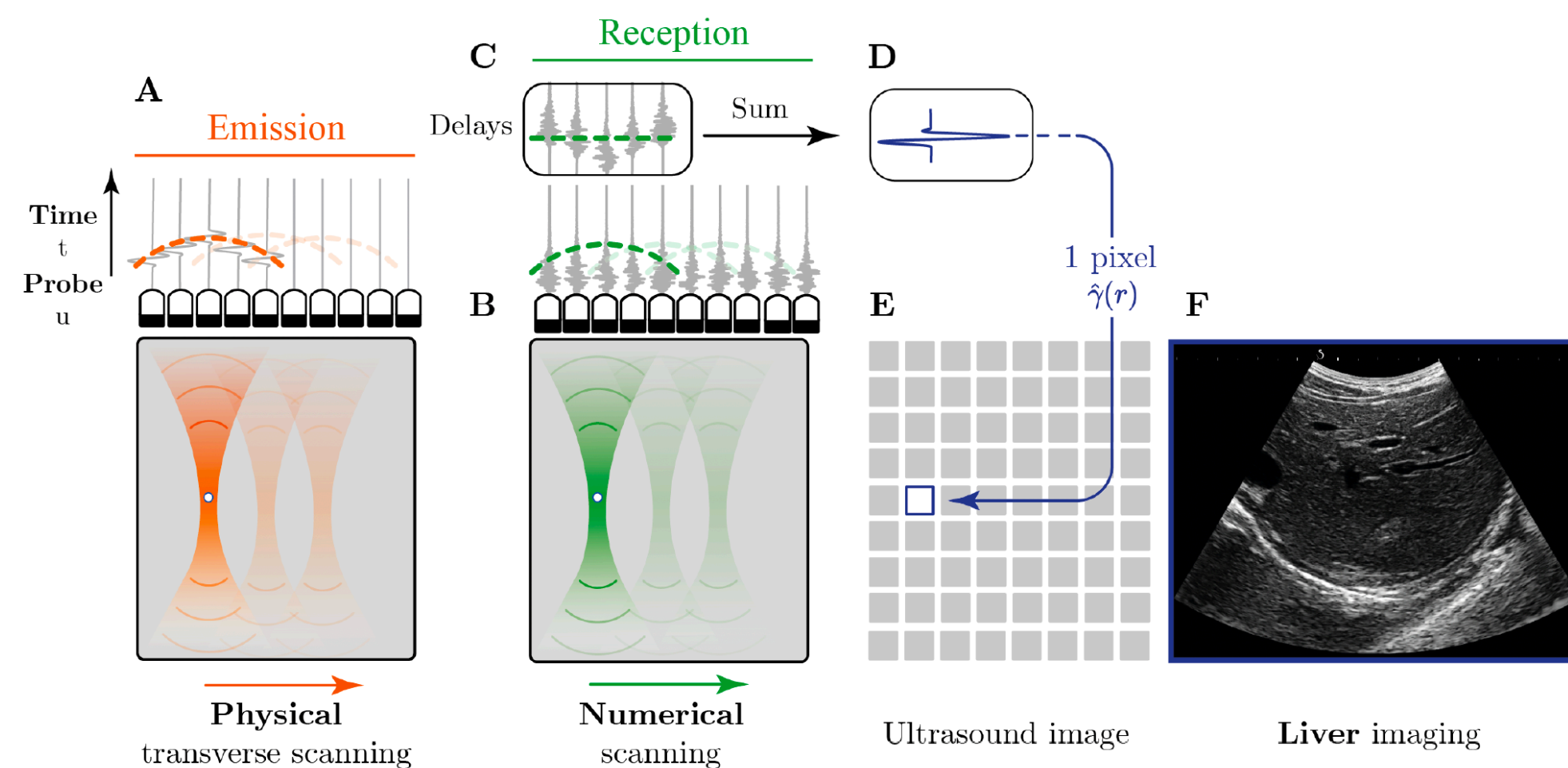
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Improvements

Access to S.O.S

SNR, contrast, resolution, diagnosis..



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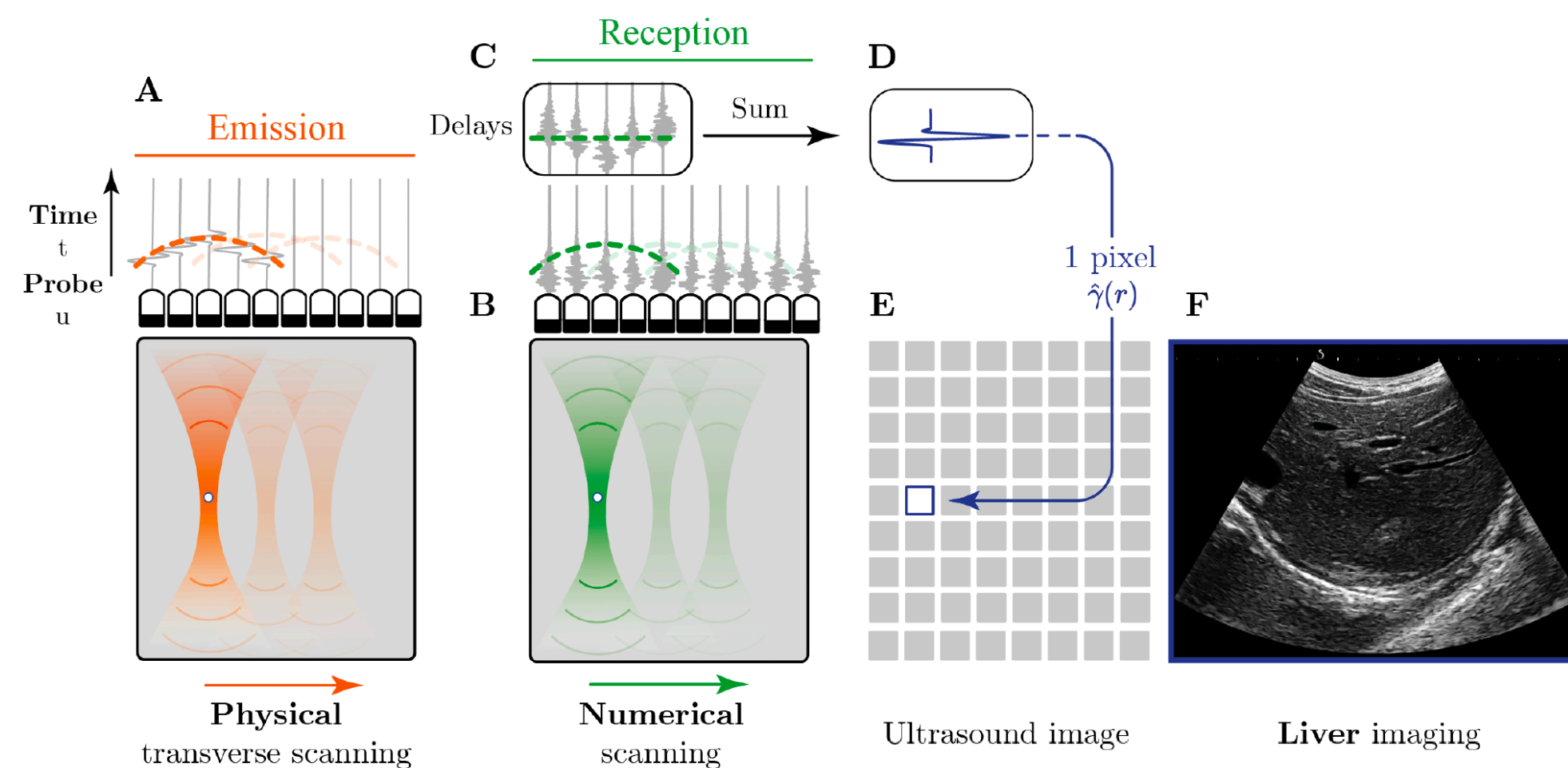
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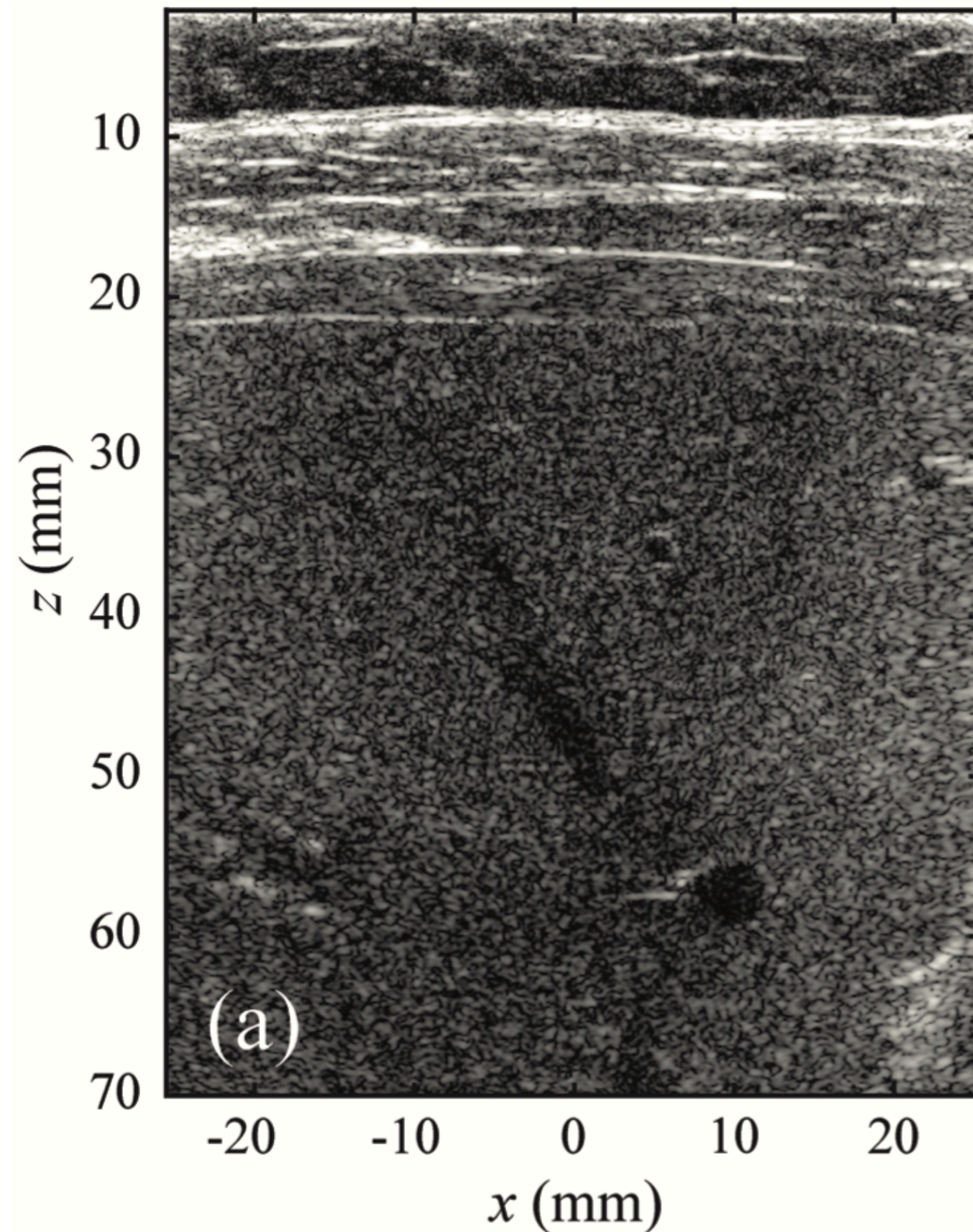
SNR, contrast, resolution, diagnosis..

Signal is the backscattered field

No easy access to travel times



Ultrasound images in soft tissues



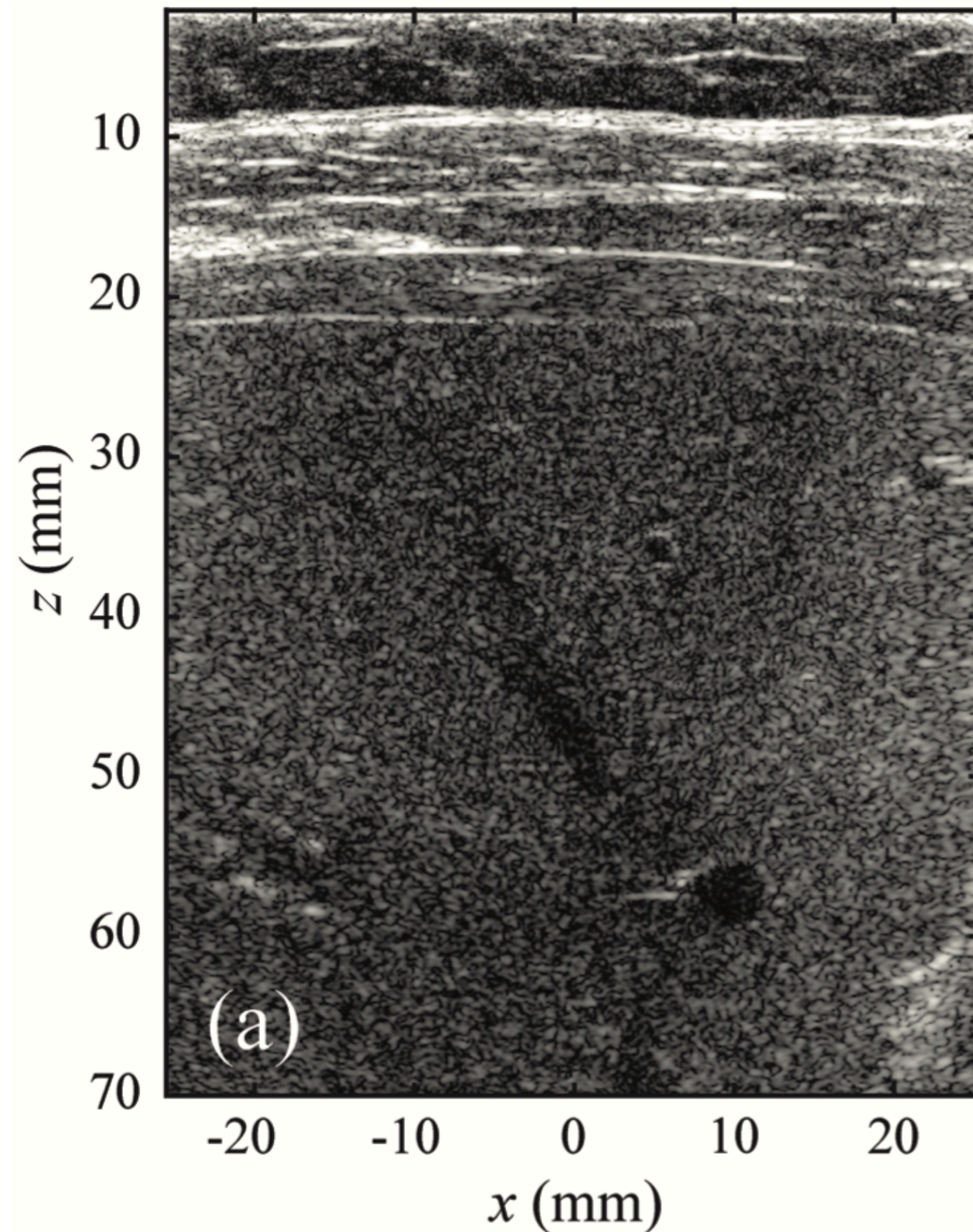
Ultrasound image of a liver
(W. Lambert)

Backscattered signal is generated by discontinuities of acoustic impedance $Z = \sqrt{\frac{\rho}{K}}$

Density

Compressibility

Ultrasound images in soft tissues



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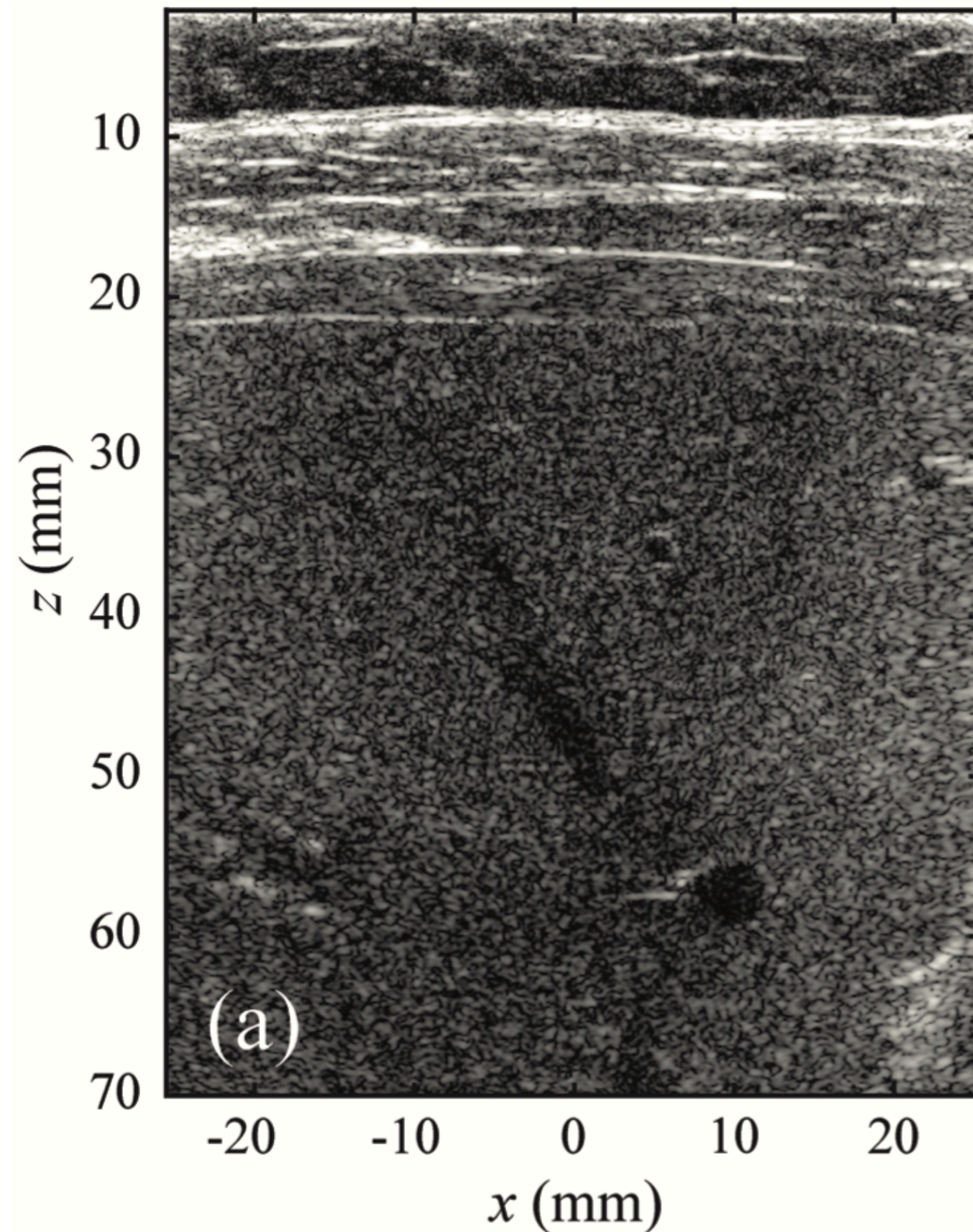
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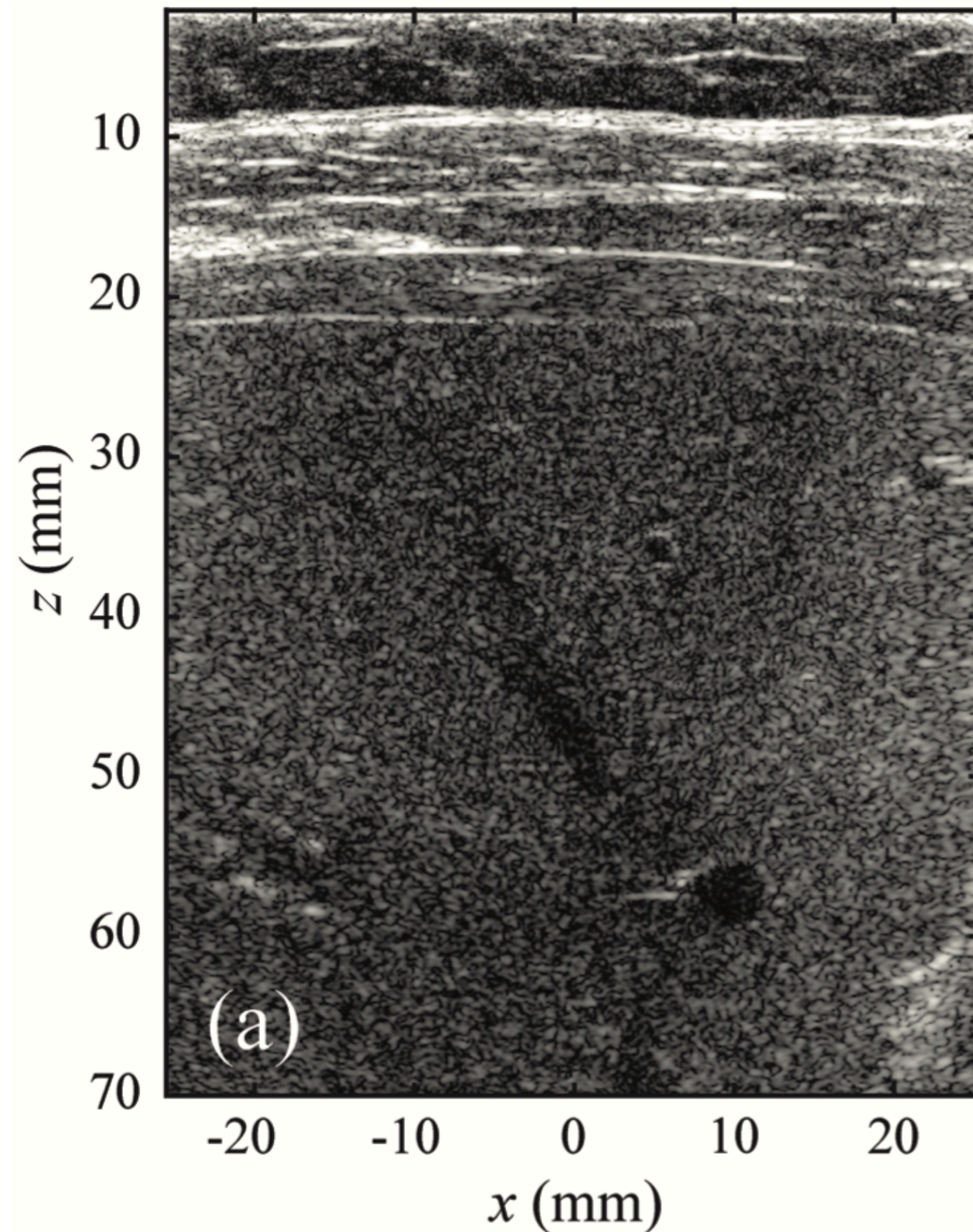
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No access to the PSF

PSF probing in the speckle

Reflection Matrix Imaging for Wave Velocity Tomography

Flavien Bureau,¹ Elsa Giraudat,¹ Arthur Le Ber,¹ William Lambert,²

Louis Carmier,³ Aymeric Guibal,⁴ Mathias Fink,¹ and Alexandre Aubry*¹

¹*Institut Langevin, ESPCI Paris, PSL University, CNRS, 75005 Paris, France*

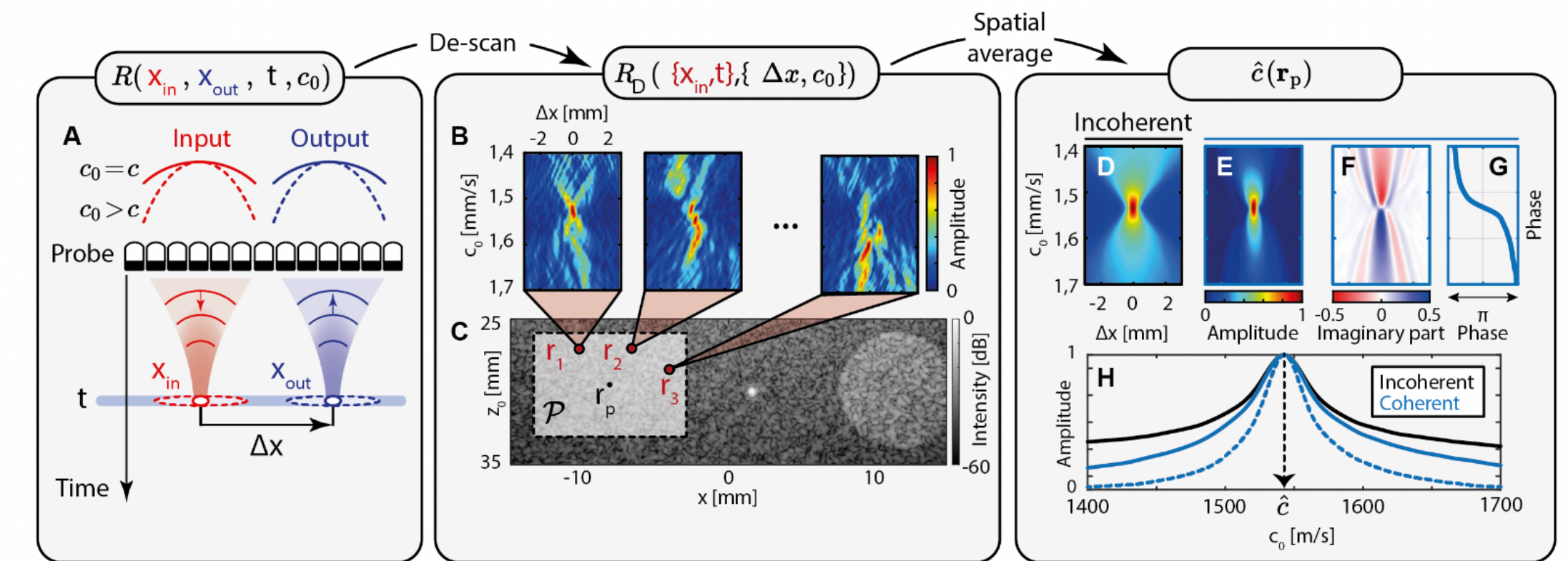
²*SuperSonic Imagine, Aix-en-Provence, France*

³*Department of Radiology, Centre Hospitalier Universitaire de Montpellier, France*

⁴*Department of Radiology, Centre Hospitalier Général de Perpignan, France*

*Corresponding author (e-mail: alexandre.aubry@espci.fr)

(Dated: September 24, 2024)



Experimental work by A. Aubry and his team at Institut Langevin.

New method to reconstruct the **propagation speed** of ultrasounds in **soft tissues** inspired by adaptative optics

Provide a robust mathematical model for this inverse problem

Content

1. MODEL / DIRECT PROBLEM

2. INVERSE PROBLEM

Content

1. MODEL / DIRECT PROBLEM

2. INVERSE PROBLEM

What is is that we measure

What do we do with those measurements

Content

1. Stochastic Homogenization of the Wave Equation

1.1. The Scattering Problem

1.2. Model for Soft Tissues

1.3. Homogenization & Representation Of The Scattered Field

2. Ultrasound Imaging Analysis

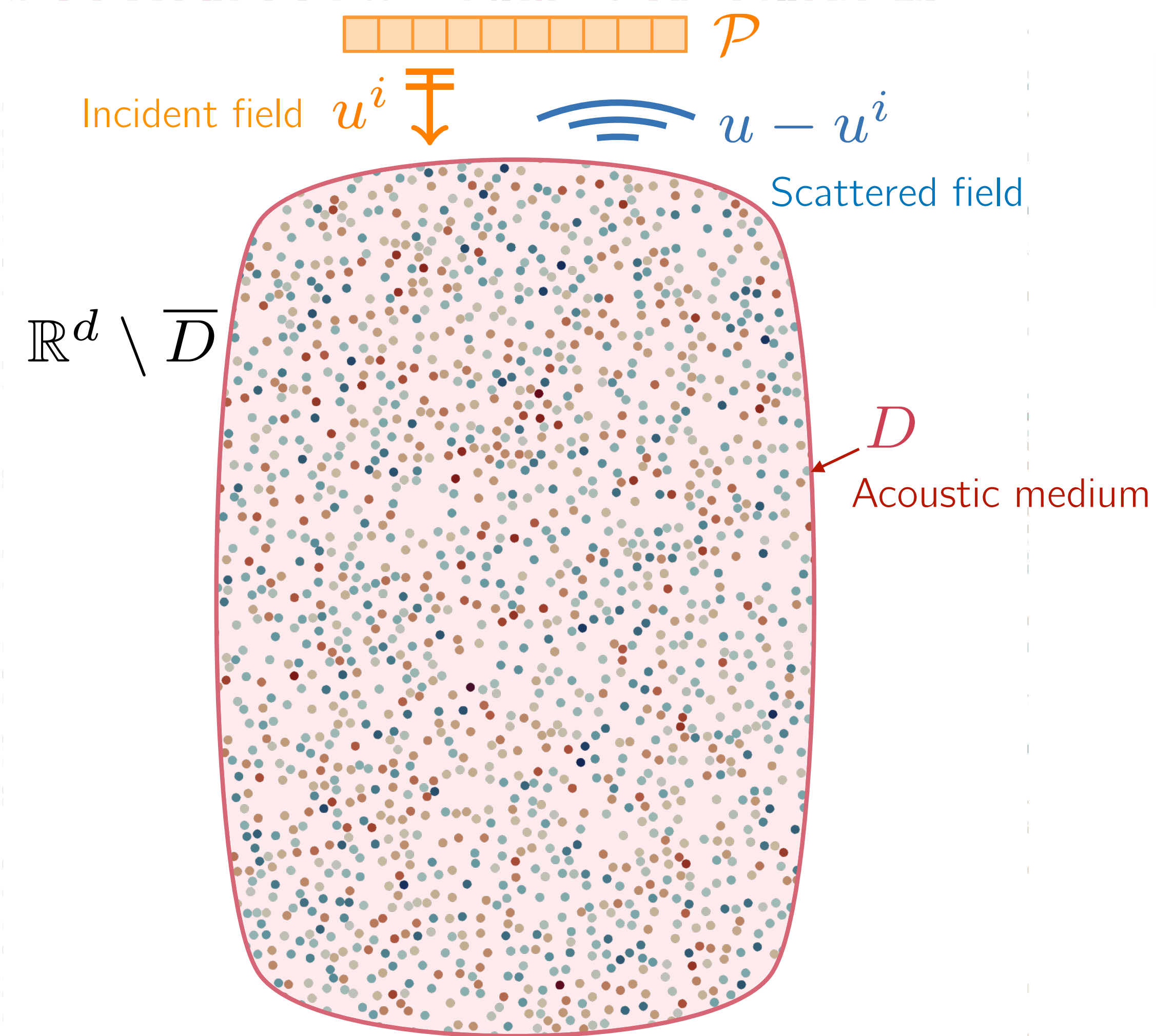
2.1. Mathematical Model

2.2. The Focal Spot

2.3. Sound Speed Estimators

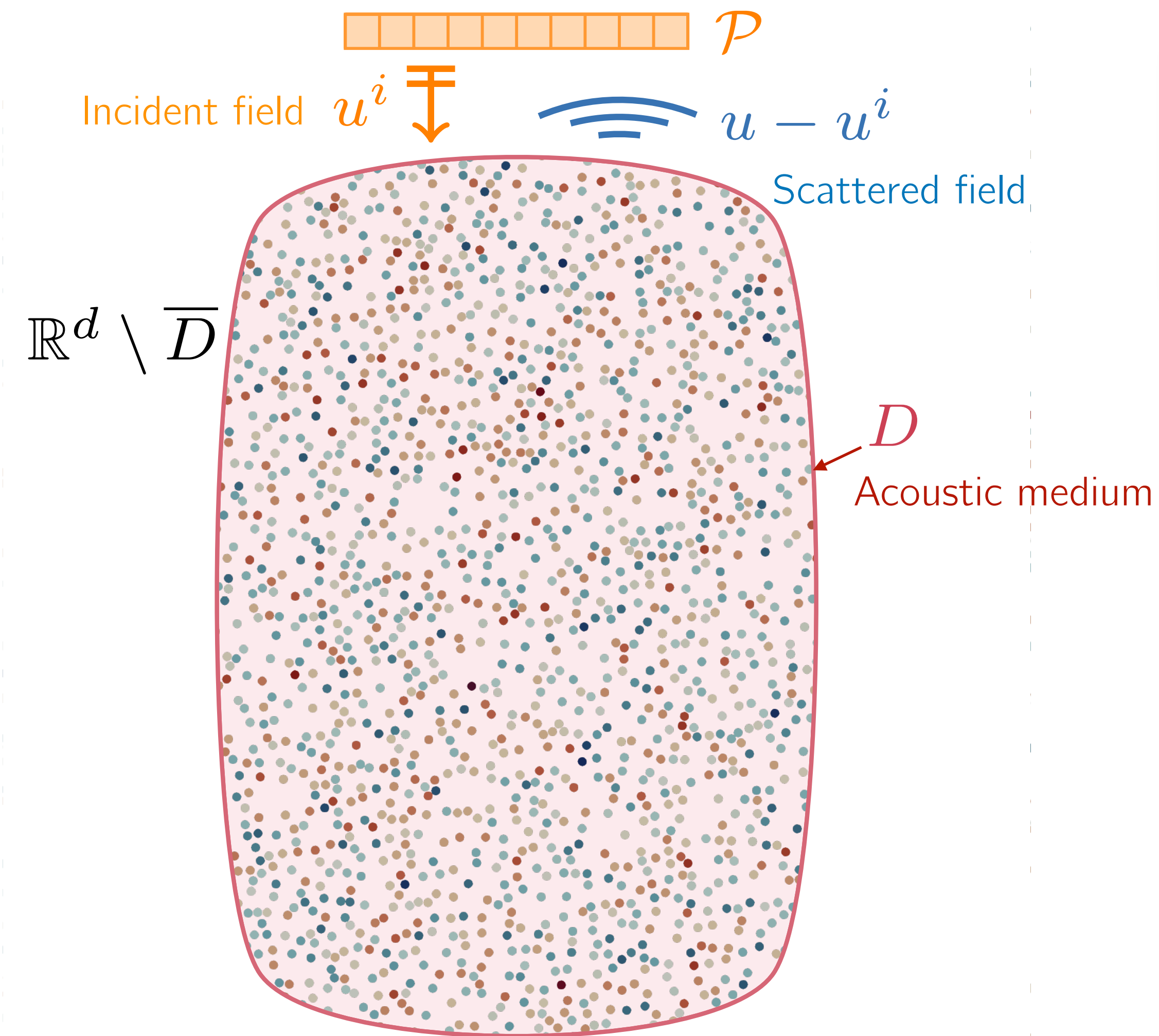
2.4. Focusing in the speckle

The acoustic scattering problem



$$\begin{cases} \nabla \cdot (a \nabla u) + \omega^2 n u = 0 \\ \lim_{|x| \rightarrow \infty} |x|^{\frac{d-1}{2}} \left(\partial_{|x|} (u - u^i) - i k_0 (u - u^i) \right) = 0. \end{cases}$$

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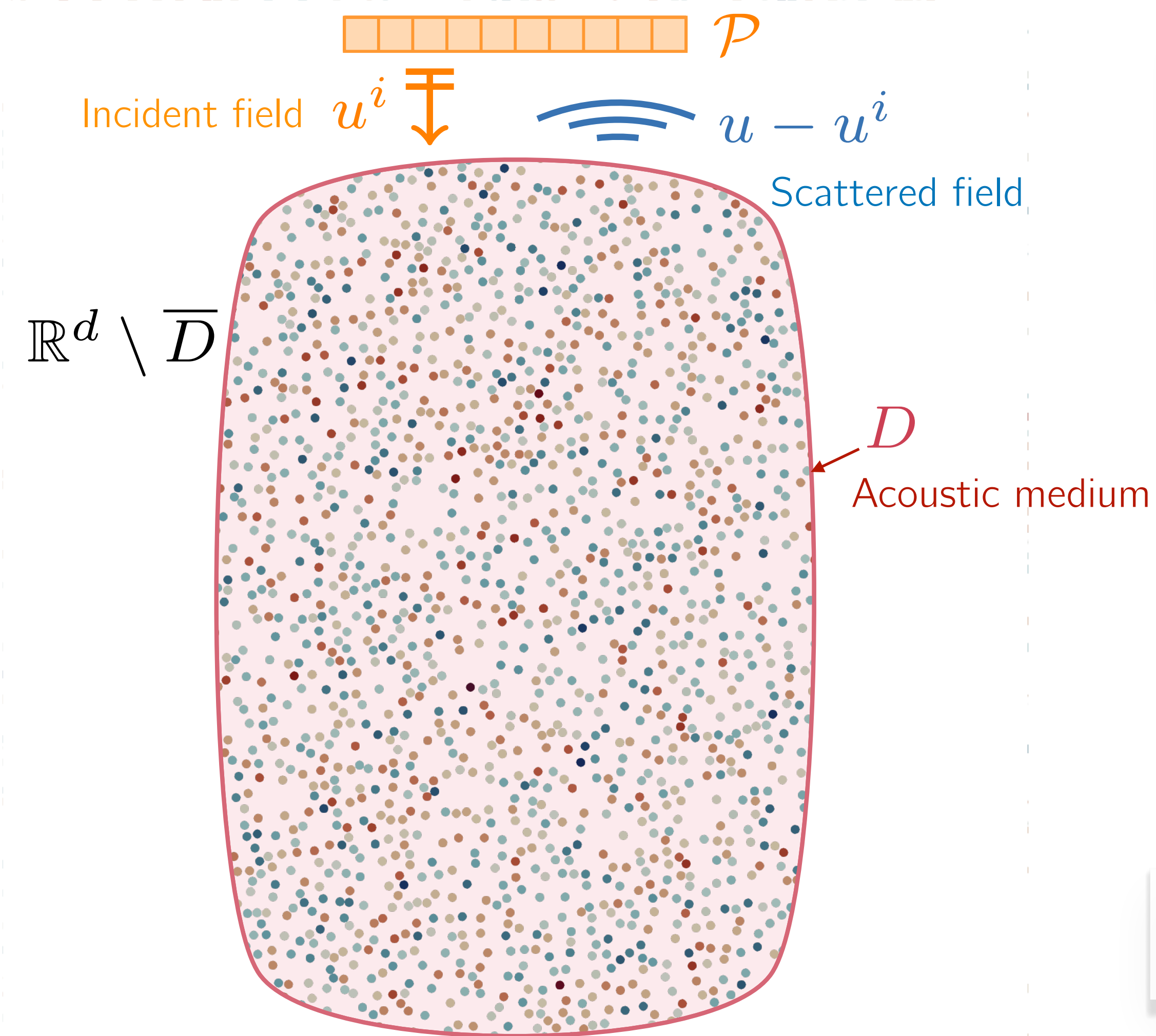
Physical parameters:

$$a(x) := a_0 \mathbb{1}_{\mathbb{R}^d \setminus \overline{D}} + a_D(x) \mathbb{1}_D,$$

$$n(x) := n_0 \mathbb{1}_{\mathbb{R}^d \setminus \overline{D}} + n_D(x) \mathbb{1}_D.$$

$$k_0 := \omega \sqrt{n_0 a_0^{-1}}$$

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$$k_0 := \omega \sqrt{n_0 a_0^{-1}}$$

What is a good model for $a(x)$ and $n(x)$?

Model for soft tissues

Soft tissues are incredibly complex

Realistic model for $a(x)$ and $n(x)$ is a lost cause

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Tissue-mimicking phantoms are much simpler :

LOTS of small scatterers densely embedded in an homogeneous matrix

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Variation in speed of sound obtained by locally changing the repartition of scatterers

Mathematical framework requirements

Random

Stable w/ respect to size and number of scatterers

Can infer macroscopic quantities from the micro-structure

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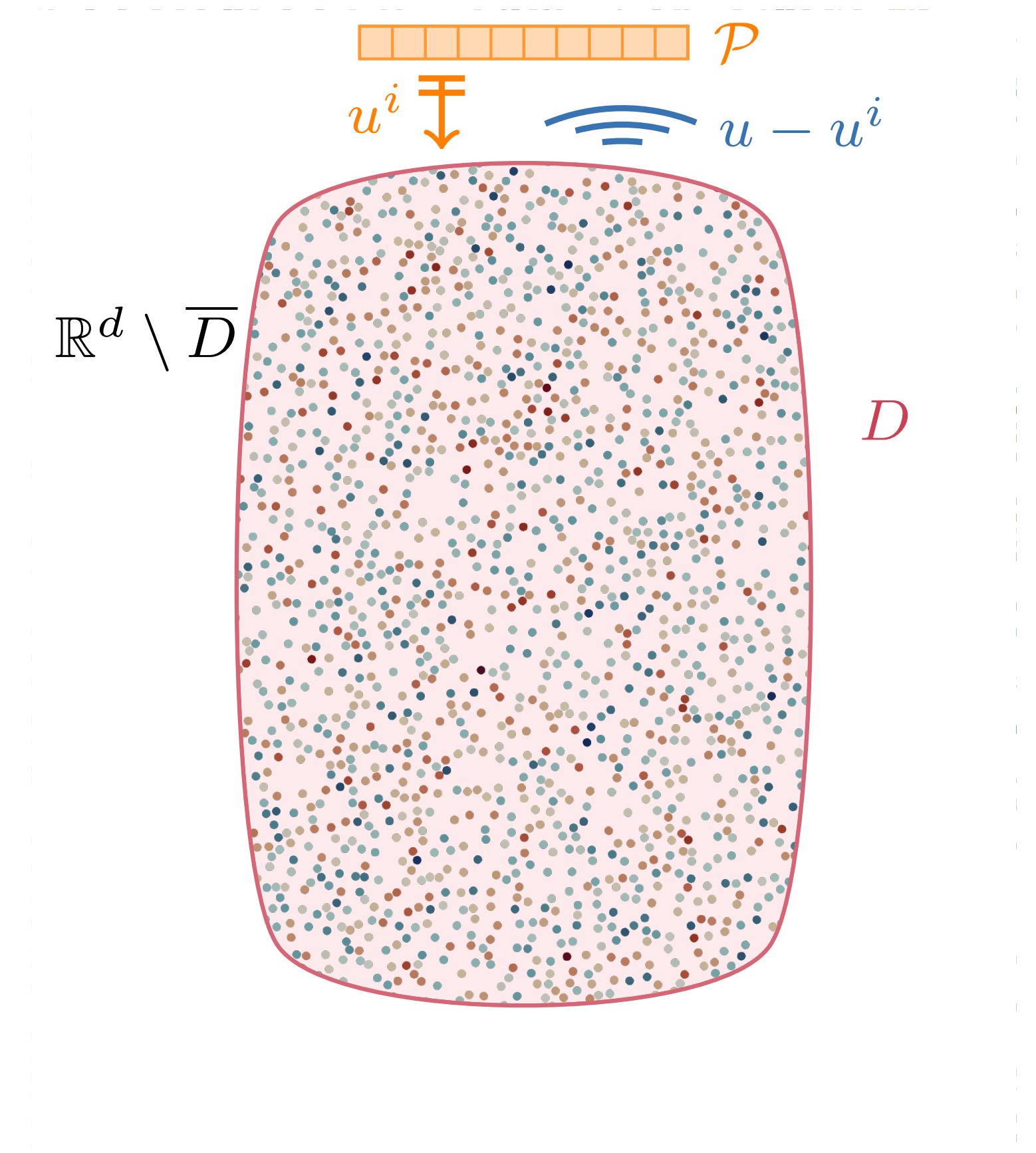
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Stochastic Homogenization

Mathematical description of the micro-structured medium

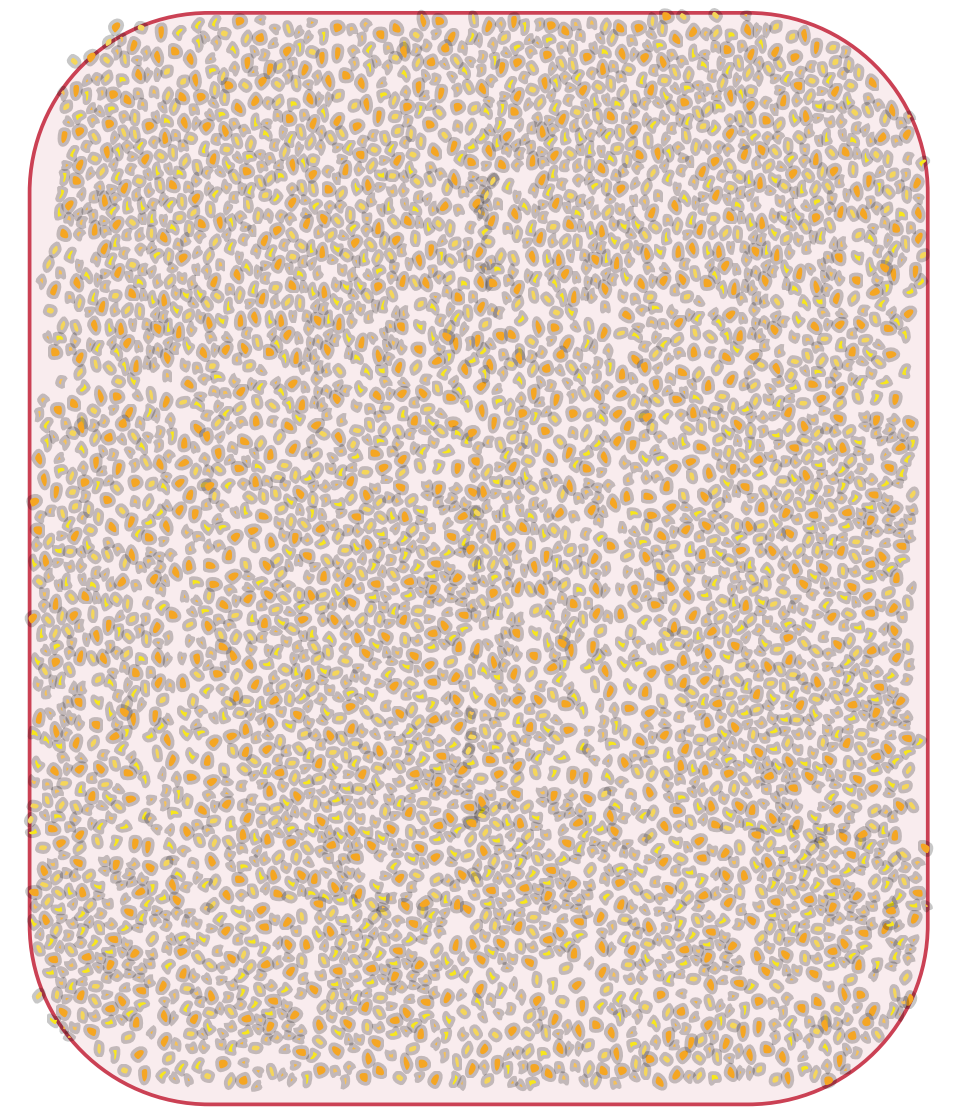
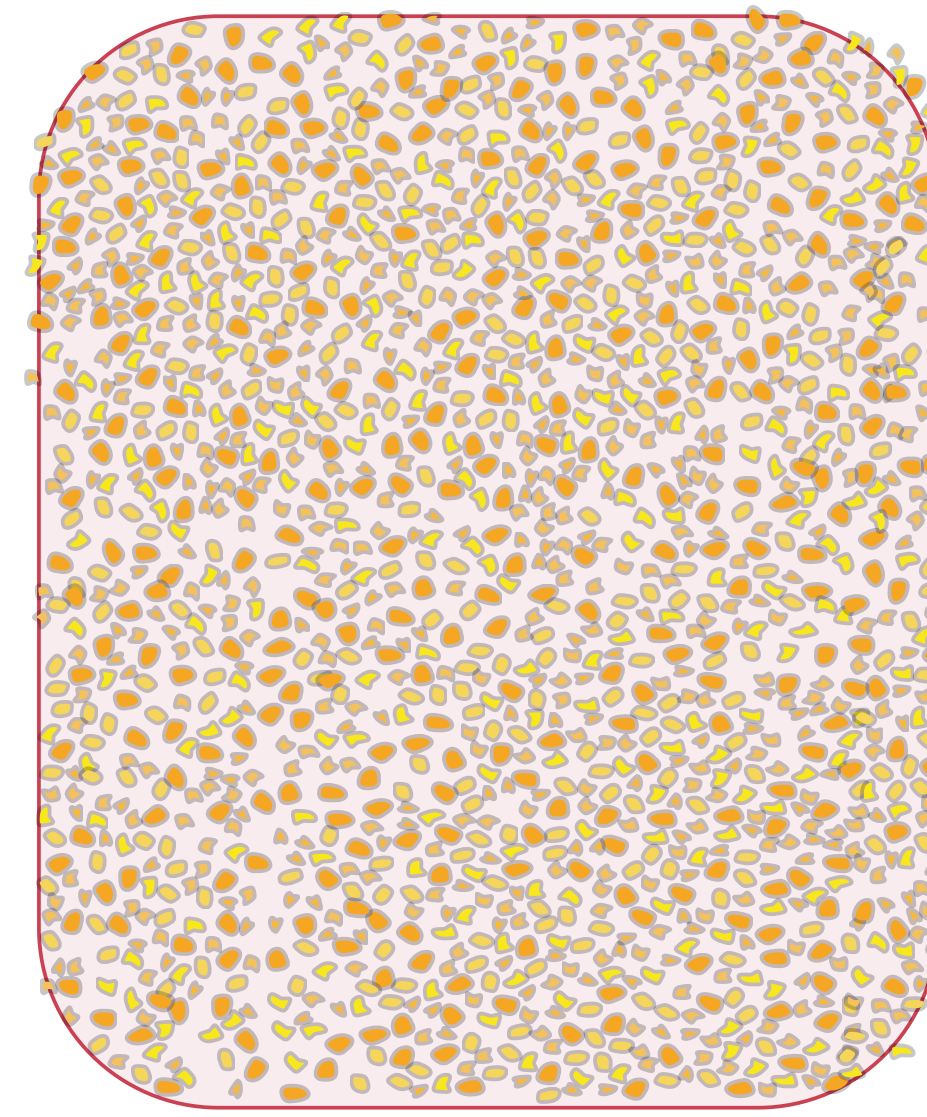
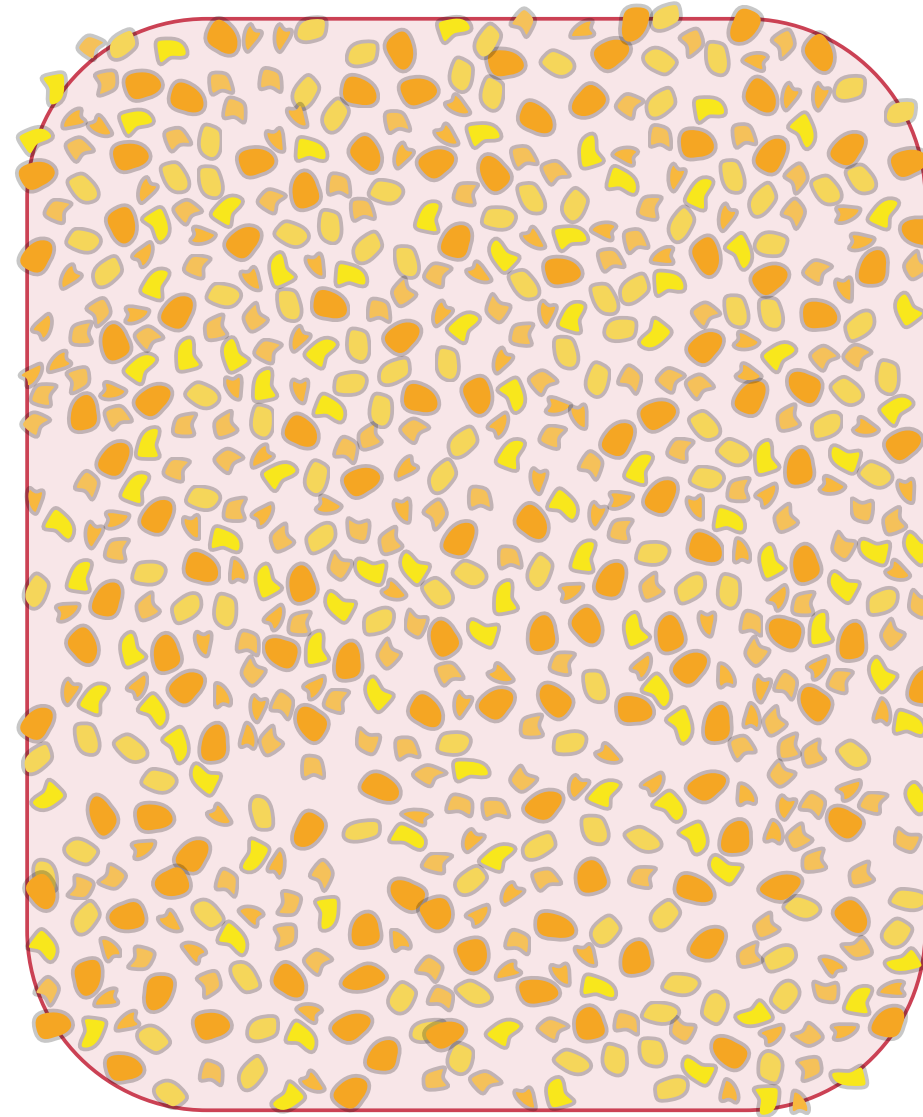
$\mathcal{Q}_i$ Domains of measure 1

x_i Random centers distributed in $\mathbb{R}^d$

$S = \cup_i \{x_i + \mathcal{Q}\}$ Set of size 1 scatterers

$$\begin{cases} a_1 := a_M \mathbb{1}_{\mathbb{R}^d \setminus \overline{S}} + a_S \mathbb{1}_S, \\ n_1 := n_M \mathbb{1}_{\mathbb{R}^d \setminus \overline{S}} + n_S \mathbb{1}_S. \end{cases}$$

$$\forall x \in D \begin{cases} a_D^\varepsilon(x) = a_1 \left(\frac{x}{\varepsilon} \right), \\ n_D^\varepsilon(x) := n_1 \left(\frac{x}{\varepsilon} \right). \end{cases}$$



Example with $\varepsilon_1 > \varepsilon_2 > \varepsilon_3$

Mathematical description of the micro-structured medium

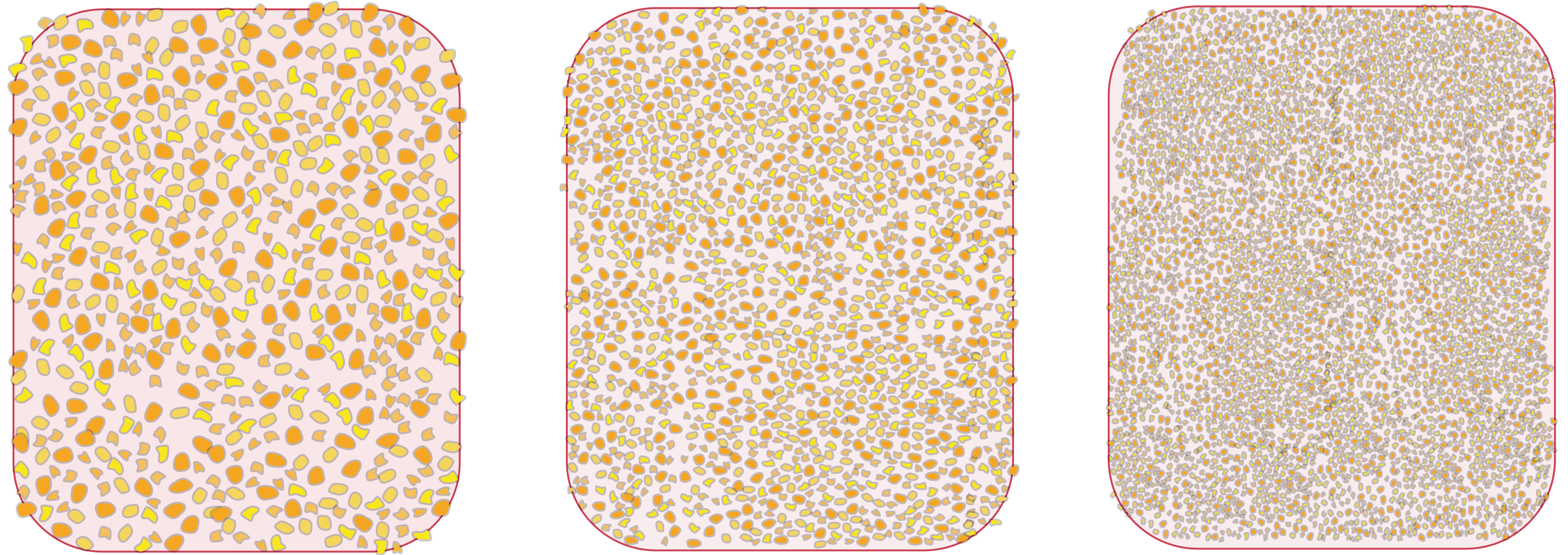
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Simplification $a \equiv 1$

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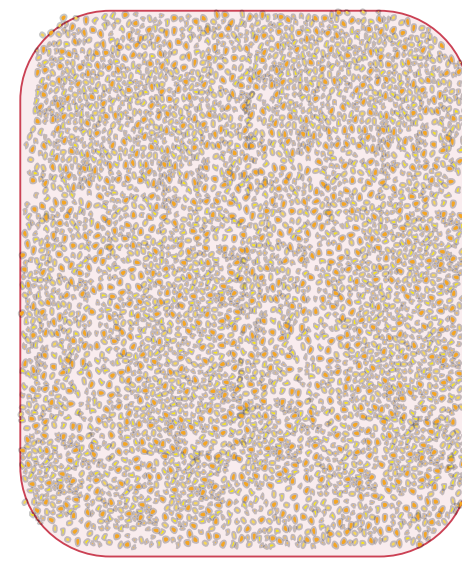
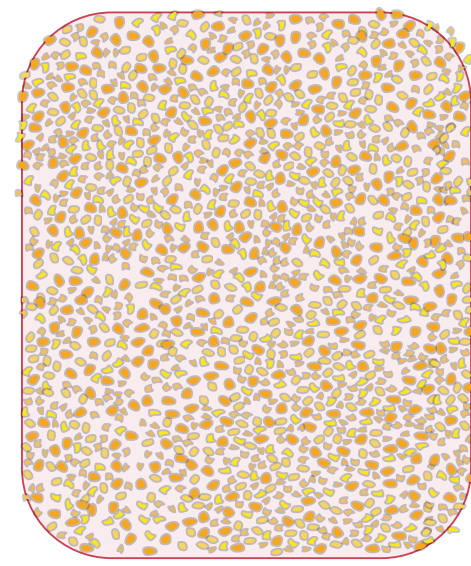
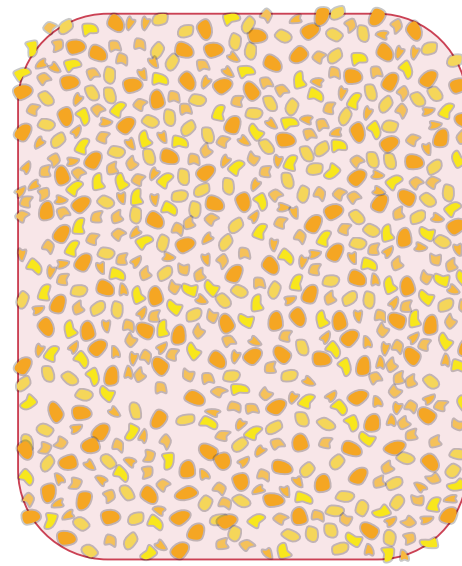
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Example with $\varepsilon_1 > \varepsilon_2 > \varepsilon_3$



Simplification $a \equiv 1$

For the case $a \neq 1$
see L. Giovangigli's talk

The coherent field

Governing equation total field u

$$\begin{cases} \Delta u + \omega^2(n_0 + (n_\varepsilon - n_0)\mathbb{1}_D)u = 0 \\ \lim_{|x| \rightarrow \infty} |x|^{\frac{d-1}{2}} \left(\partial_{|x|} (u - u^i) - ik_0 (u - u^i) \right) = 0. \end{cases}$$

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Governing equation coherent field u_0

$$\begin{cases} \Delta u_0 + \omega^2(n_0 + (\textcolor{red}{n}^\star - n_0)\mathbb{1}_D)u_0 = 0 \\ \lim_{|x| \rightarrow \infty} |x|^{\frac{d-1}{2}} \left(\partial_{|x|} (u_0 - u^i) - ik_0 (u_0 - u^i) \right) = 0. \end{cases}$$

Effective index in D

$$\textcolor{red}{n}^\star \equiv \mathbb{E}[n_\varepsilon]$$

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Speed of sound outside of D

Effective speed of sound in D

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Effective index in D

$$\textcolor{red}{n}^\star \equiv \mathbb{E}[n_\varepsilon]$$

Homogenized Green function

$$\begin{cases} \Delta G^\star(\cdot, y) + \omega^2(n_0 + (\textcolor{red}{n}^\star - n_0)\mathbb{1}_D)G^\star(\cdot, y) = \delta_y \\ \lim_{|x| \rightarrow \infty} |x|^{\frac{d-1}{2}} (\partial_{|x|} G^\star(x, y) - ik_0 G^\star(x, y)) = 0. \end{cases}$$

$$k_0 := \omega \sqrt{n_0} := \frac{\omega}{c_0}$$

Speed of sound outside of D

$$\textcolor{red}{k}^\star := \omega \sqrt{\textcolor{red}{n}^\star} := \frac{\omega}{\textcolor{red}{c}^\star}$$

Effective speed of sound in D

The scattered field

$$\mathcal{U}^s := \omega^2 \int_D (n_\varepsilon(y) - n^\star) u_0(y) G^\star(\cdot, y) dy.$$

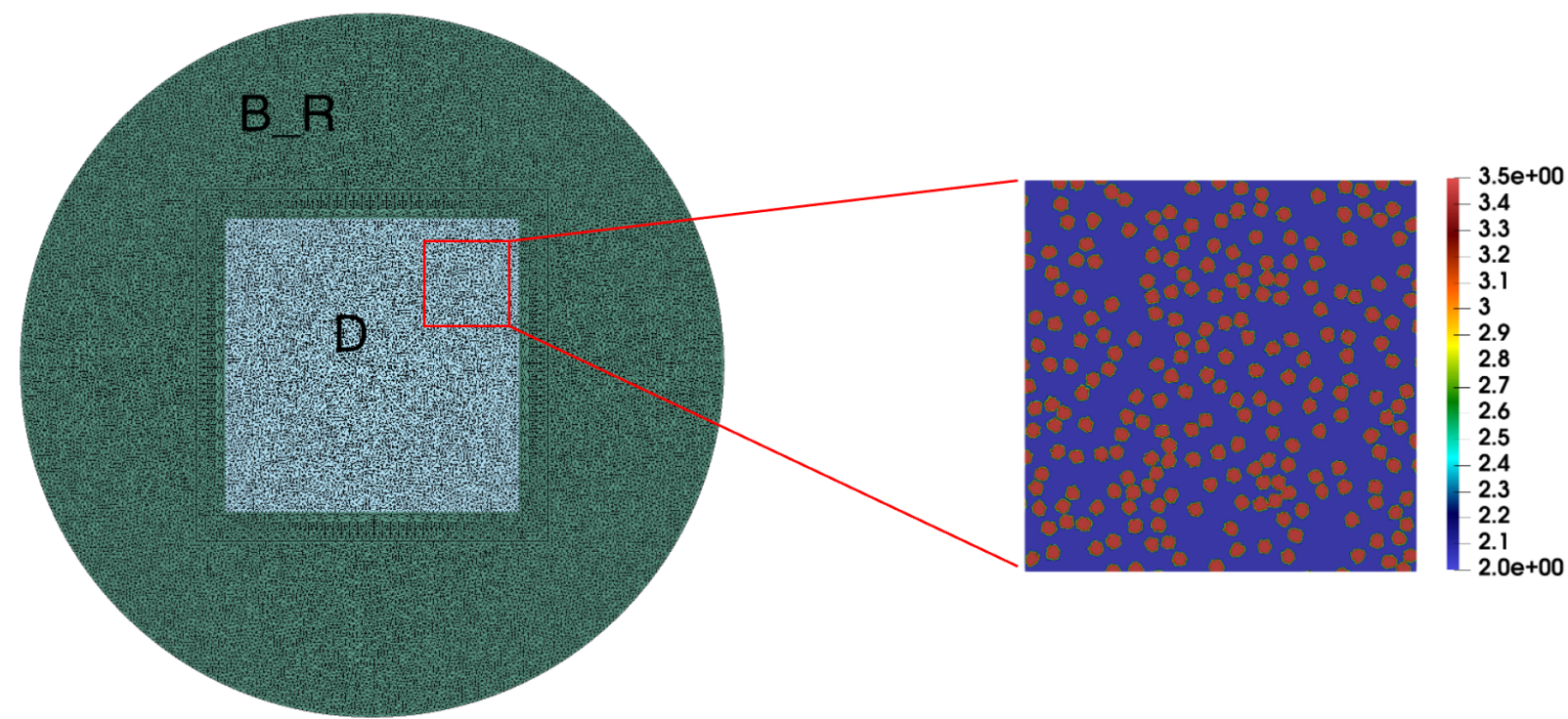
Quantitative Homogenization Theorem (Garnier, Giovangigli, Goepfert, M.)

$$\|u(x) - u^i(x) - \mathcal{U}^s(x)\|_{L^2(\Omega)} \leq C_\omega \varepsilon^{\frac{d}{p'}} \quad \forall x \in \mathcal{P}$$

$$C_\omega \text{ indep. of } \varepsilon \text{ and } x. \quad p' = \frac{2 + \beta}{1 + \beta} \quad \text{w/} \quad \sup_{x \in D} \int_D |G^\star(x, y)|^{2+\beta} dy < \infty$$

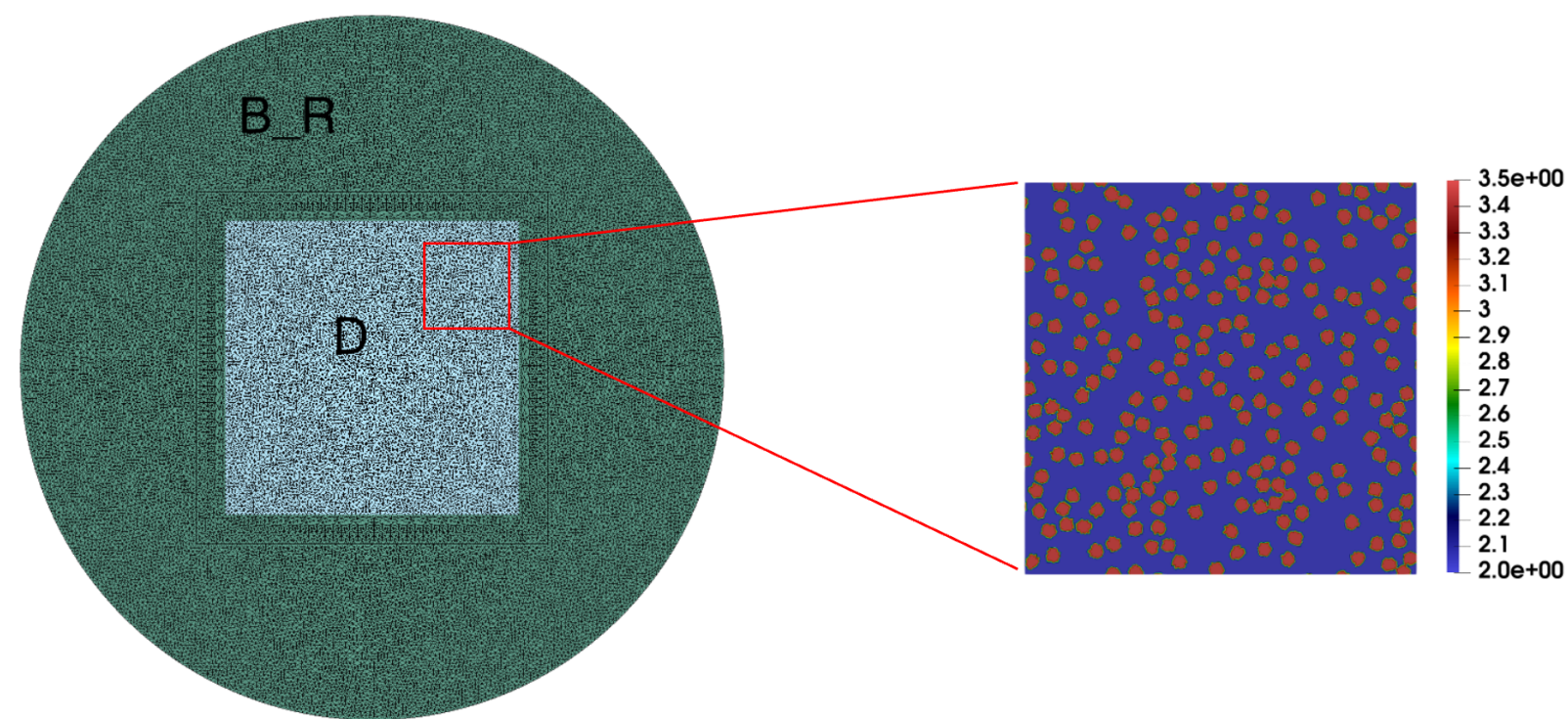
Illustrations

Example of domain

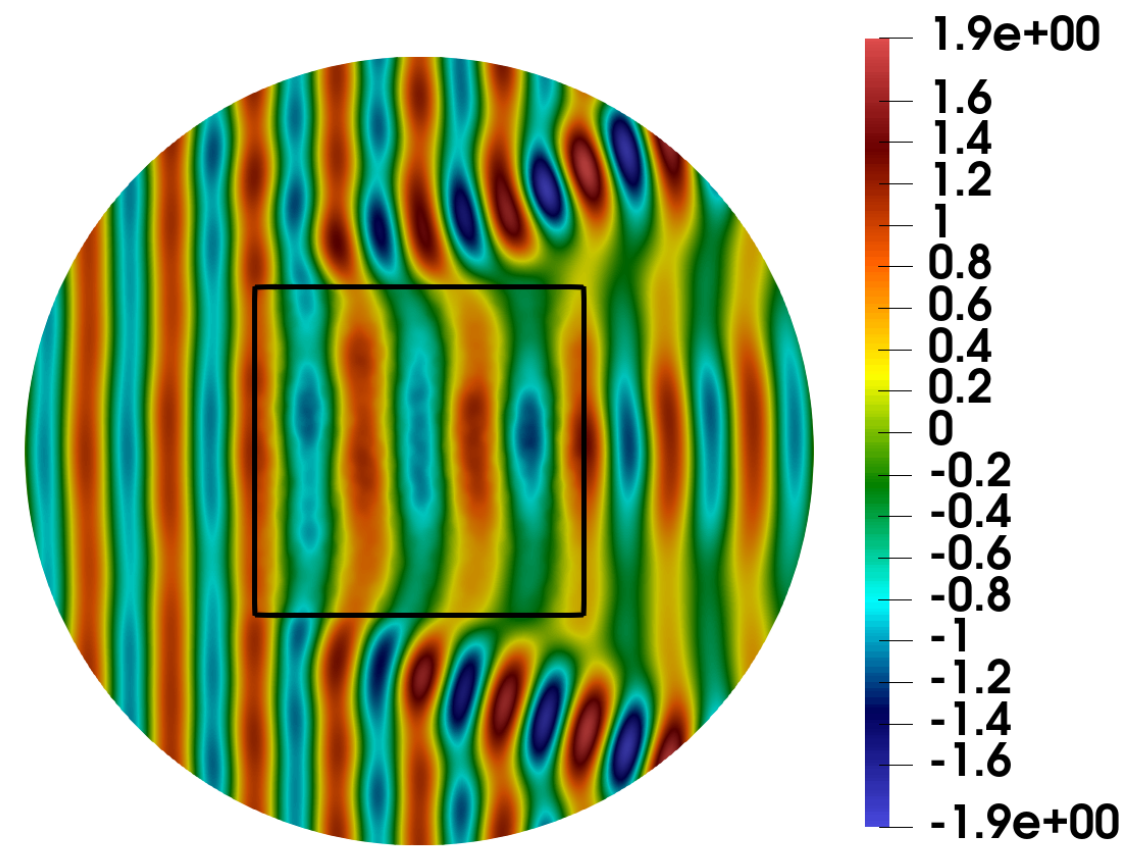


Illustrations

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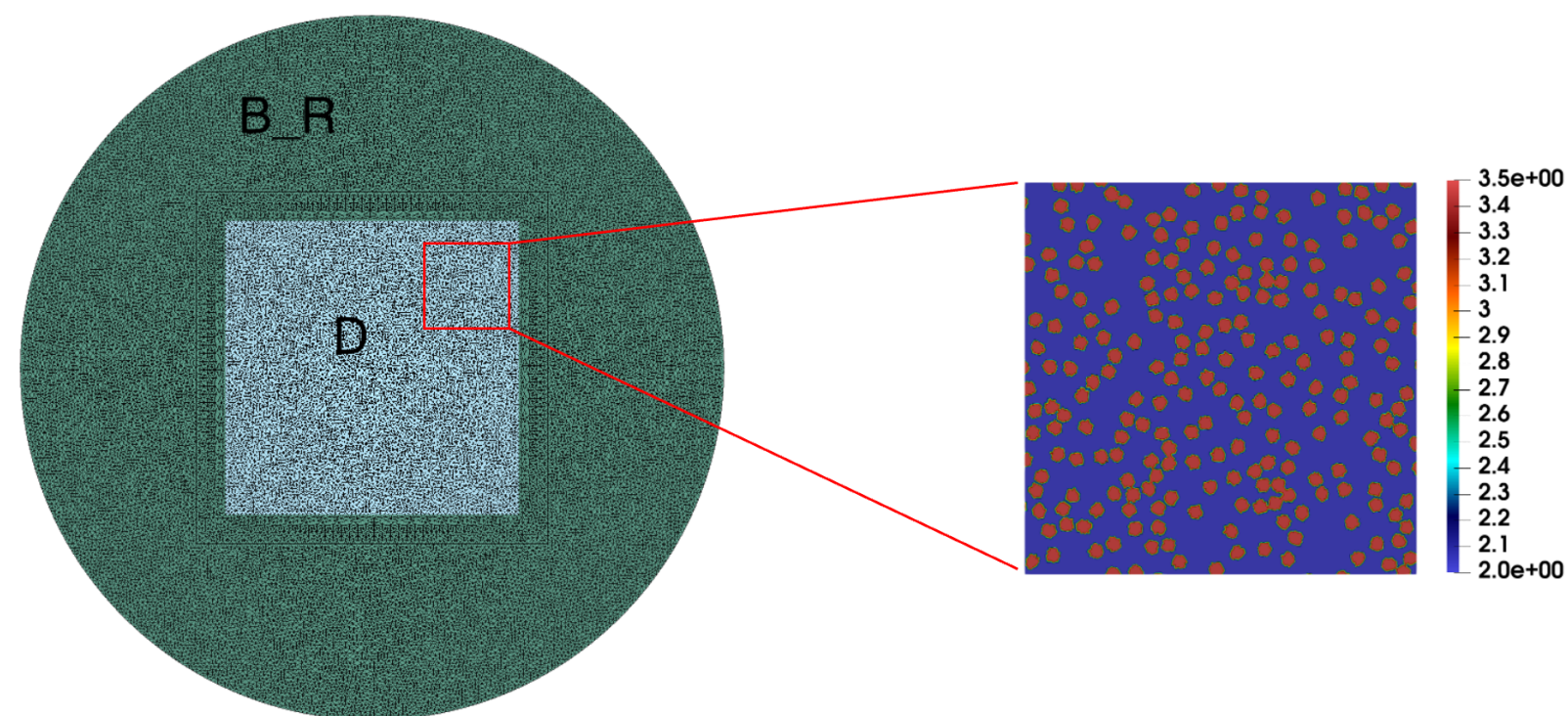


Total field u^ε

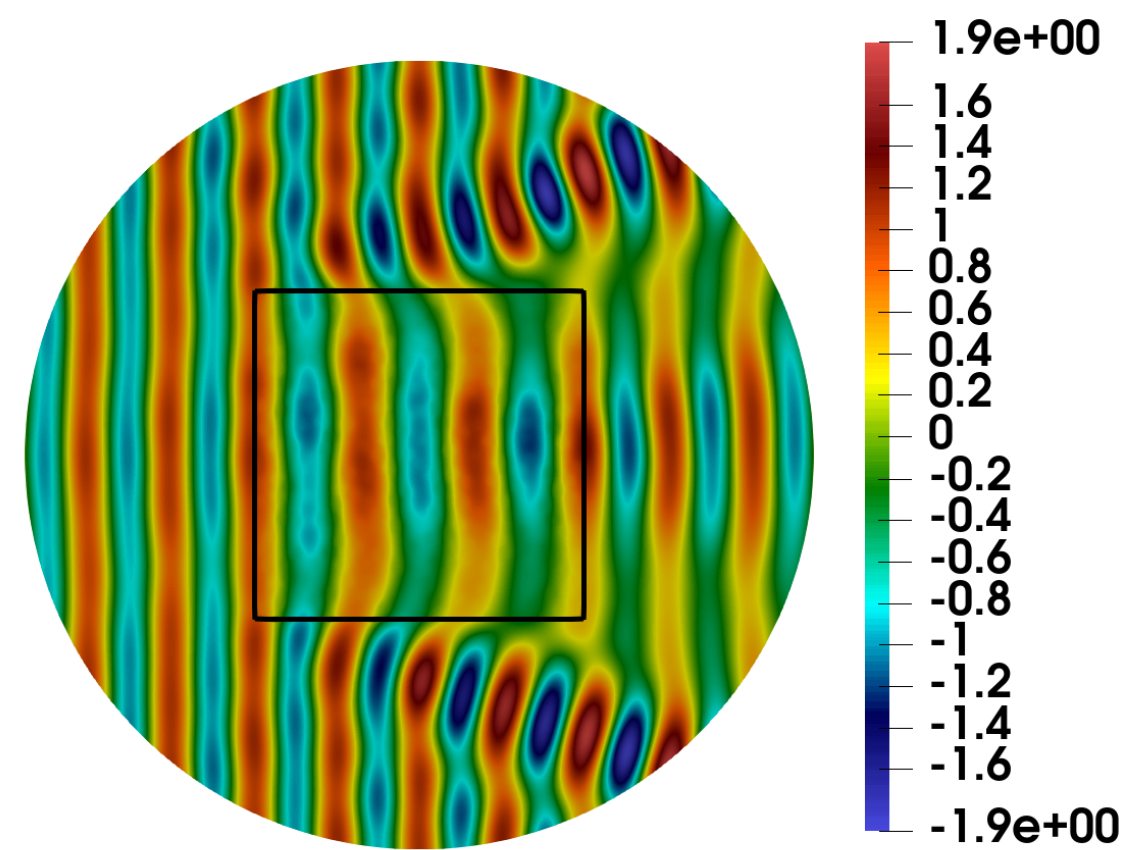


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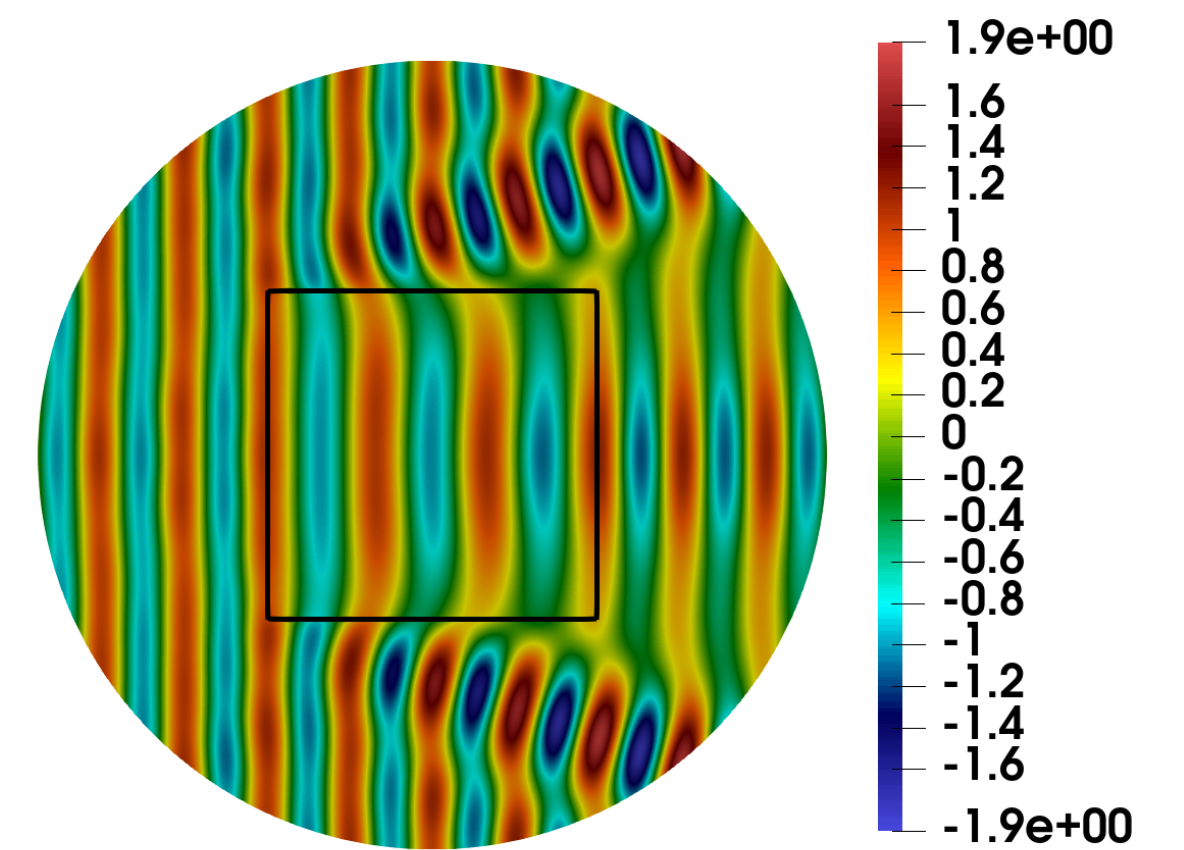
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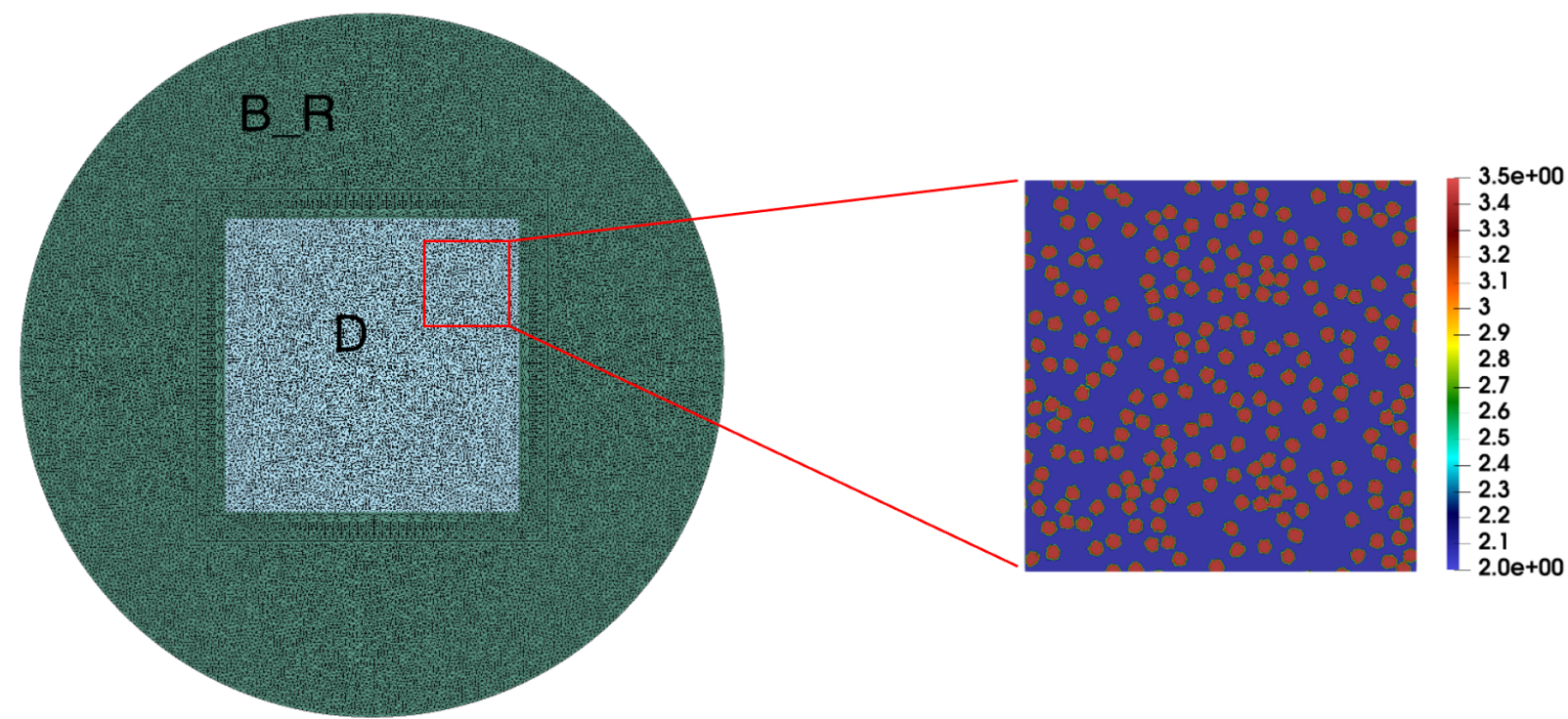


Coherent field u_0

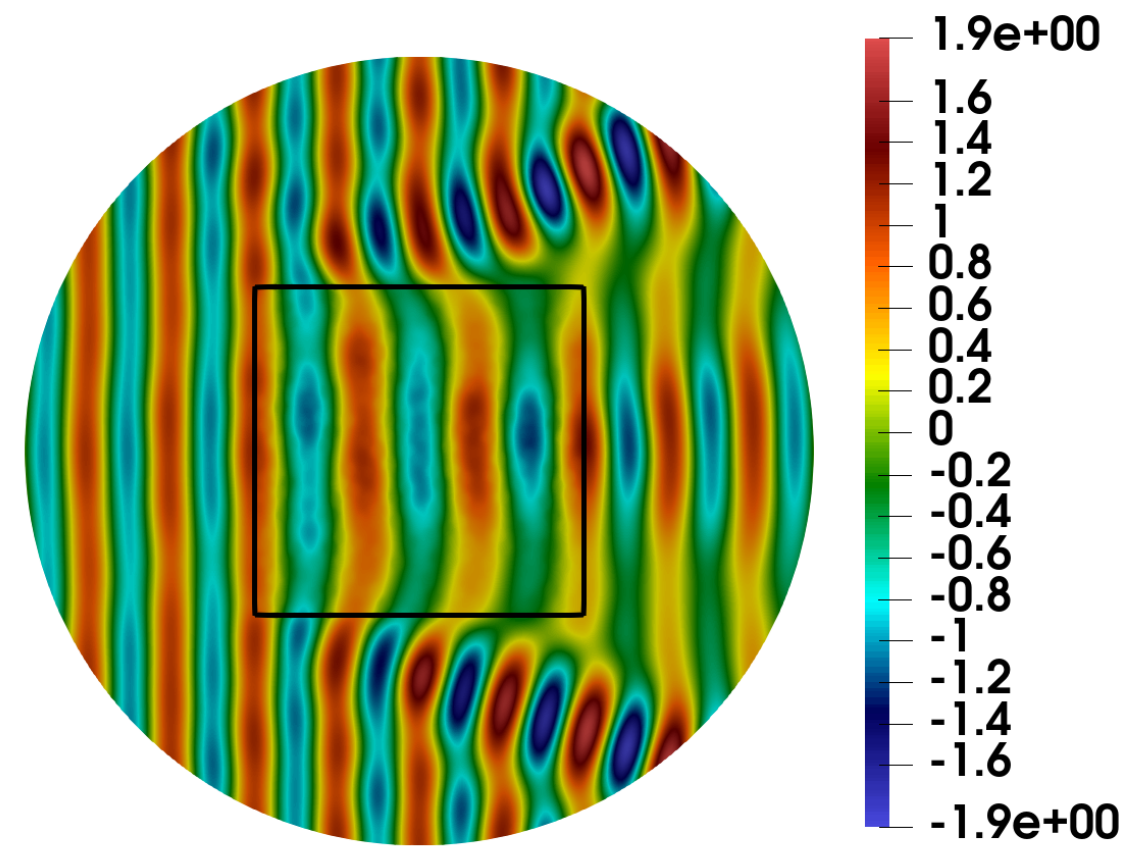


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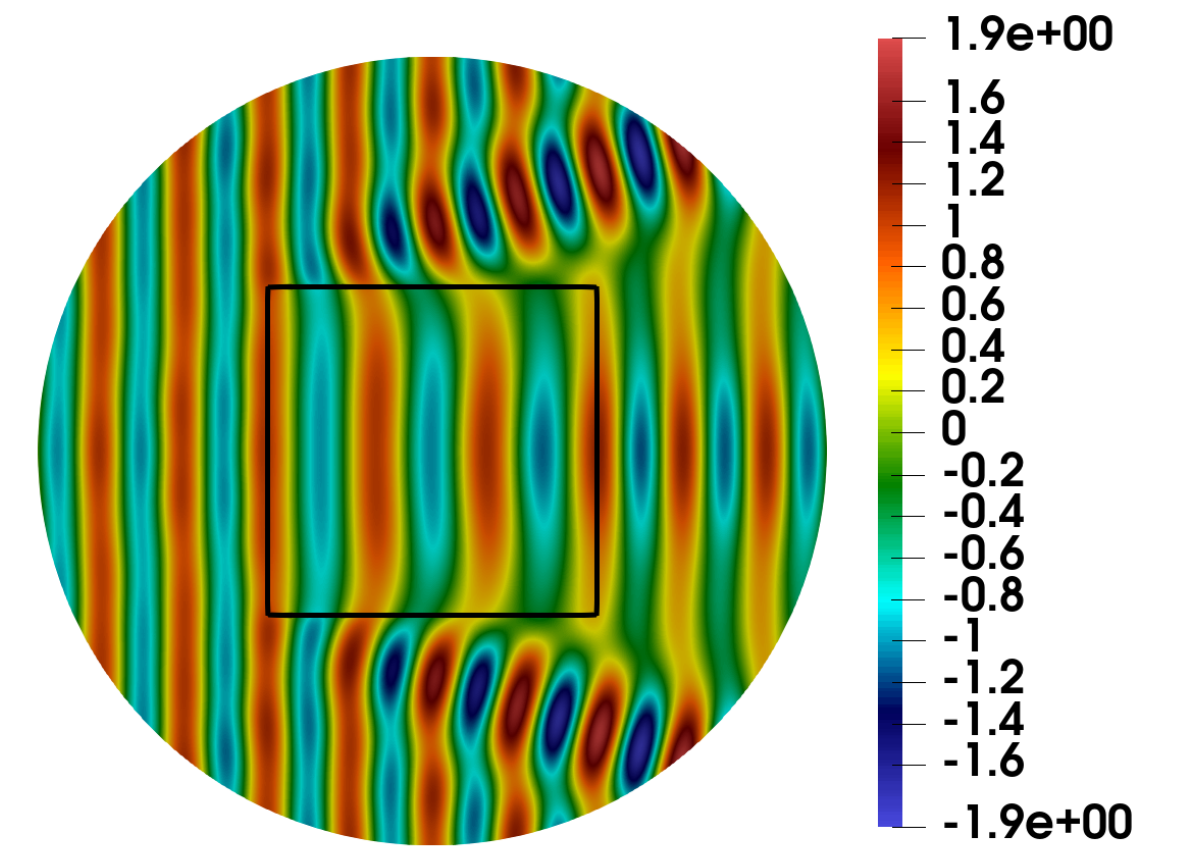
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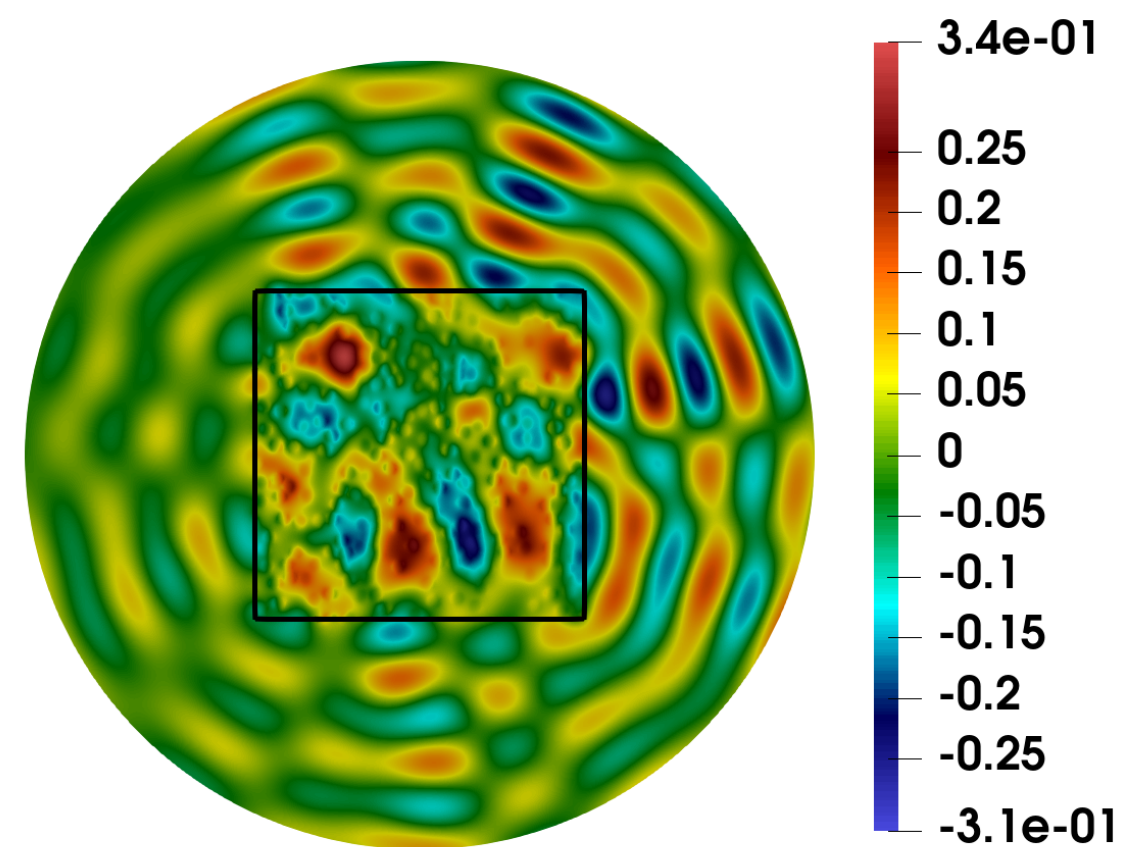
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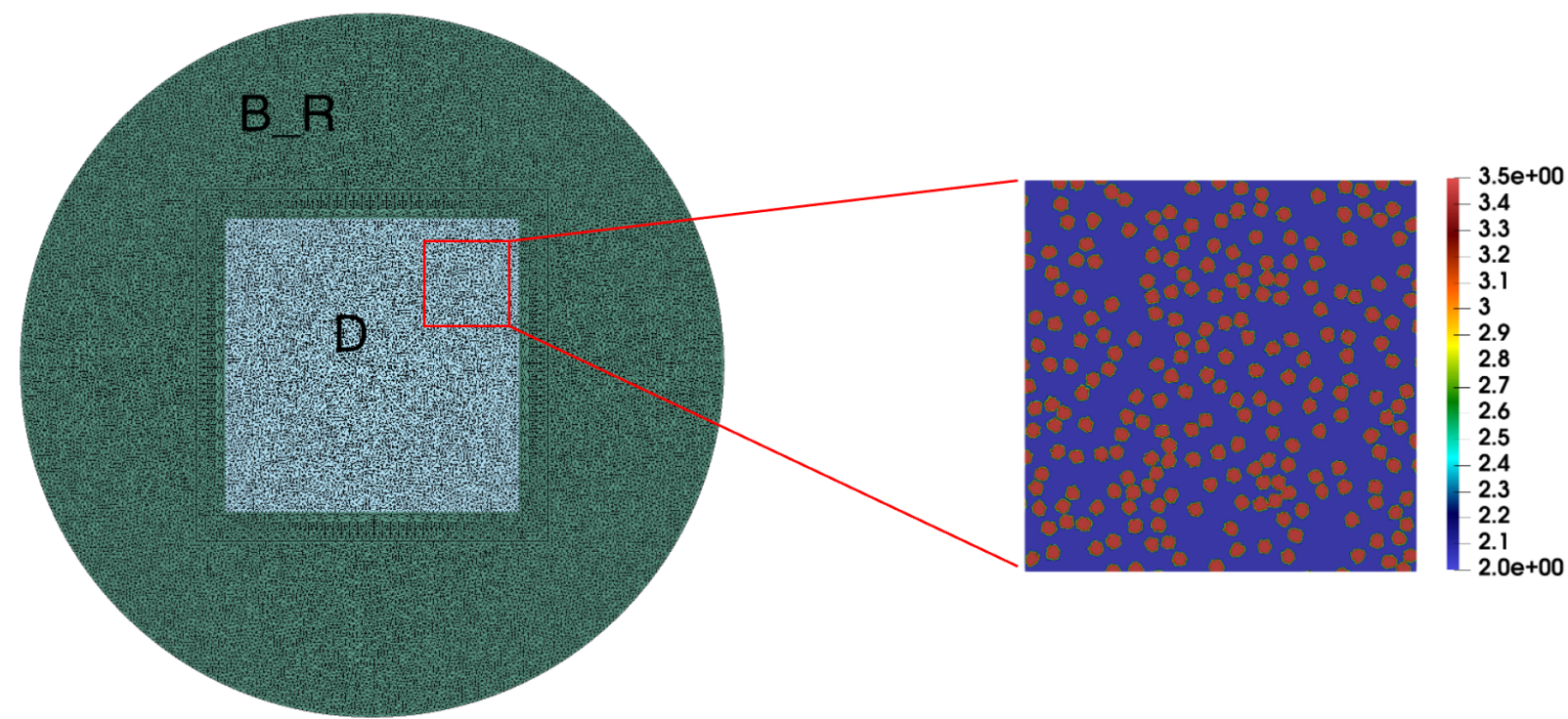


« Incoherent » field $u^\varepsilon - u_0$

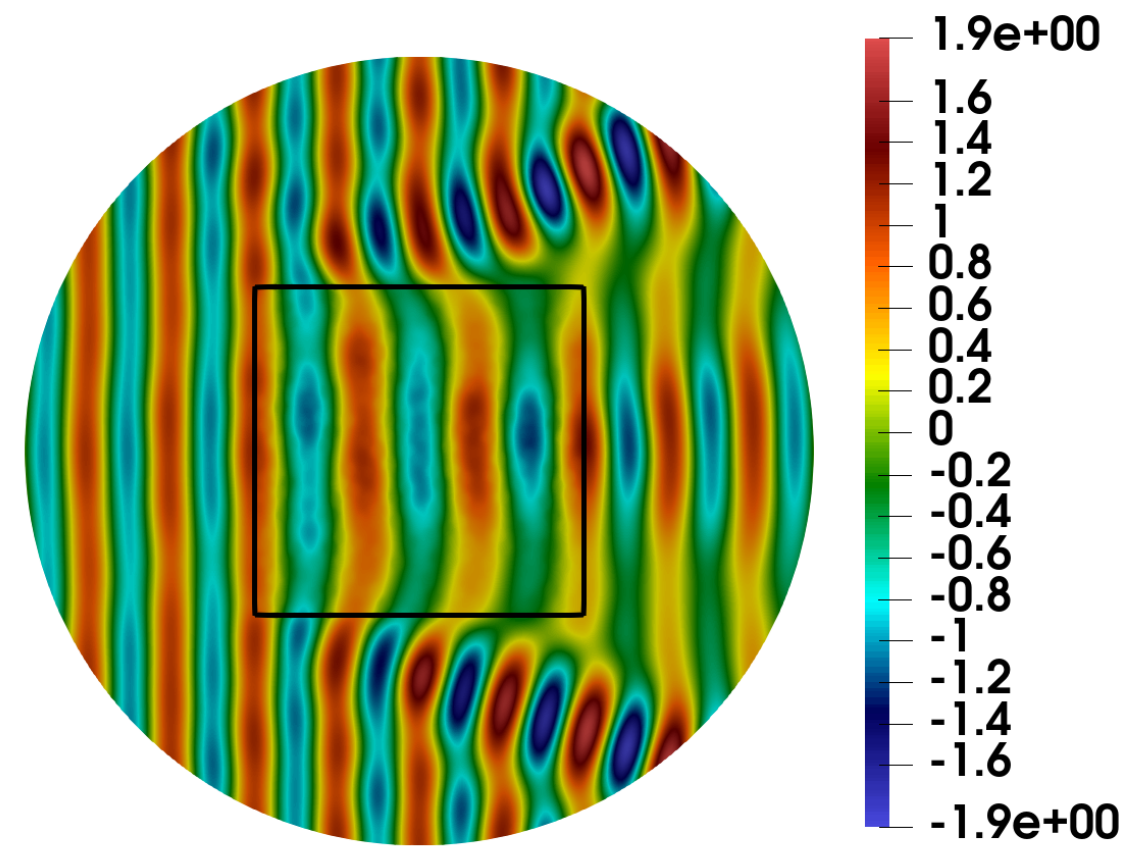


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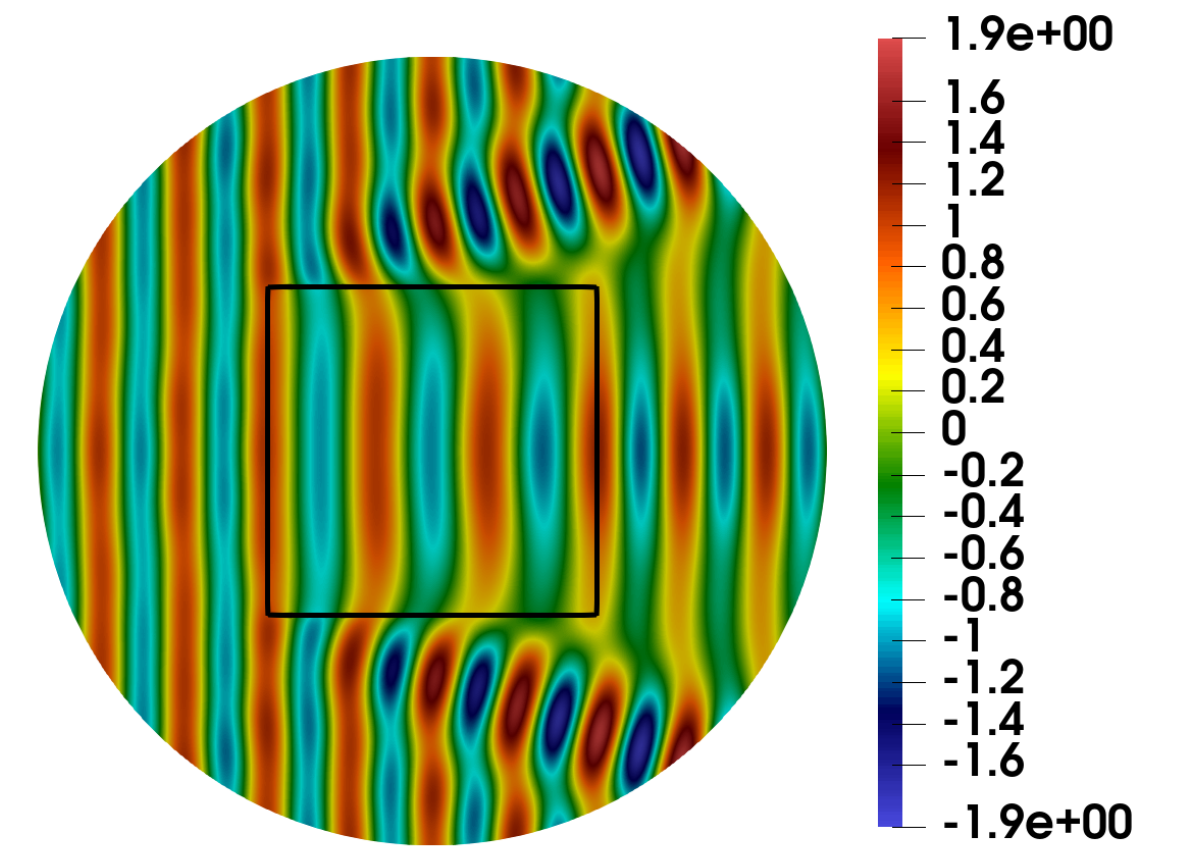
Example of domain



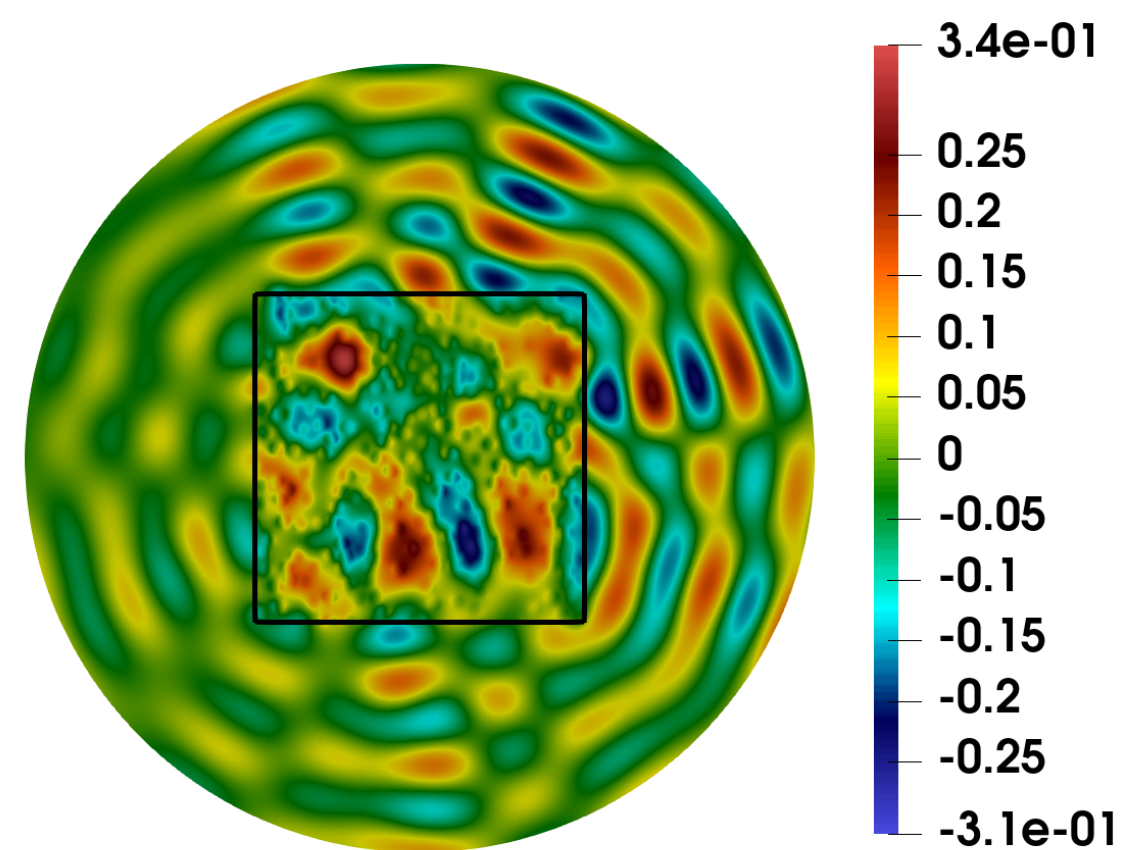
Total field u^ε



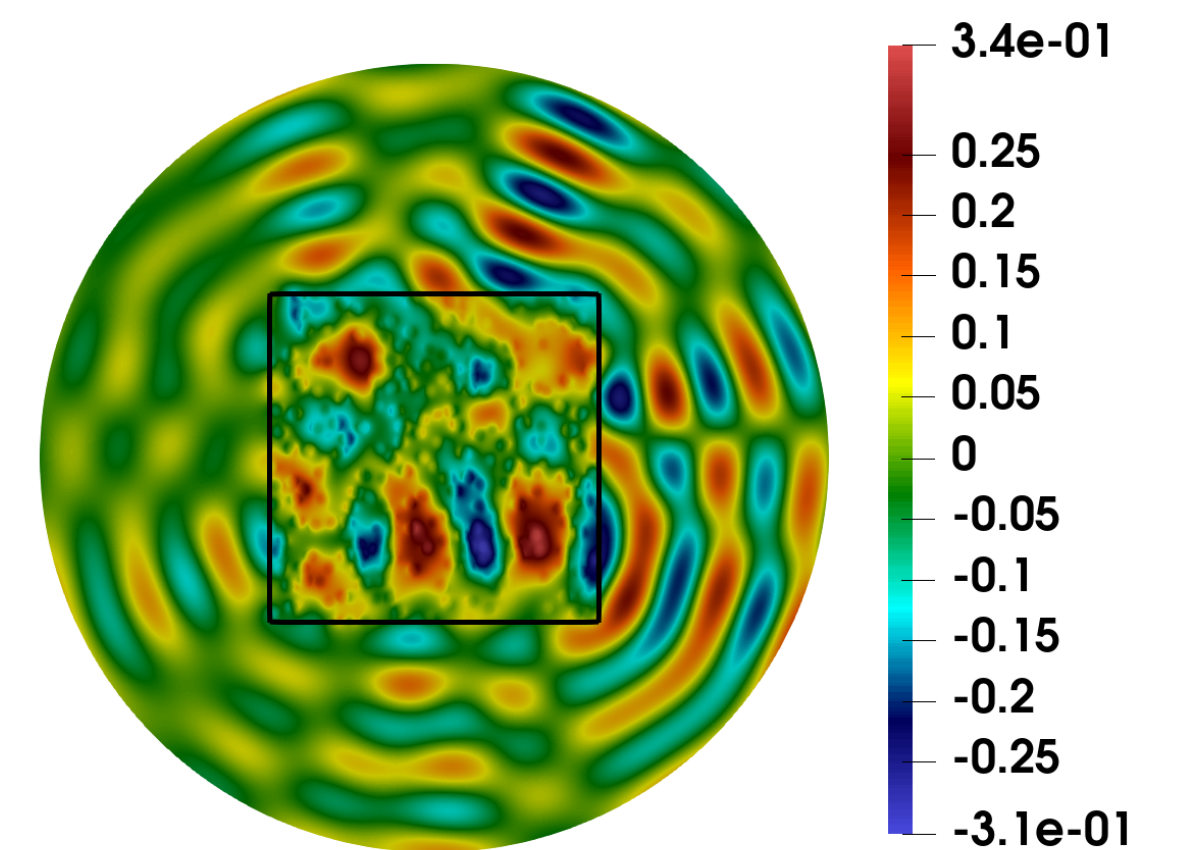
Coherent field u_0



« Incoherent » field $u^\varepsilon - u_0$



$\mathcal{U}^s$ (First order approximation)



Conclusion of part 1

It is possible to derive effective properties for the ultrasound propagation from the statistical properties of the micro-structure

It is possible to approximate the backscattered field as a function of the micro-structure and the coherent field

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1.3. Homogenization & Representation Of The Scattered Field

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2.2. The Focal Spot

2.3. Sound Speed Estimators

2.4. Focusing in the speckle

Simple model

Governing equation

$$\begin{cases} \Delta u + \frac{\omega^2}{(c^\star)^2} (1 + (n_\varepsilon - 1) \mathbb{1}_D) u = 0 \\ \lim_{|x| \rightarrow \infty} |x|^{\frac{d-1}{2}} \left(\partial_{|x|} (u - u^i) - i \frac{\omega}{c^\star} (u - u^i) \right) = 0. \end{cases}$$

Another simplification for the medium:

Simple model

Governing equation

$$\begin{cases} \Delta u + \frac{\omega^2}{(c^\star)^2} (1 + (n_\varepsilon - 1) \mathbb{1}_D) u = 0 \\ \lim_{|x| \rightarrow \infty} |x|^{\frac{d-1}{2}} \left(\partial_{|x|} (u - u^i) - i \frac{\omega}{c^\star} (u - u^i) \right) = 0. \end{cases}$$

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$$n_\varepsilon(x) = 1 + \tilde{n} \left(\frac{x}{\varepsilon} \right) \text{ with } \mathbb{E} [\tilde{n}(x)] = 0,$$

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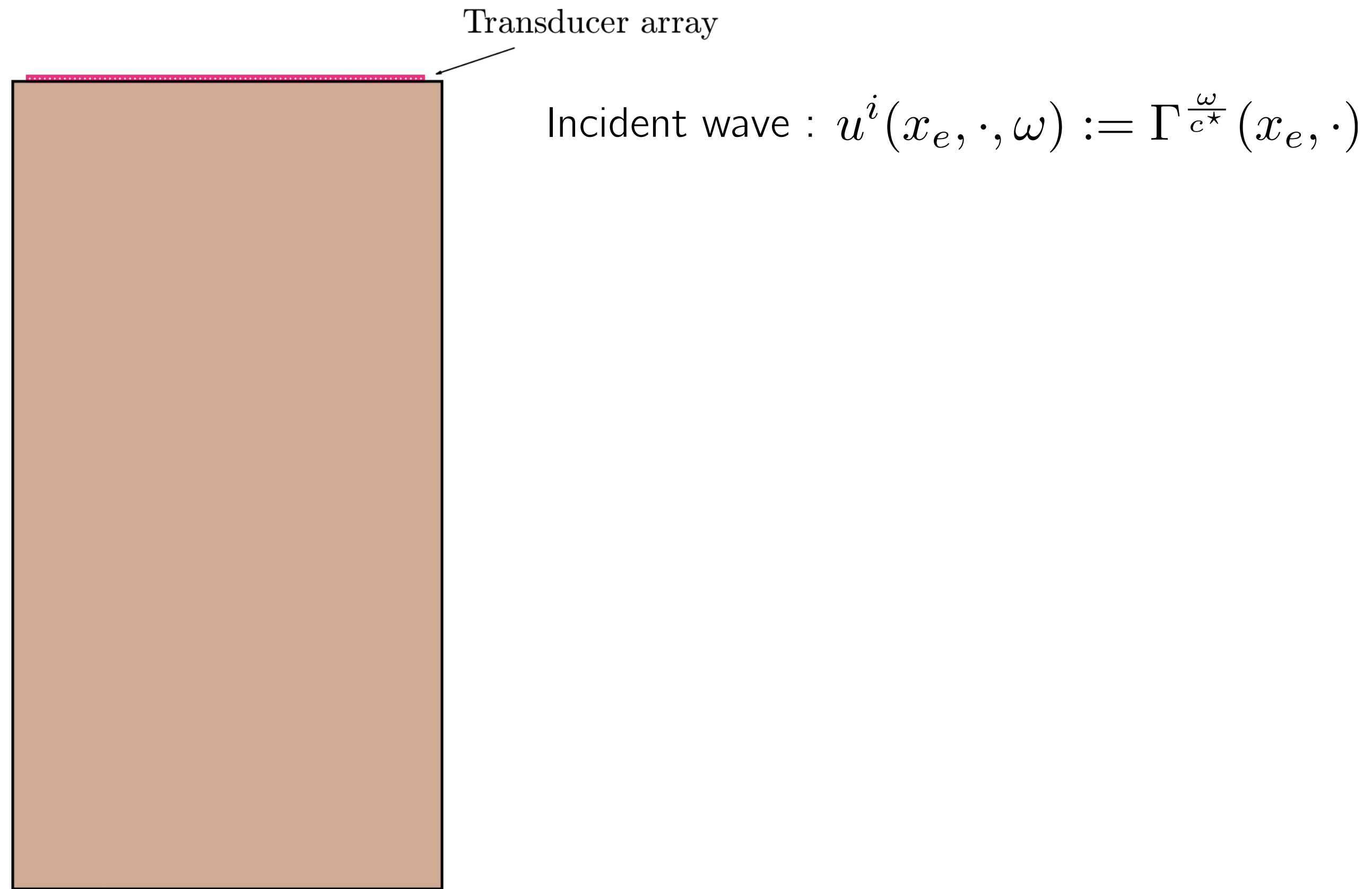
$$n_\varepsilon(x) = 1 + \tilde{n} \left(\frac{x}{\varepsilon} \right) \text{ with } \mathbb{E} [\tilde{n}(x)] = 0,$$

« non-restrictive », just technical simplification to get :

Match between homogenized and outer medium

$$G^\star(\cdot, z) = \Gamma_{\frac{\omega}{c^\star}}(\cdot, z) \text{ and } u^i = u_0.$$

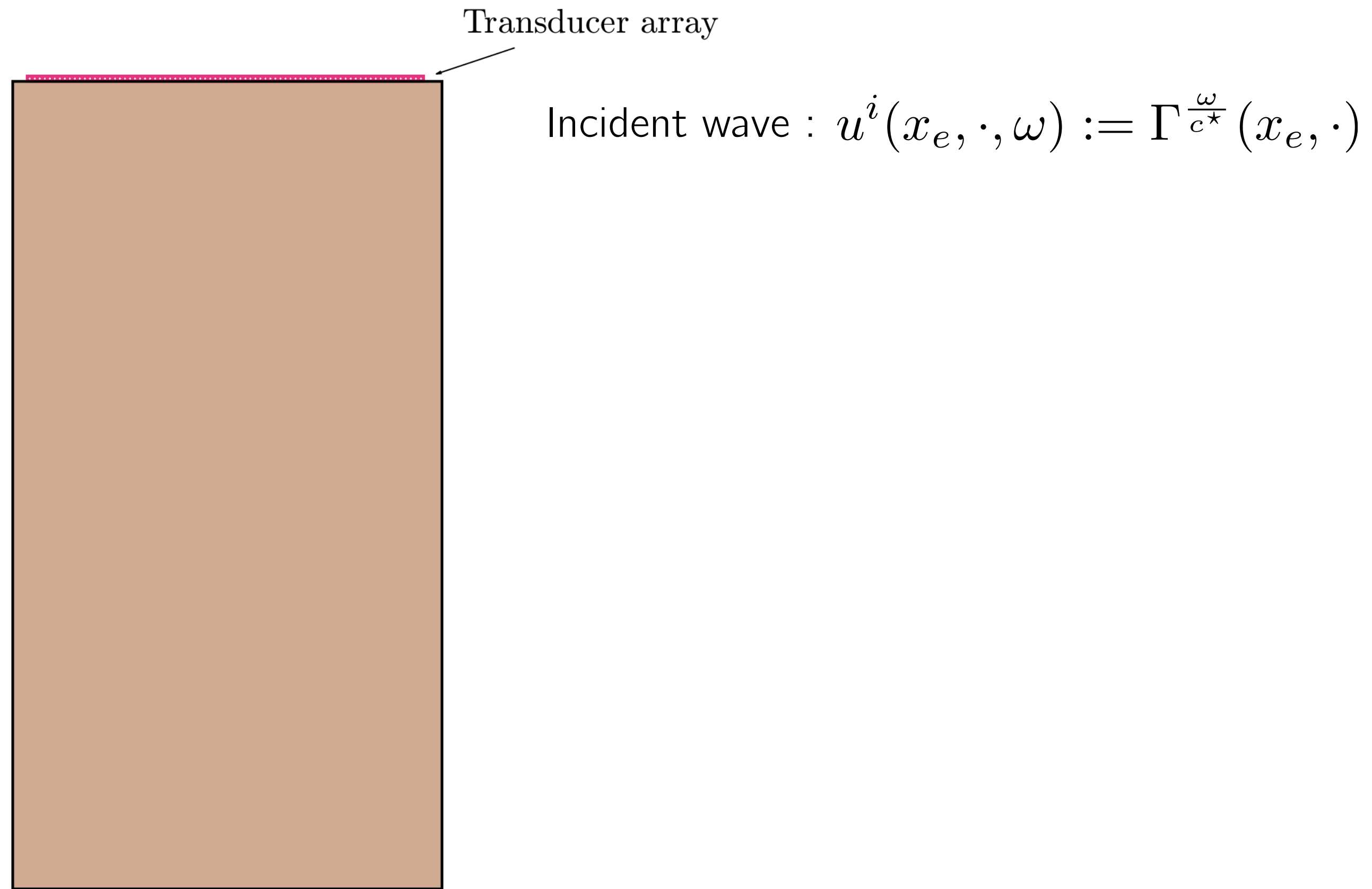
Measurement matrix and imaging functional



Simulation of US experiment

Physical domain D

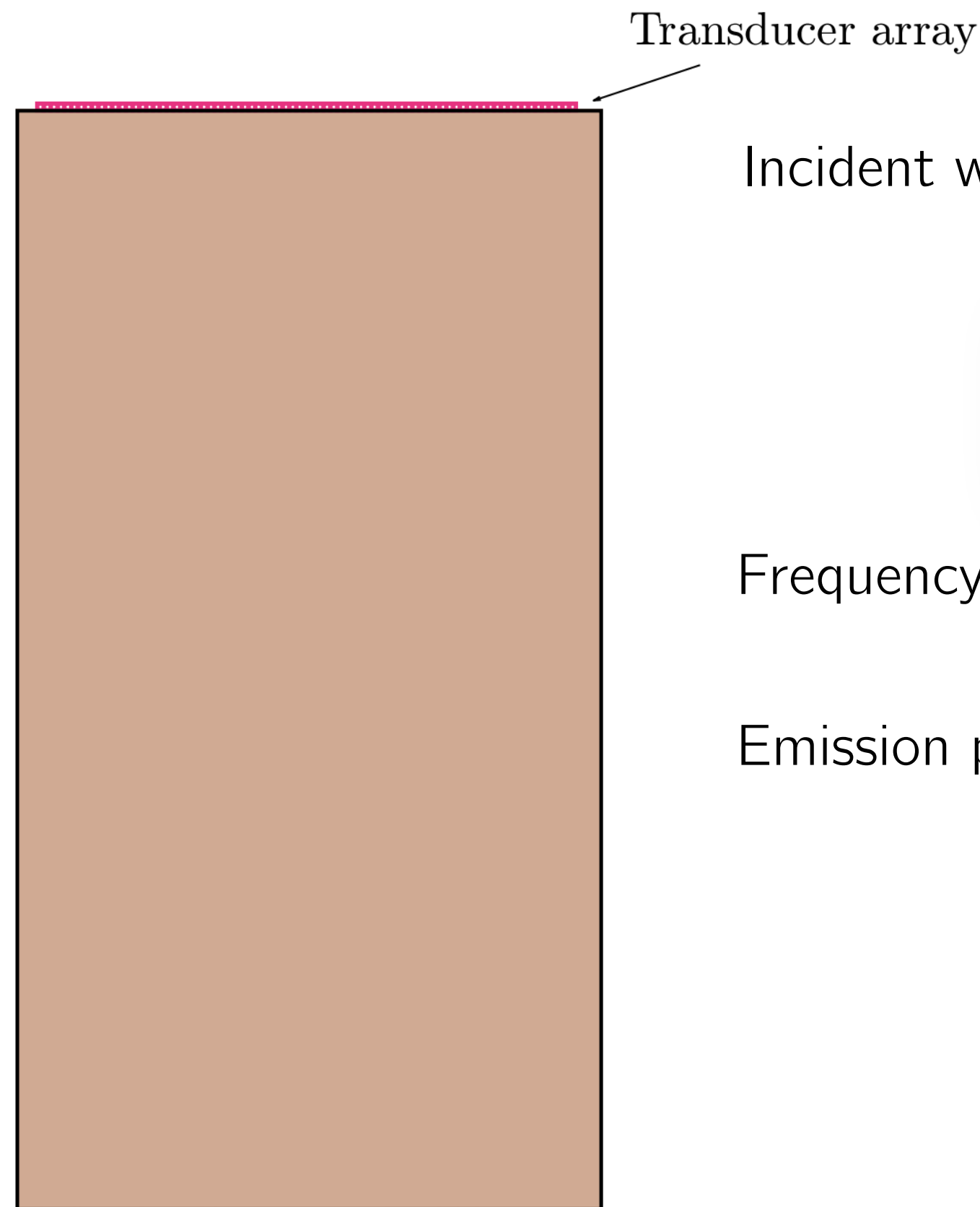
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Simulation of US experiment

Physical domain D

Measurement matrix and imaging functional



Incident wave : $u^i(x_e, \cdot, \omega) := \Gamma^{\frac{\omega}{c^*}}(x_e, \cdot)$

Measurement matrix: $M_{e,r}(\omega) := u^s(x_e, x_r, \omega)$

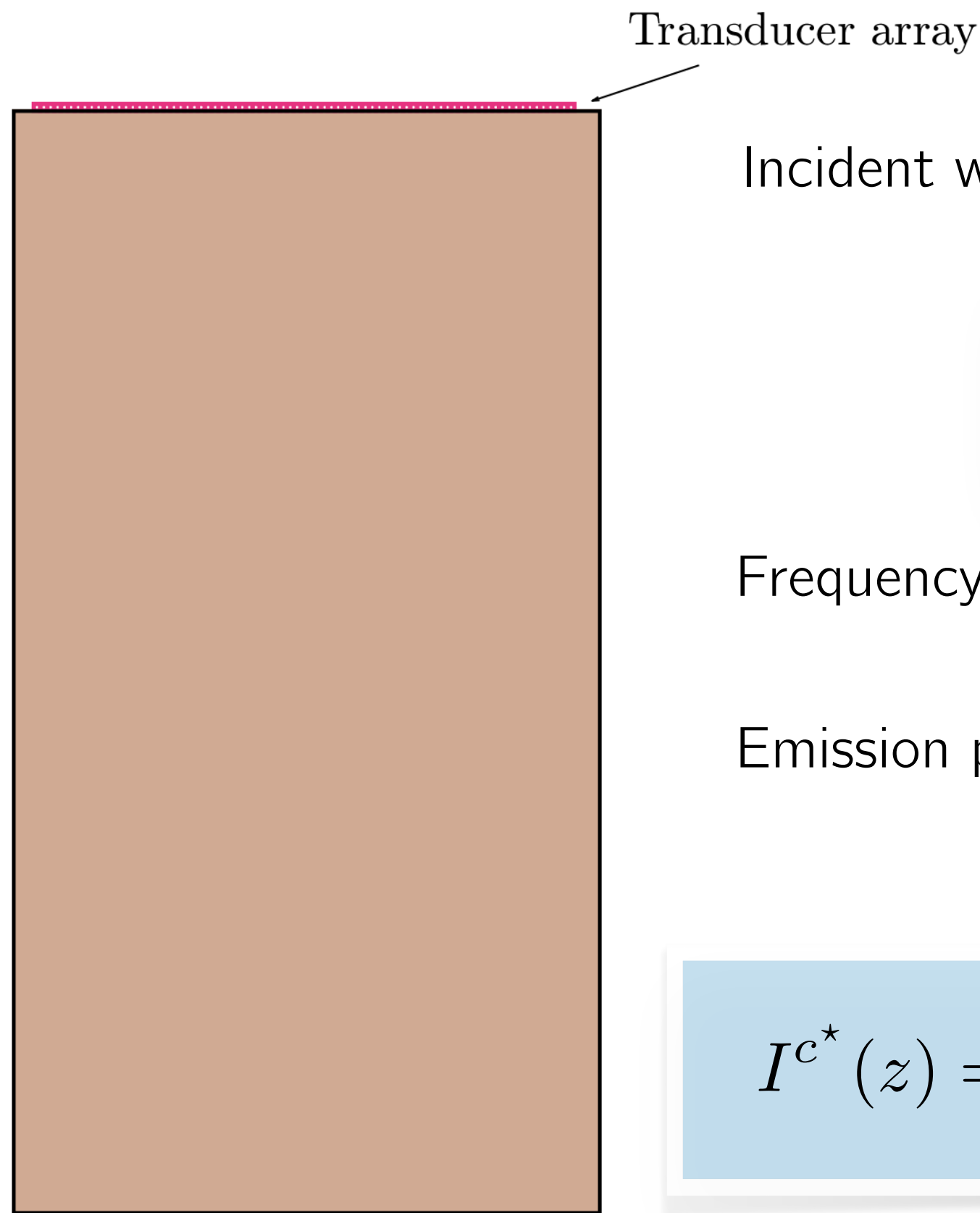
Frequency $\omega \in \mathcal{B}$ (bandwidth). Effective speed of sound c^* . Probe $\mathcal{P} = [-\frac{a}{2}, \frac{a}{2}] \times 0$,

Emission point $x_e \in \mathcal{P}$, reception point $x_r \in \mathcal{P}$.

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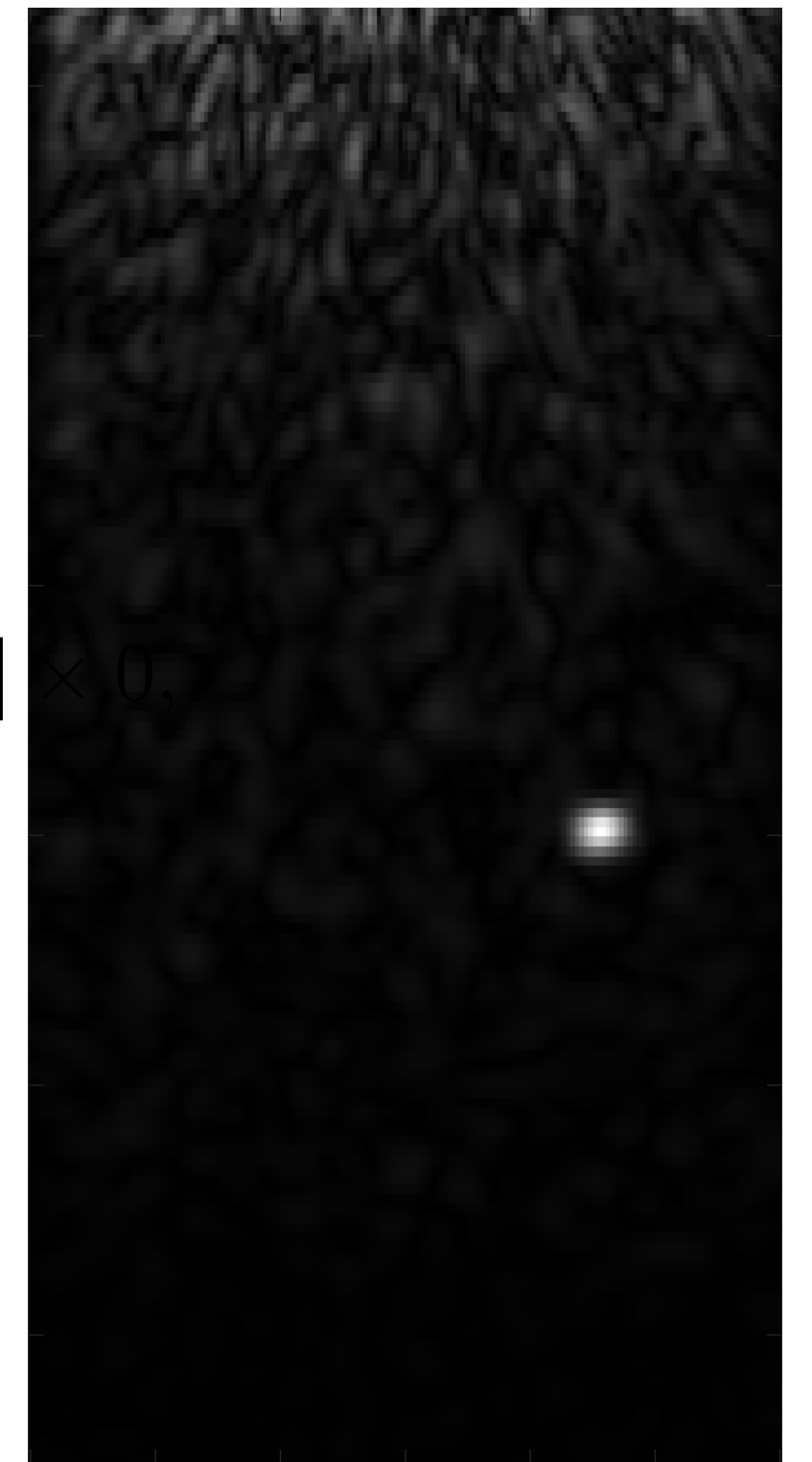
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Imaging functional

$$I^{c^*}(z) = \int_{\mathcal{A} \times \mathcal{A} \times \mathcal{B}} \overline{u^s(x_e, x_r, \omega)} \Gamma^{\frac{\omega}{c^*}}(x_e, z) \Gamma^{\frac{\omega}{c^*}}(x_r, z) dx_e dx_r d\omega$$



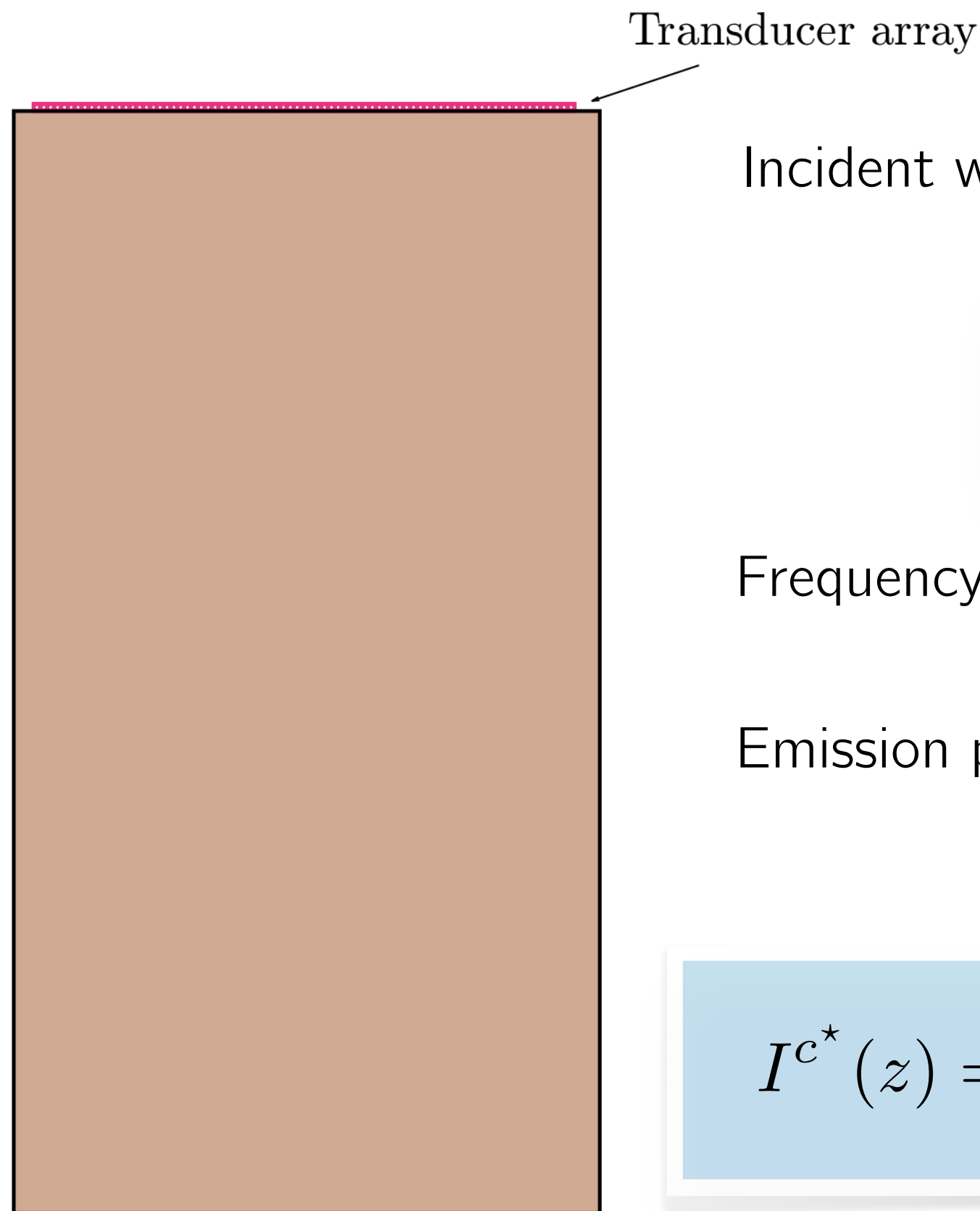
Simulation of US experiment

Physical domain D

Computed Image

Imaging domain D'

Measurement matrix and imaging functional



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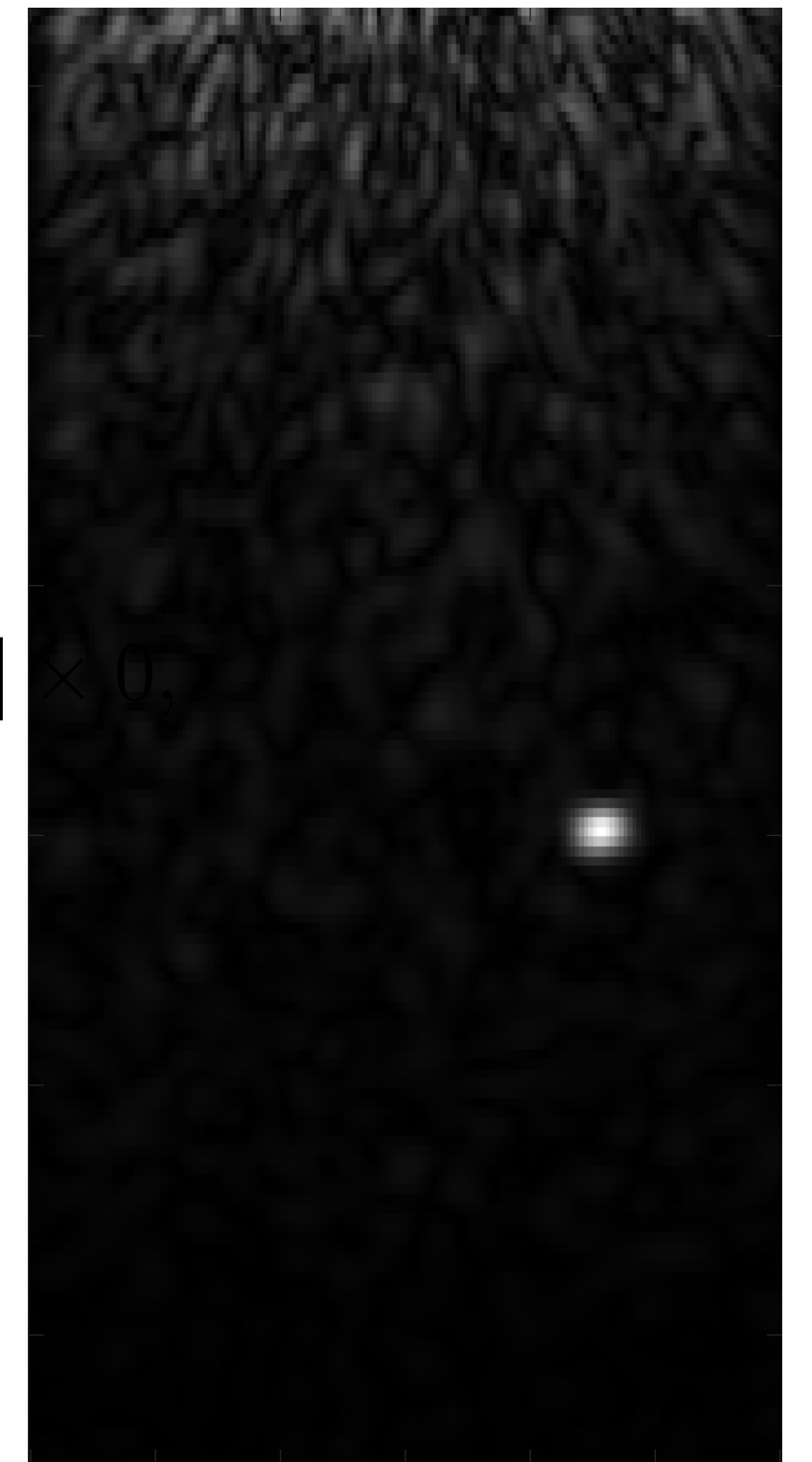
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Simulation of US experiment

Physical domain D

What if c^* is not known ?

Computed Image

Imaging domain D'

Characterization of the problem

Geometry

Active array of sources / sensor outside the medium

Reflection geometry

Large domain

Regime

Random fluctuations of the medium:
short correlation length & order 1 amplitude

Dense distribution of scatterers (no sparsity)

Goal

Find the effective speed of sound *in situ*
(geometrical component of the focusing law)

Constraints

Low computational cost

Prior

Stationarity and ergodicity of the fluctuations

The point-spread function (PSF)

First order approximation for the scattered fields

$$M(x_e, x_r, \omega) = \omega^2 \int_D (n(y) - n^*) G^*(x_r, y) G^*(x_e, y) dy$$

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Imaging functional as a convolution

$$I^*(z) = \int_D (n(y) - n^*) F^{c^*}(z, y) dy, \quad z \in D'$$

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Kernel of the operator (Point Spread Function)

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The case $c \neq c^\star$

First order approximation for the scattered fields

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(Unchanged)

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Effects of speed of sound error on the focal spot

$$\begin{aligned} D' &\longrightarrow D' \\ z &\longmapsto \left| F^{\frac{c}{c^*}}(z, y_0) \right| \end{aligned}$$

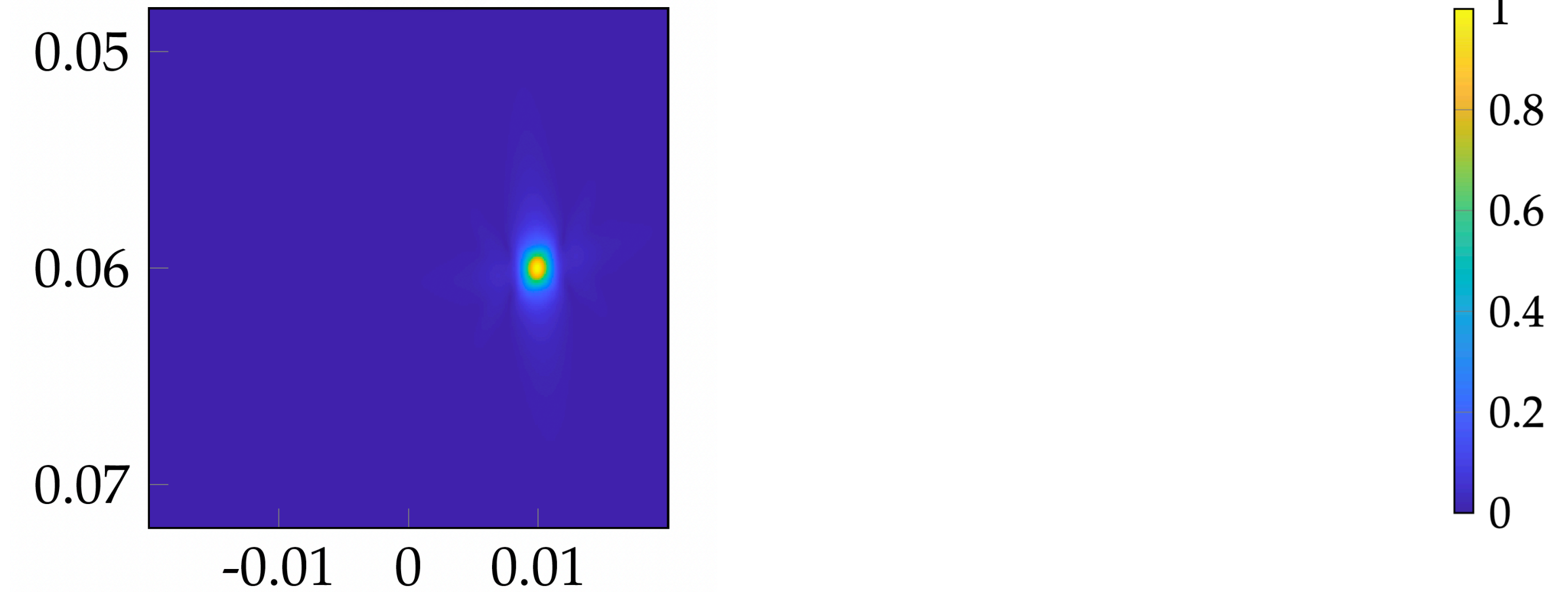
$$y_0 = (0.01, 0.06) \in D$$

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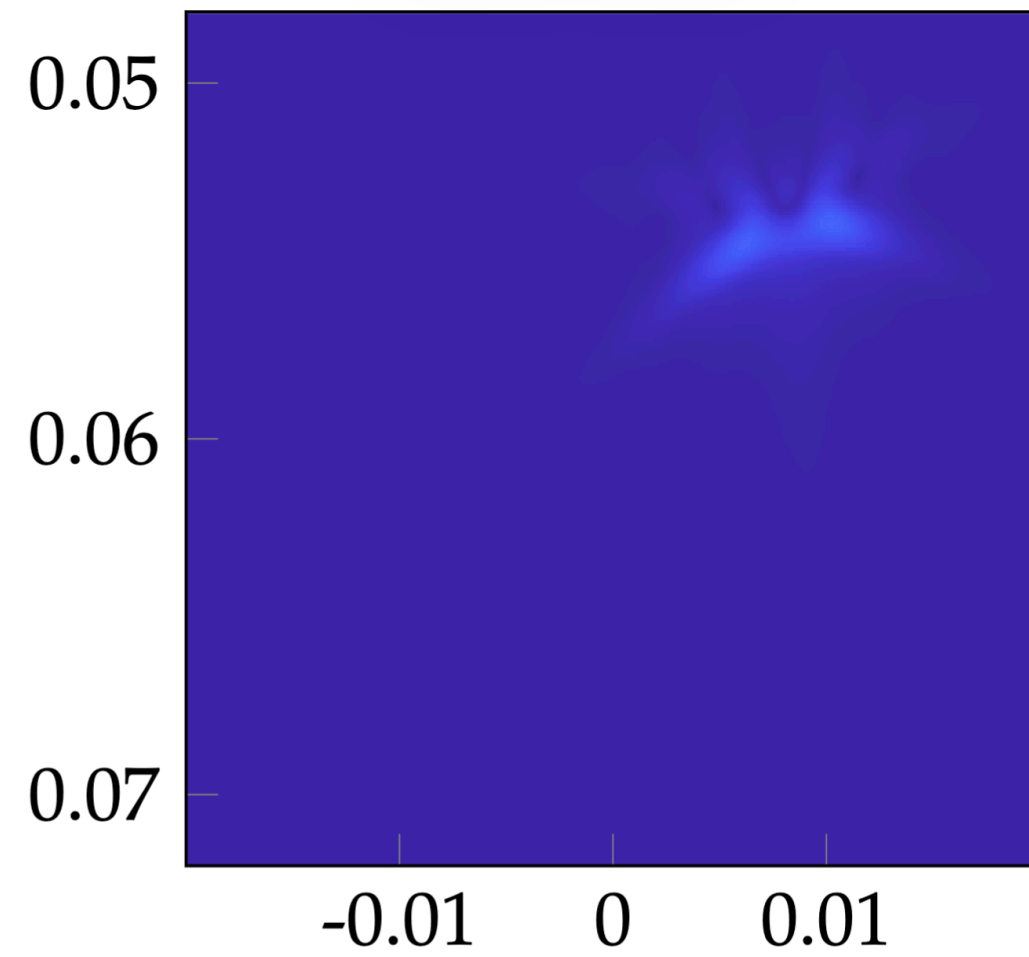


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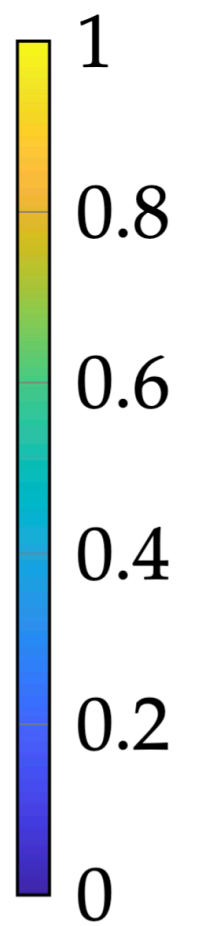
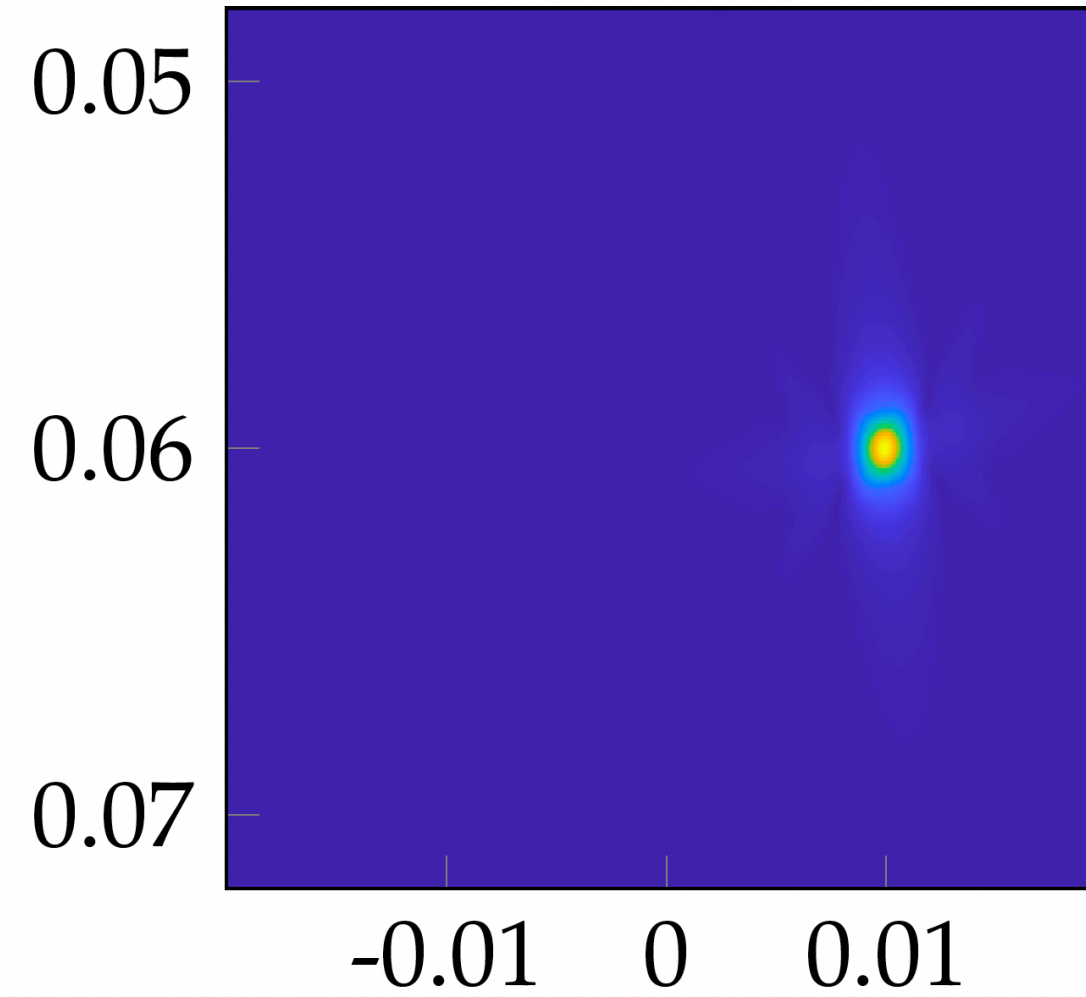
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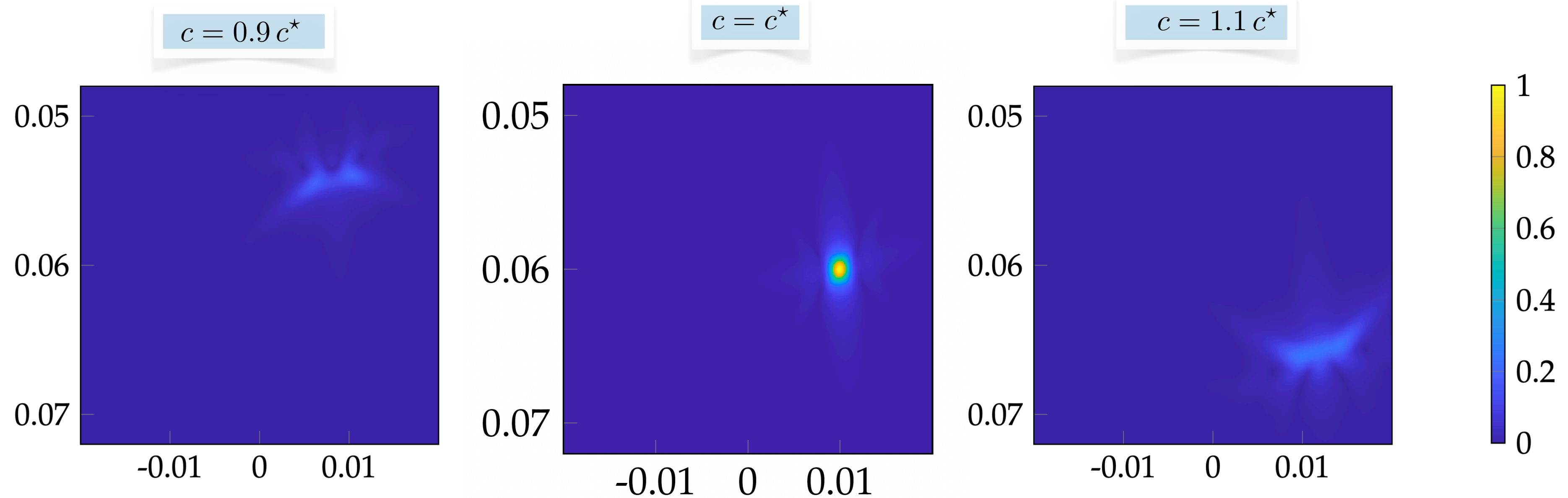
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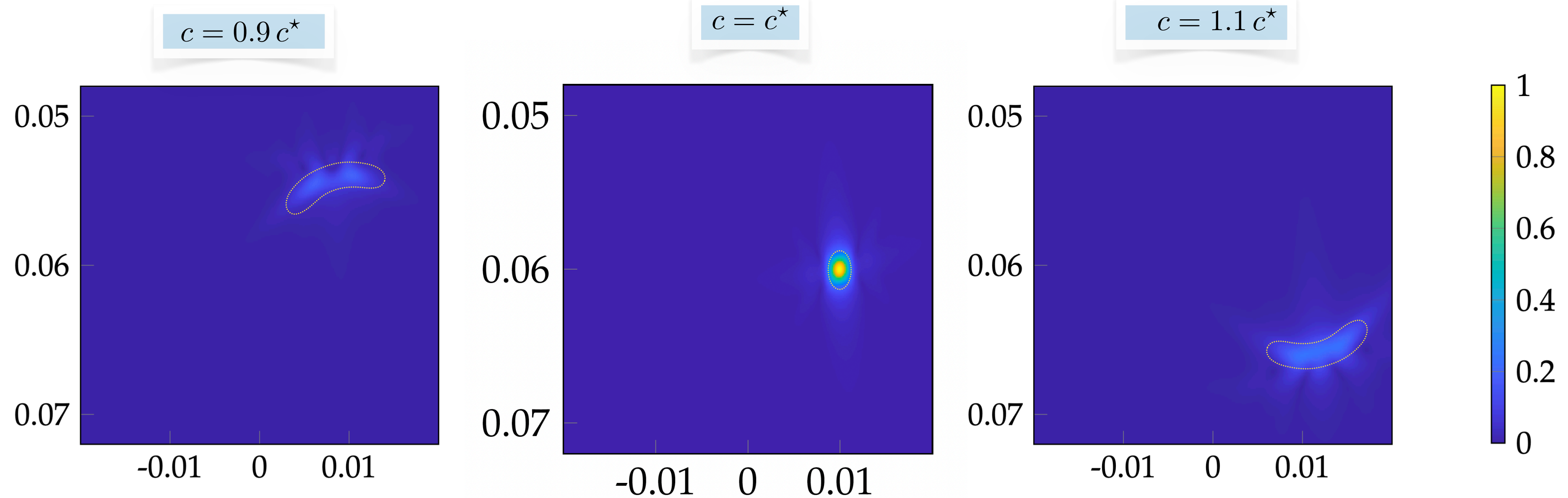
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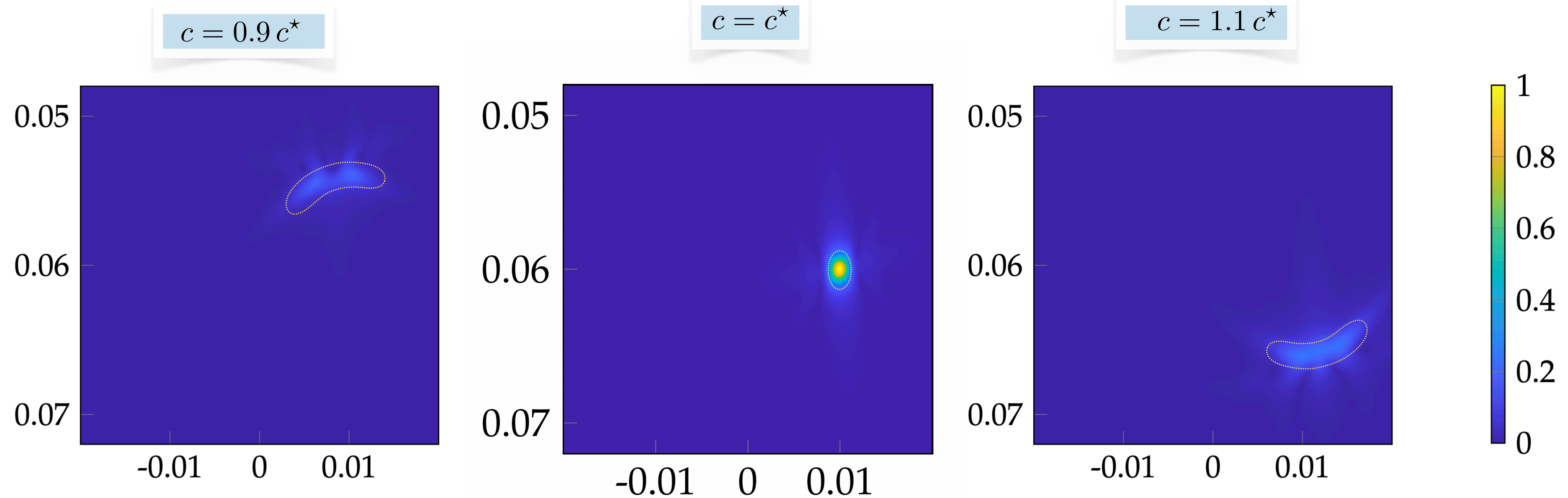
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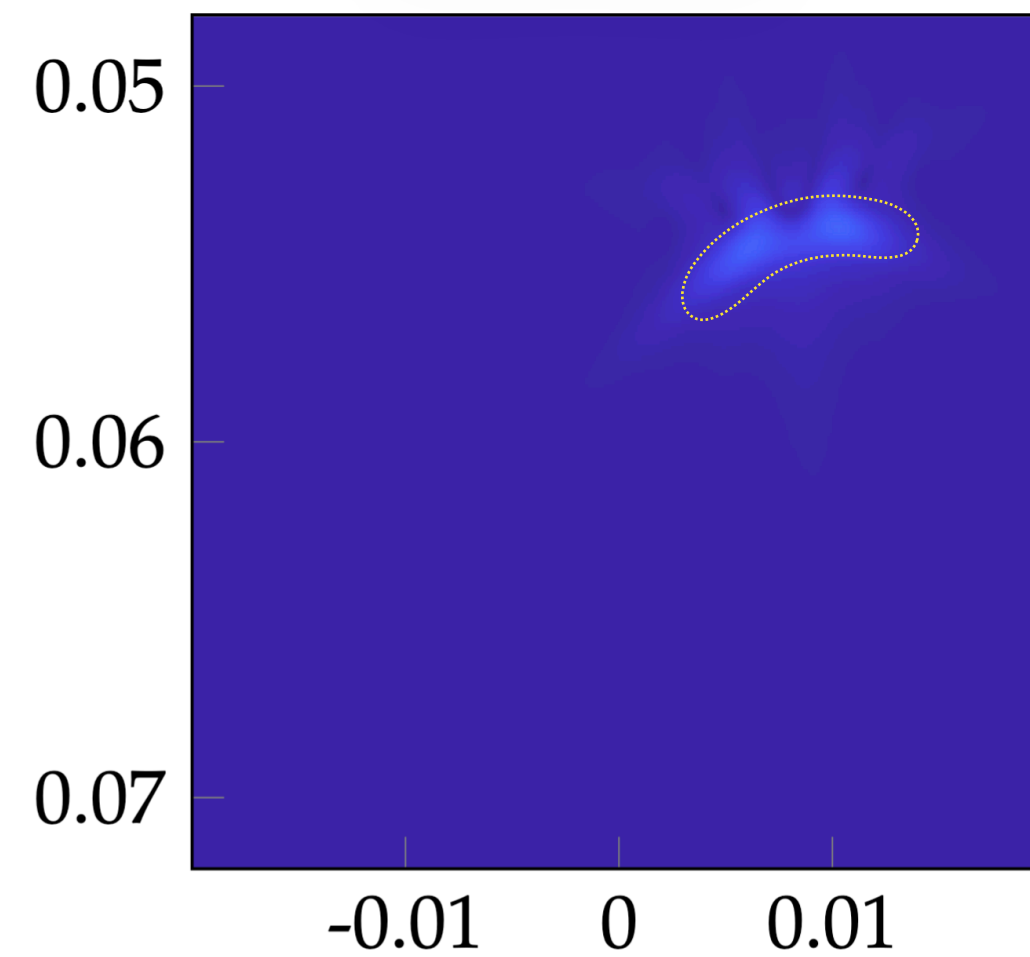
Localisation is moved

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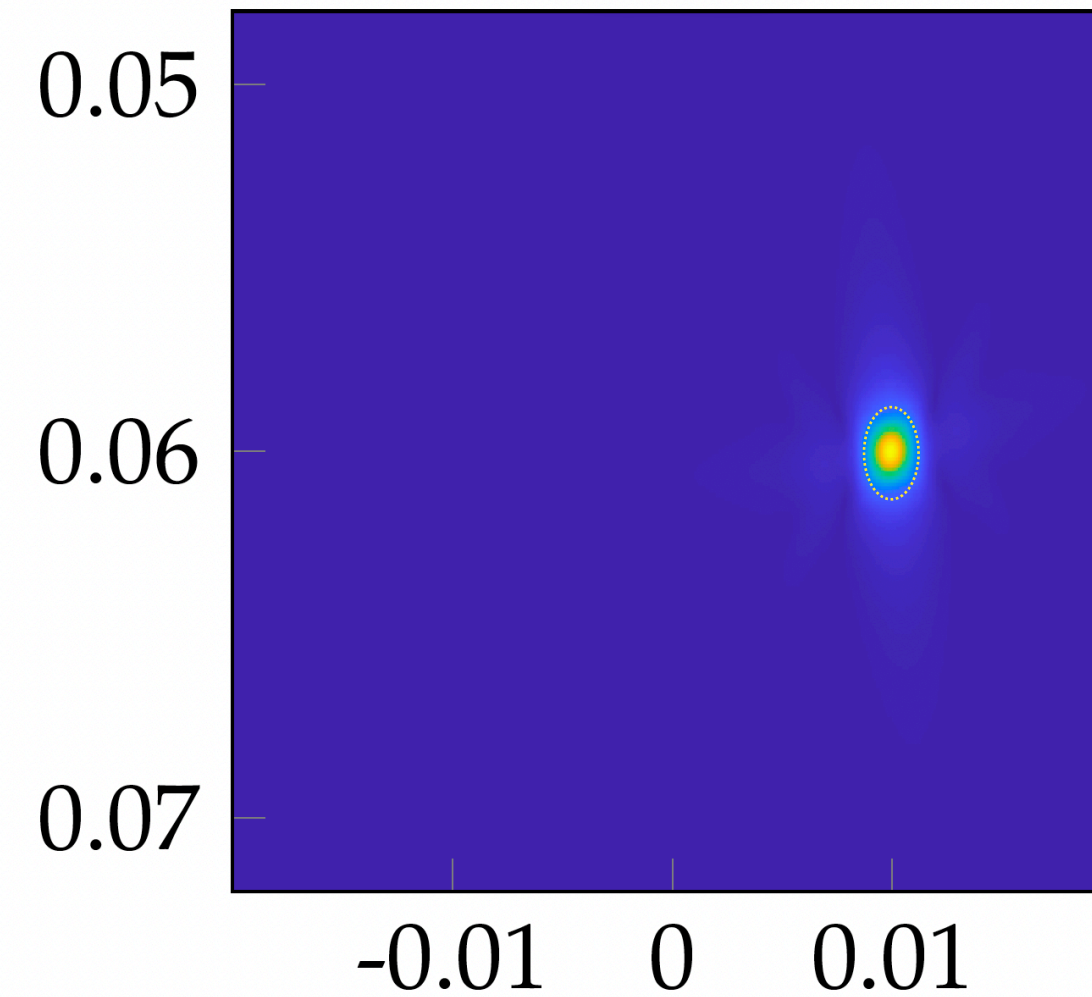
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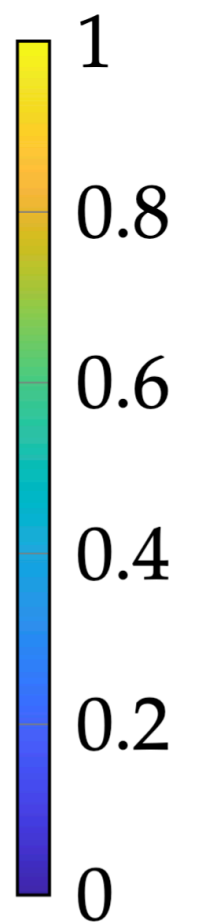
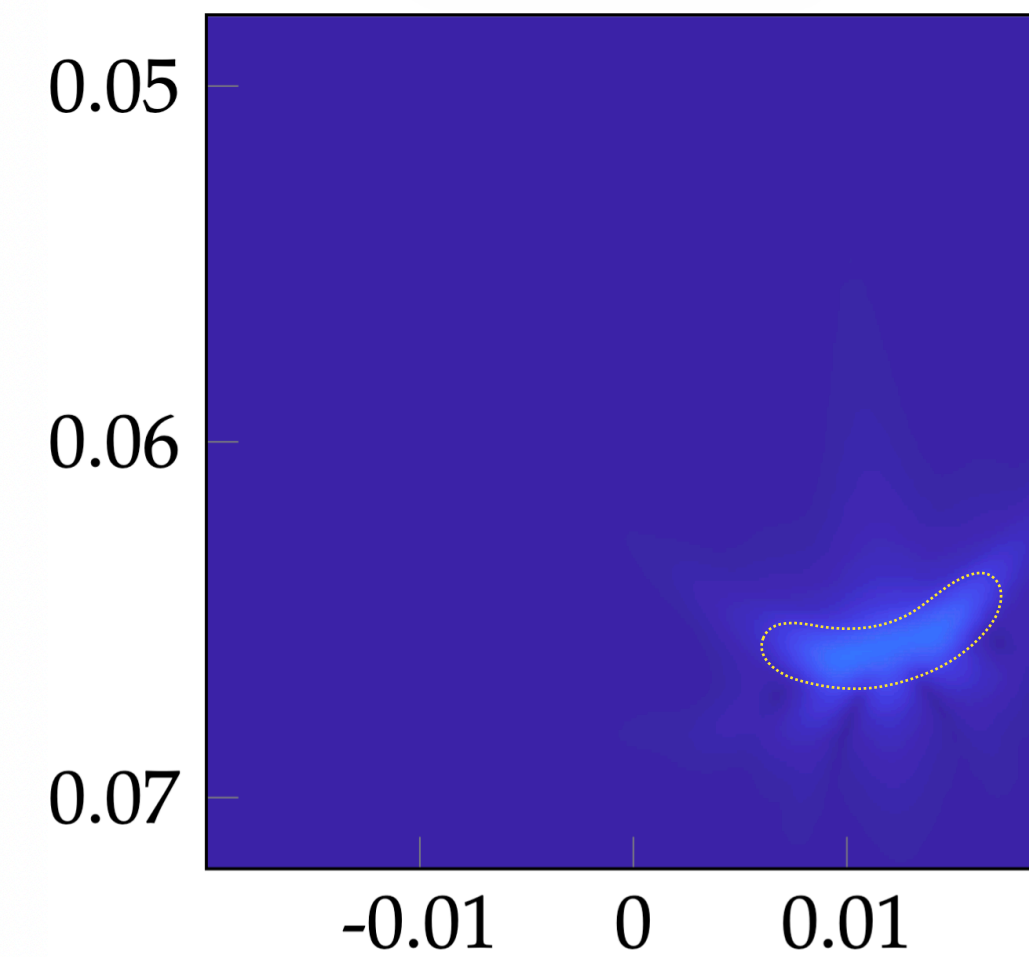
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$$c = c^*$$



Height of peak decreased

$$c = 1.1 c^*$$

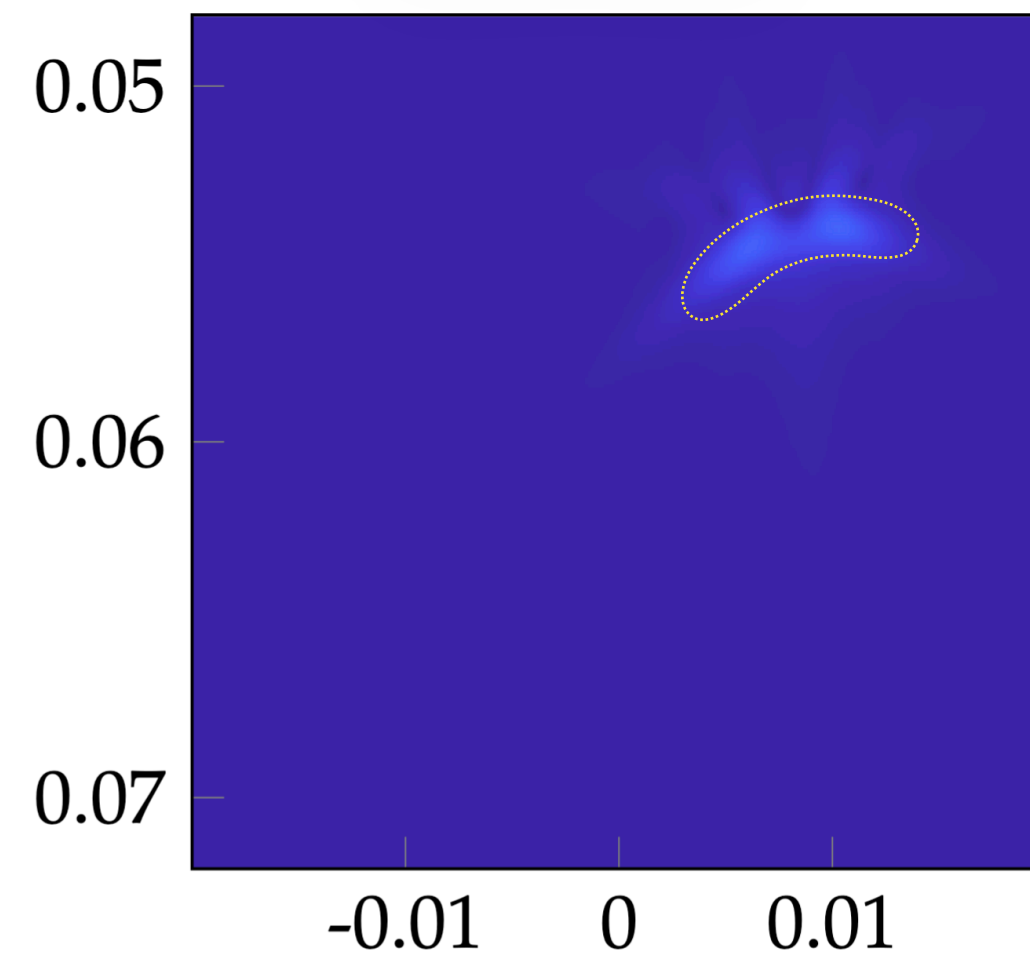


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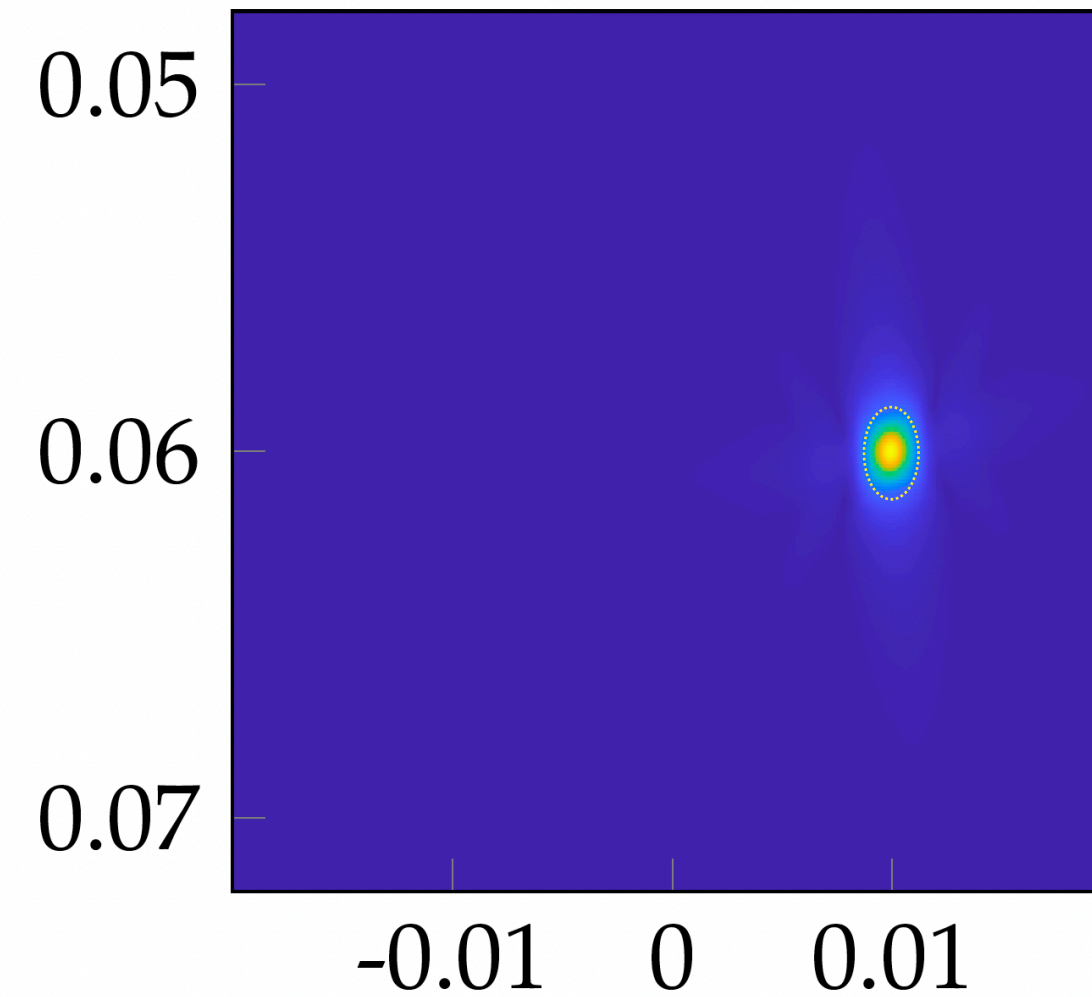
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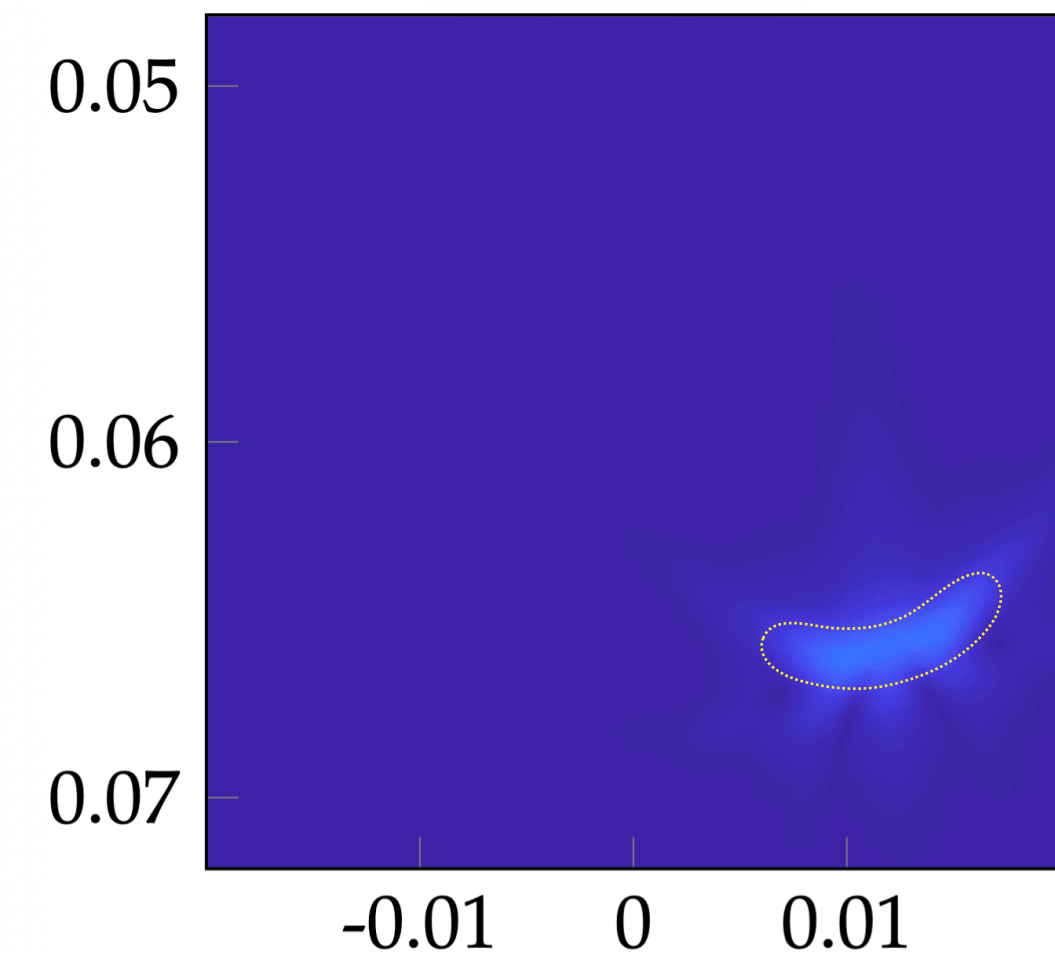
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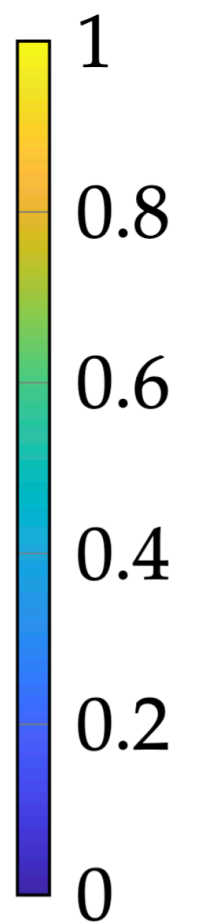


Height of peak decreased

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Size is increased

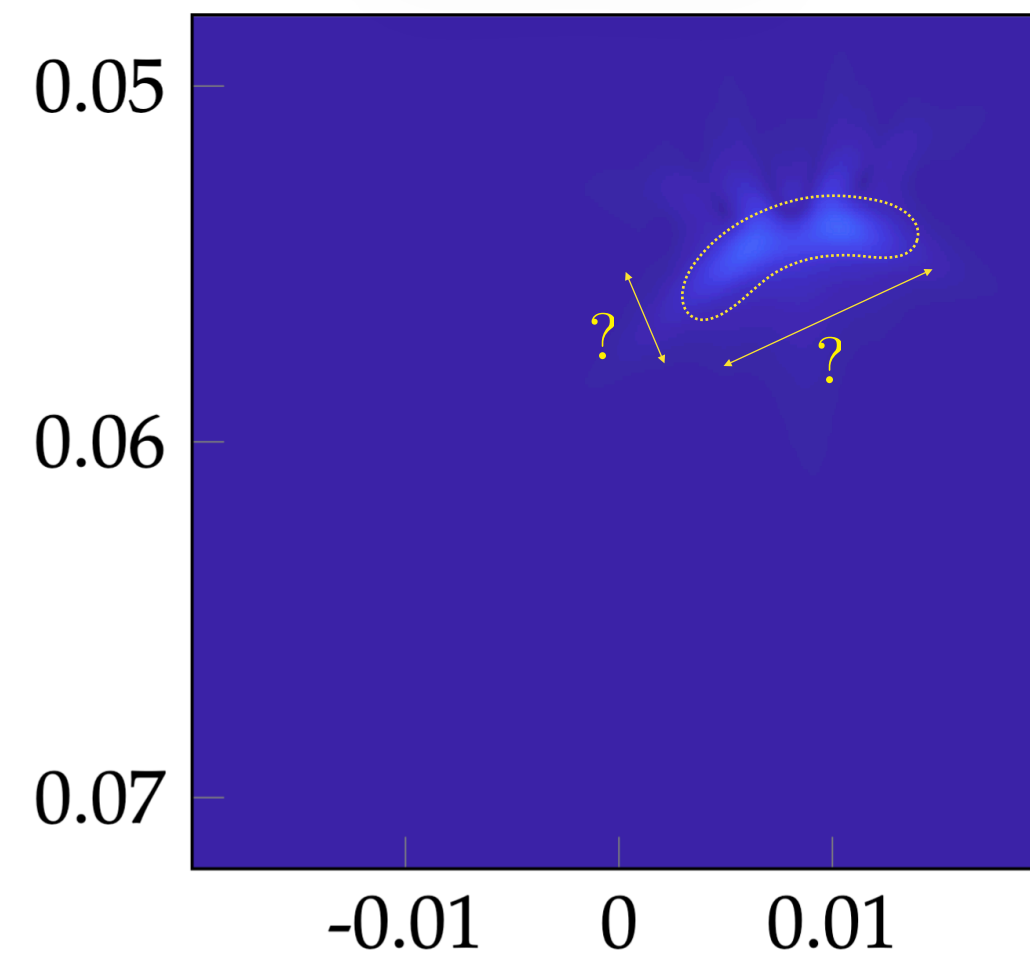


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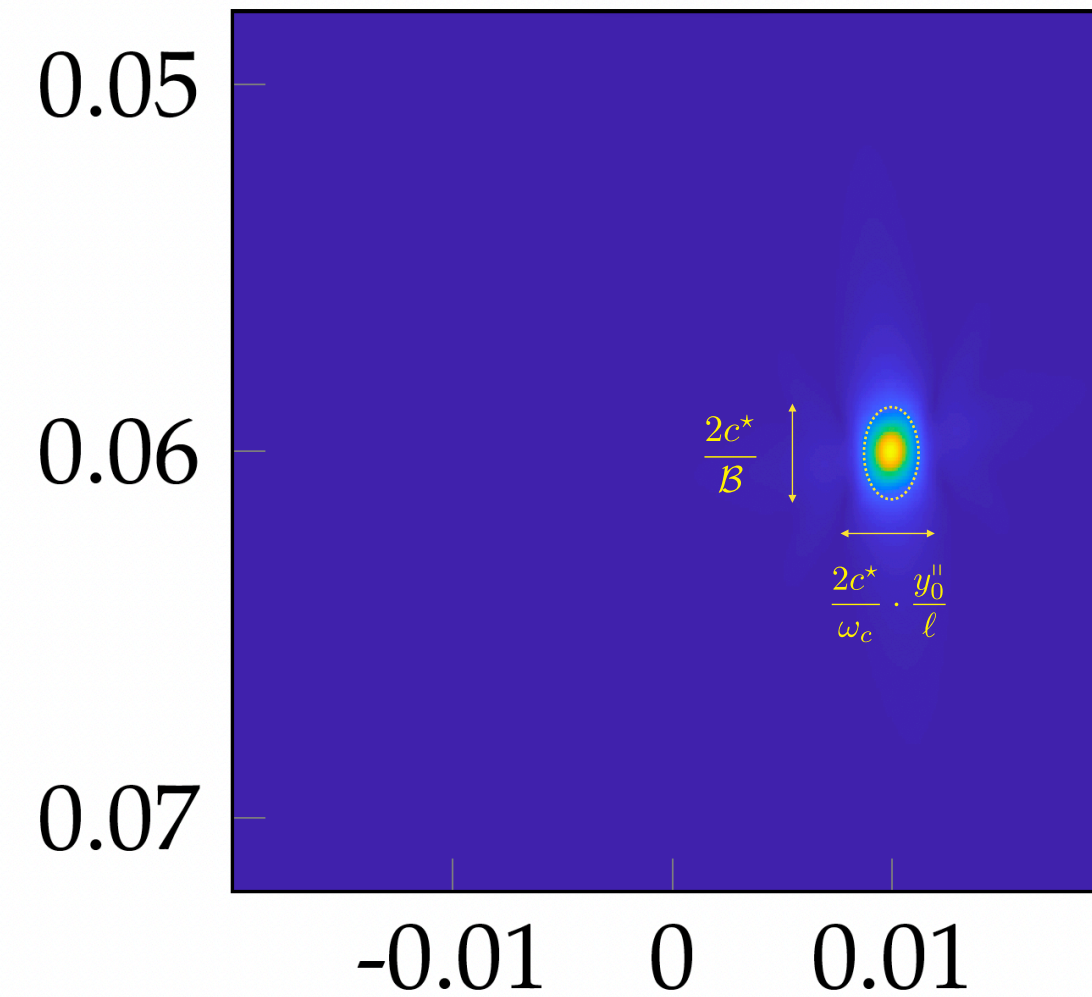
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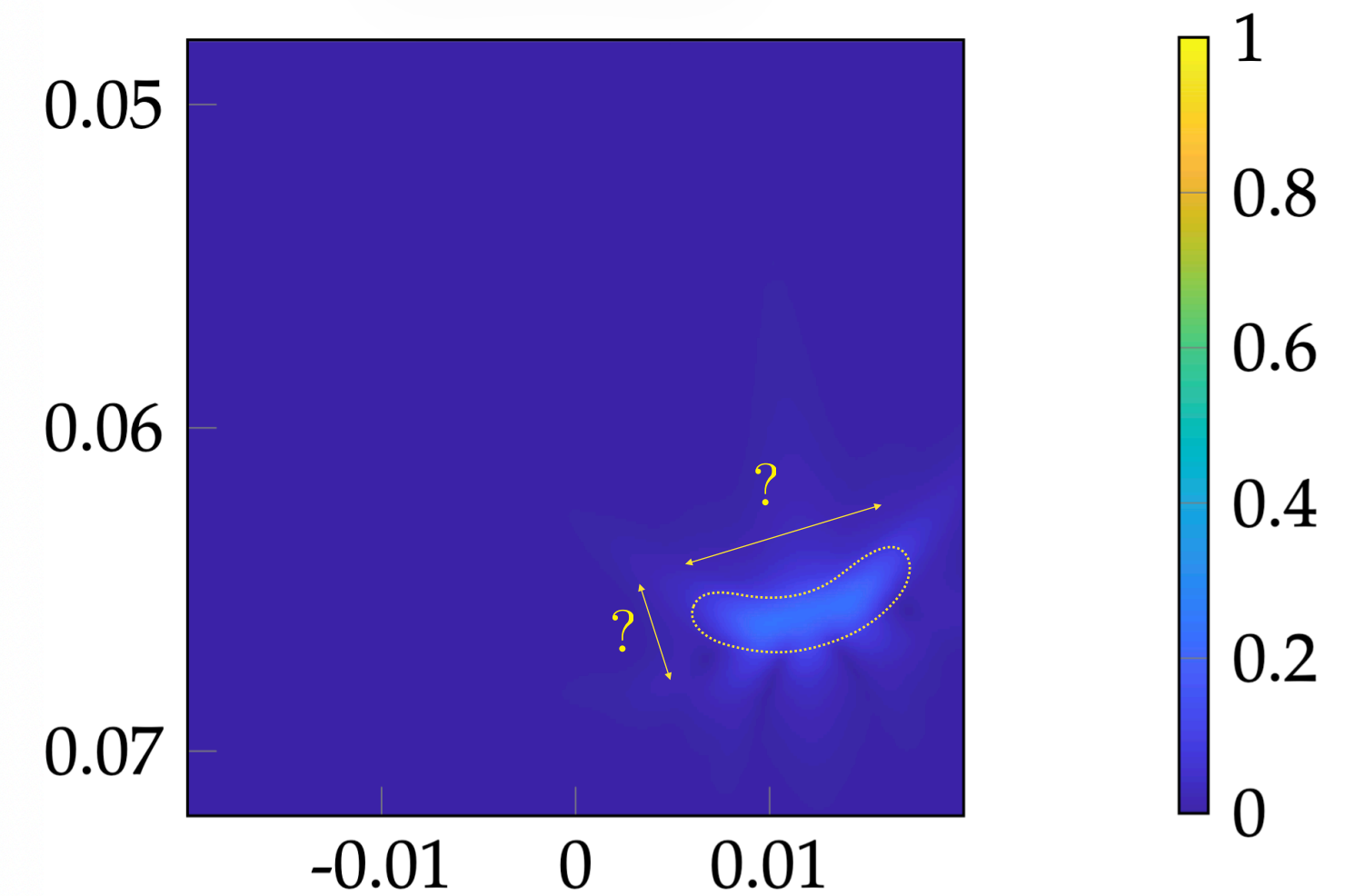
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Size is increased

Quantification of these effects ?

The focal spot

Definition : Focal spot at threshold δ

Consider $0 < \delta \ll 1$ and $y_0 \in D$. There exists a domain $D'_\delta(y_0) \subset D'$ such that

$$\int_{D' \setminus \overline{D'_\delta(y_0)}} \left| F^{c^*}(z, y_0) \right| dz < \delta \int_{D'} \left| F^{c^*}(z, y_0) \right| dz \quad \text{and} \quad \frac{|D'_\delta(y_0)|}{|D'|} \ll \delta.$$

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The function $z \mapsto |F^*(z, y_0)|$ is of order 1 in the focal spot and « very small » outside.

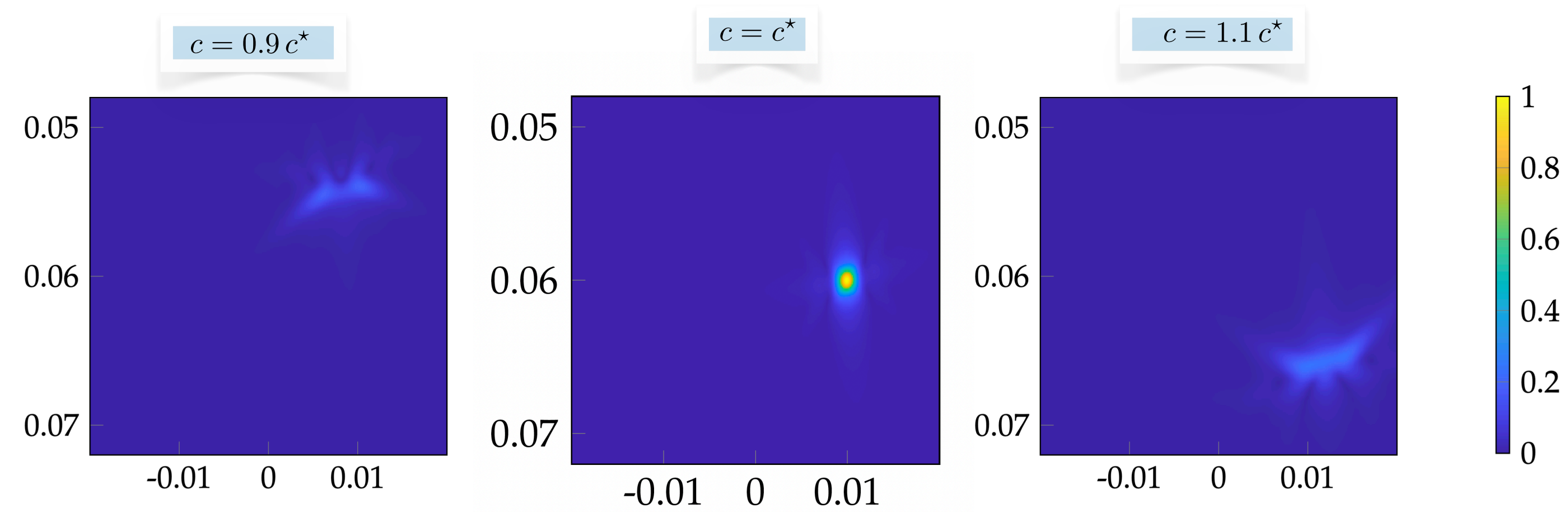
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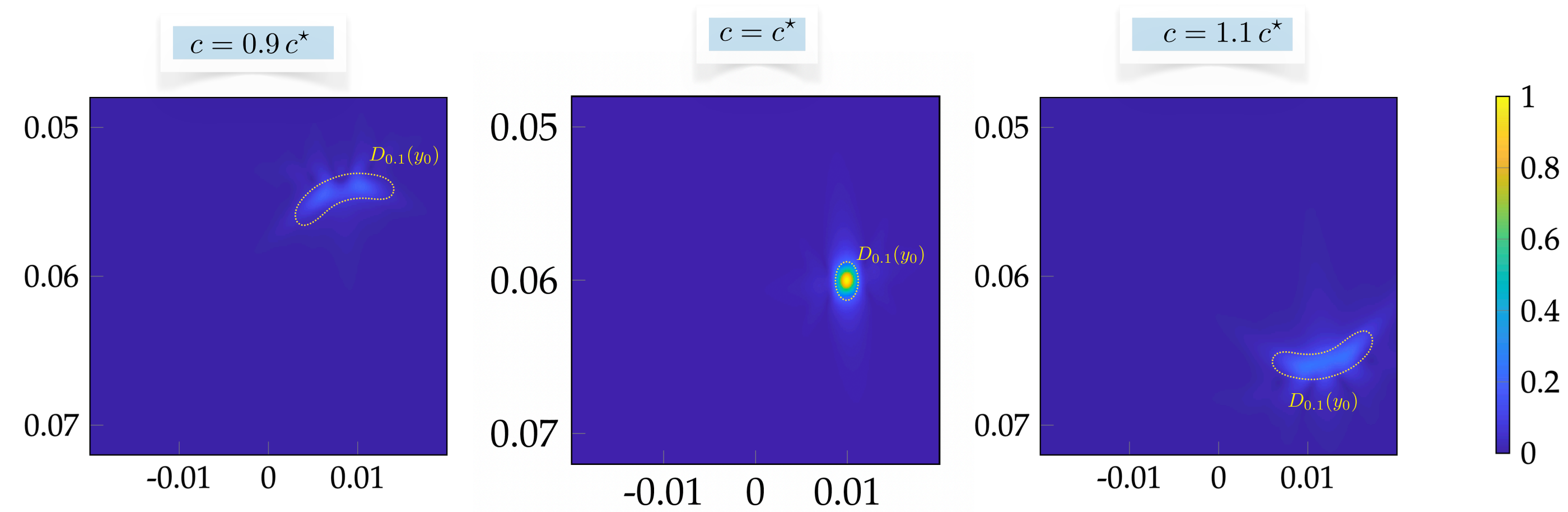
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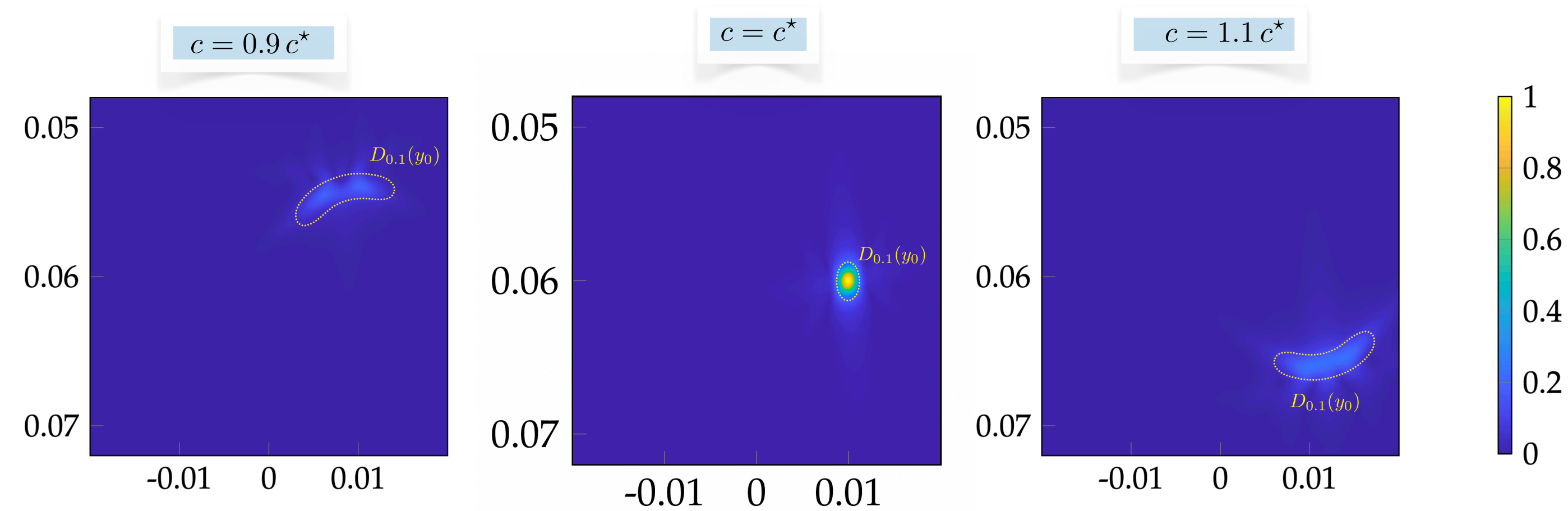
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The part of D' (the image) affected by the point $y_0 \in D$

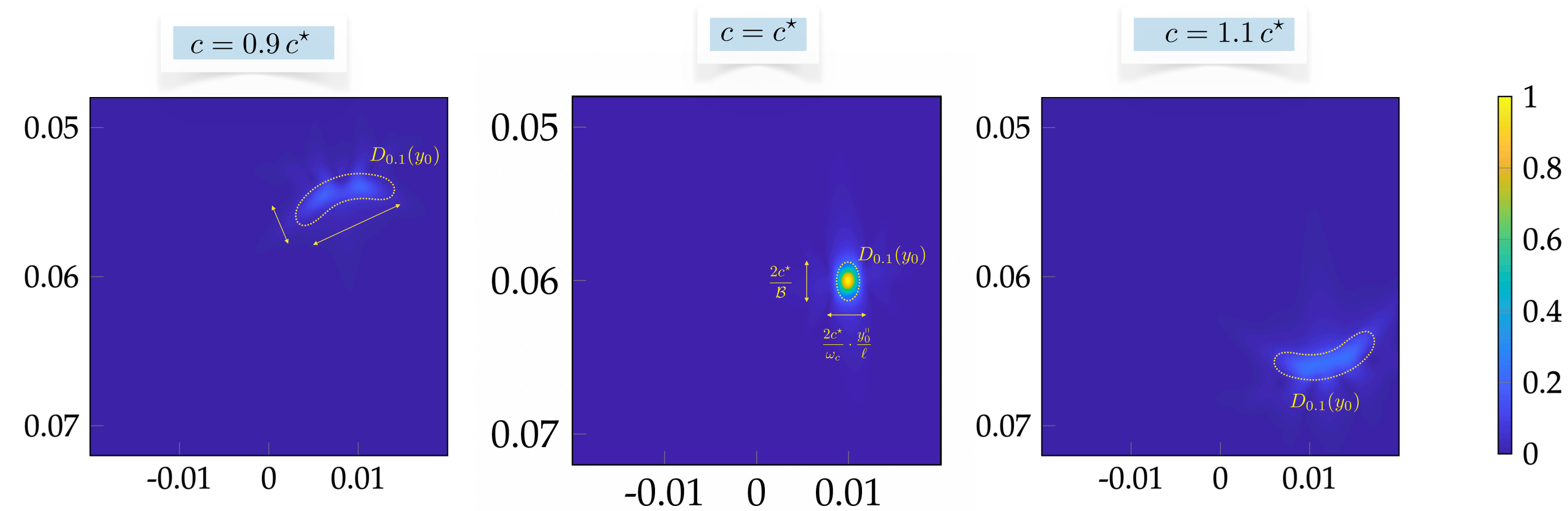
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Asymptotic analysis of the phase

Asymptotic analysis of the phase

$$F^{\frac{c}{c^*}}(z, y) = \int_{\mathcal{B}} \omega^2 \left(\int_{\mathcal{P}} \Gamma^{\frac{\omega}{c}}(z, x_r) \overline{G^*(y, x_r)} dx_r \right)^2 d\omega \quad z, y \in D' \times D.$$

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Focal spot

$$\frac{|z - x_r|}{c} - \frac{|y - x_r|}{c^*} = \mathcal{O}\left(\frac{1}{\omega}\right)$$

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Paraxial asymptotic regime ($\eta \ll 1$)

Bandwidth $\mathcal{B} := \frac{\mathcal{B}_0}{\eta}$ with $\mathcal{B}_0 := [\omega_0 - \frac{B}{2}, \omega_0 + \frac{B}{2}]$

Probe $\mathcal{P} := \eta^{\frac{1}{2}} \mathcal{P}_0$ with $\mathcal{P}_0 := [-\frac{a_0}{2}, \frac{a_0}{2}]^{d-1}$

Points $y := (y_\eta^\perp, y^\parallel) := (\eta^{\frac{1}{2}} y^\perp, y^\parallel)$

Scatterers $\varepsilon := o(\eta)$

Asymptotic analysis of the phase

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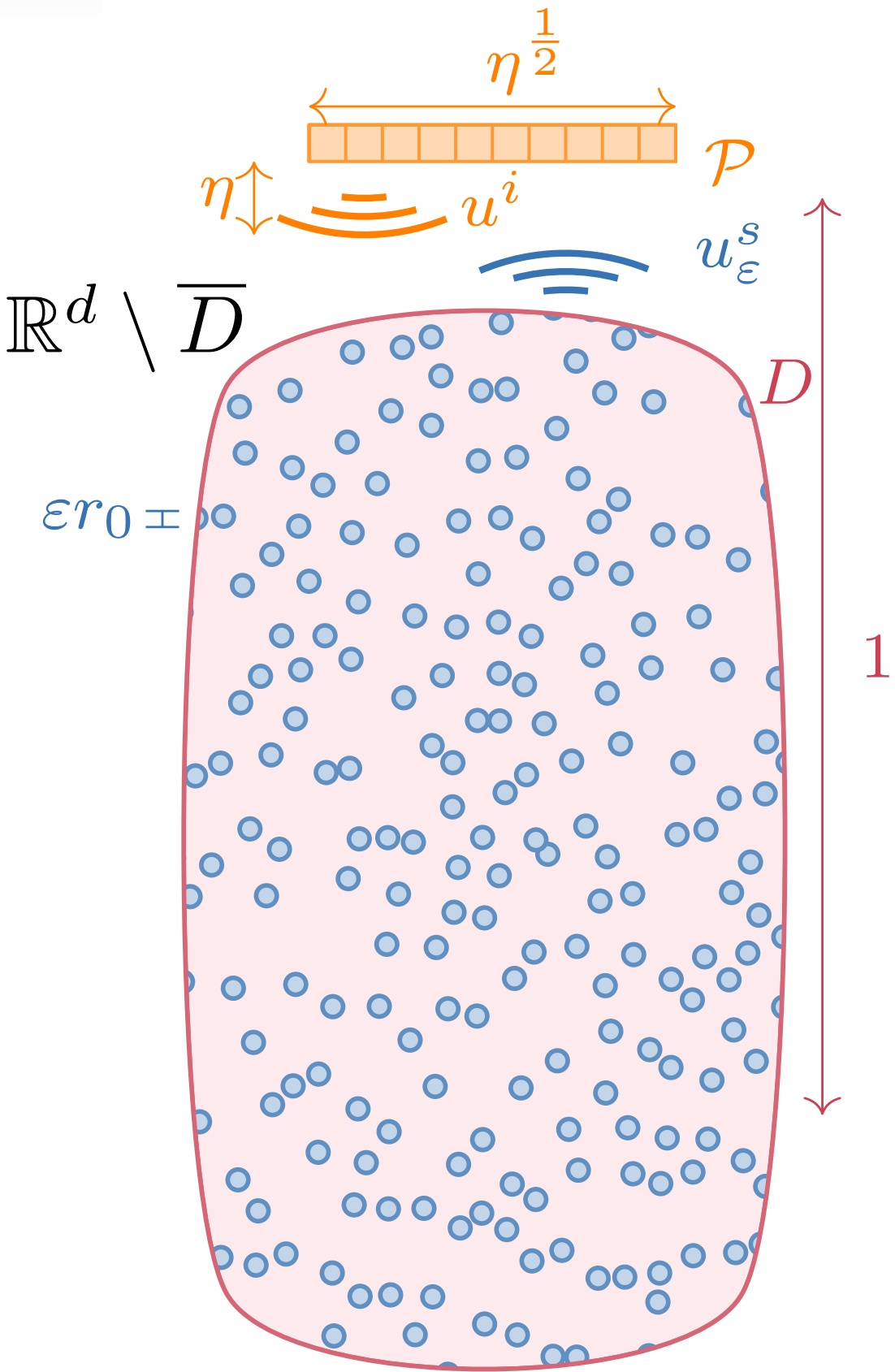
Points

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Scatterers

$\varepsilon := o(\eta)$

Parameter	Typical value
$\frac{1}{2\pi} \mathcal{B}$	[2, 6] MHz
$\frac{c^\star}{c}$	1500 m s ^{−1}
$ \mathcal{P} $	5 cm
$y^\parallel$	10 cm
$y_\eta^\perp$	5 cm
εr_0	10 μm



Center of the focal spot at a given speed c

$$y = (\eta^{\frac{1}{2}} y^{\perp}, y'')$$

$$z = (\eta^{\frac{1}{2}} z^{\perp}, z'')$$

Rewriting the phase: $\Phi(z, y) = \tilde{\Phi}(z - \varphi_c(y))$

Point in the physical domain (fixed)

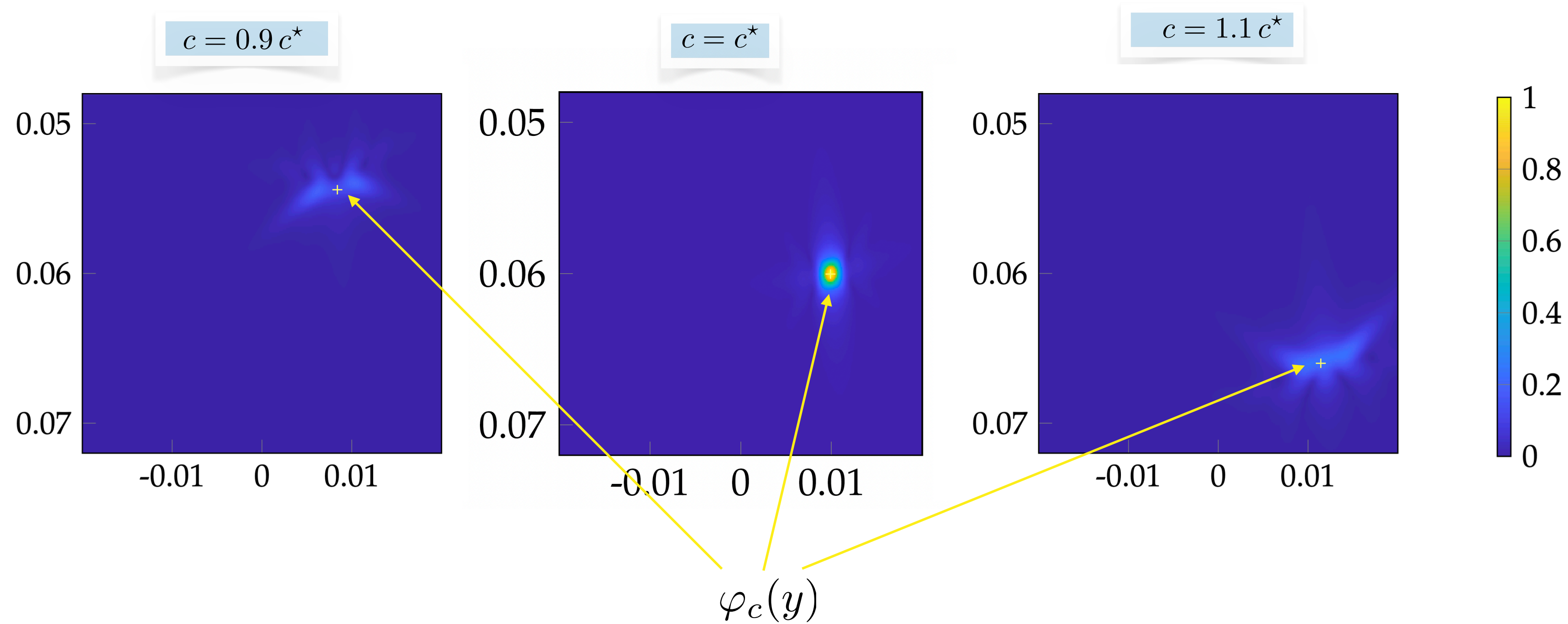
Pixel on the image

Center of focal spot in the image

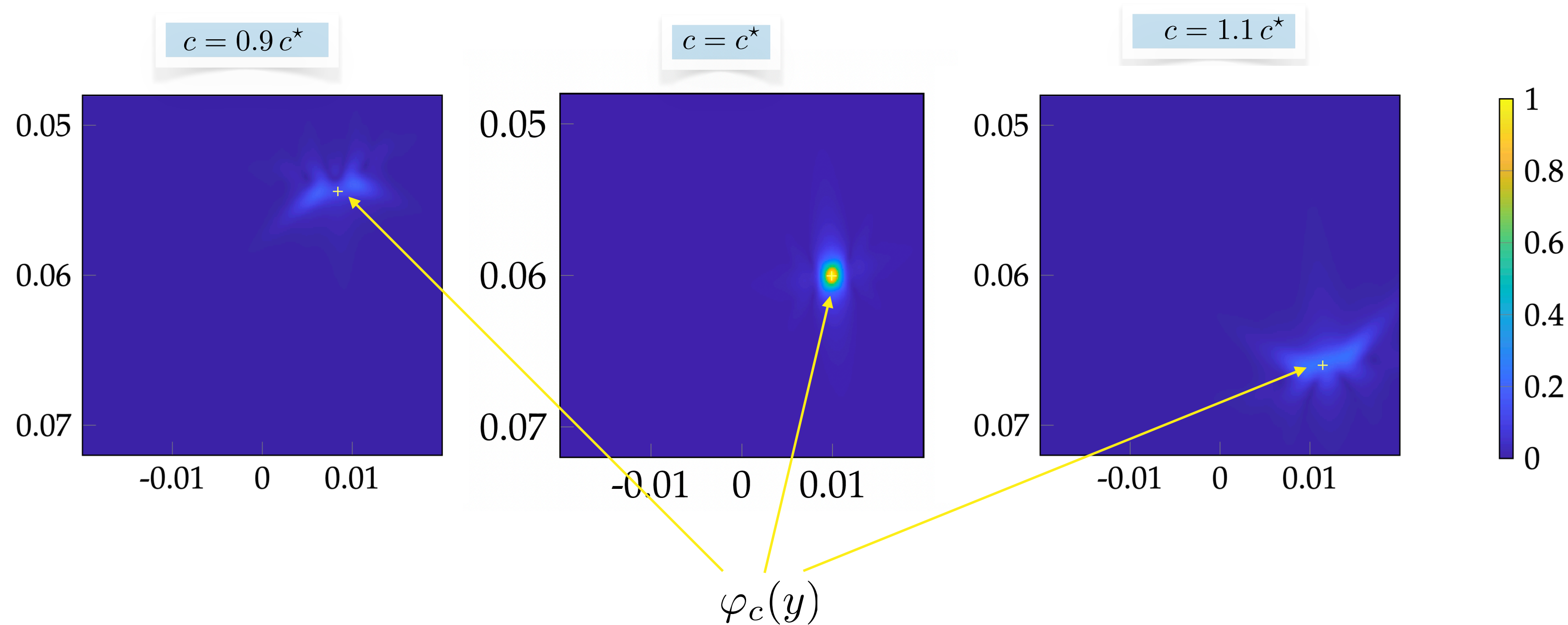
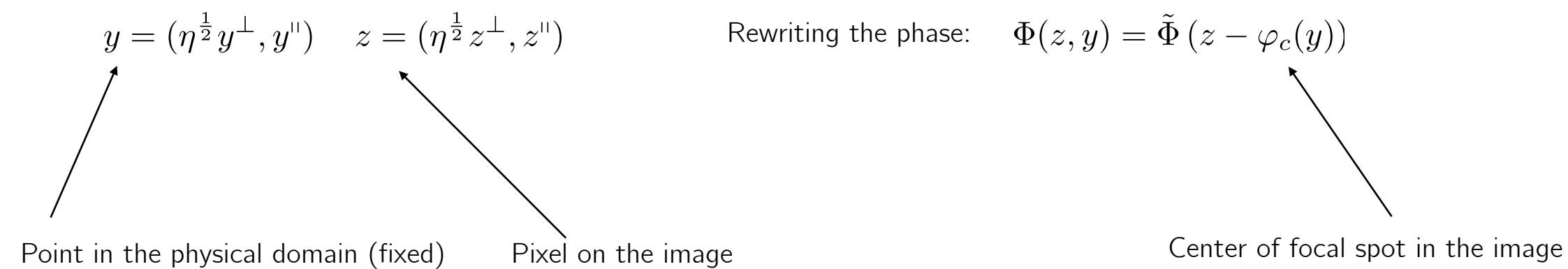
Center of the focal spot at a given speed c

$y = (\eta^{\frac{1}{2}} y^{\perp}, y^{\parallel})$ $z = (\eta^{\frac{1}{2}} z^{\perp}, z^{\parallel})$ Rewriting the phase: $\Phi(z, y) = \tilde{\Phi}(z - \varphi_c(y))$

Point in the physical domain (fixed) Pixel on the image Center of focal spot in the image



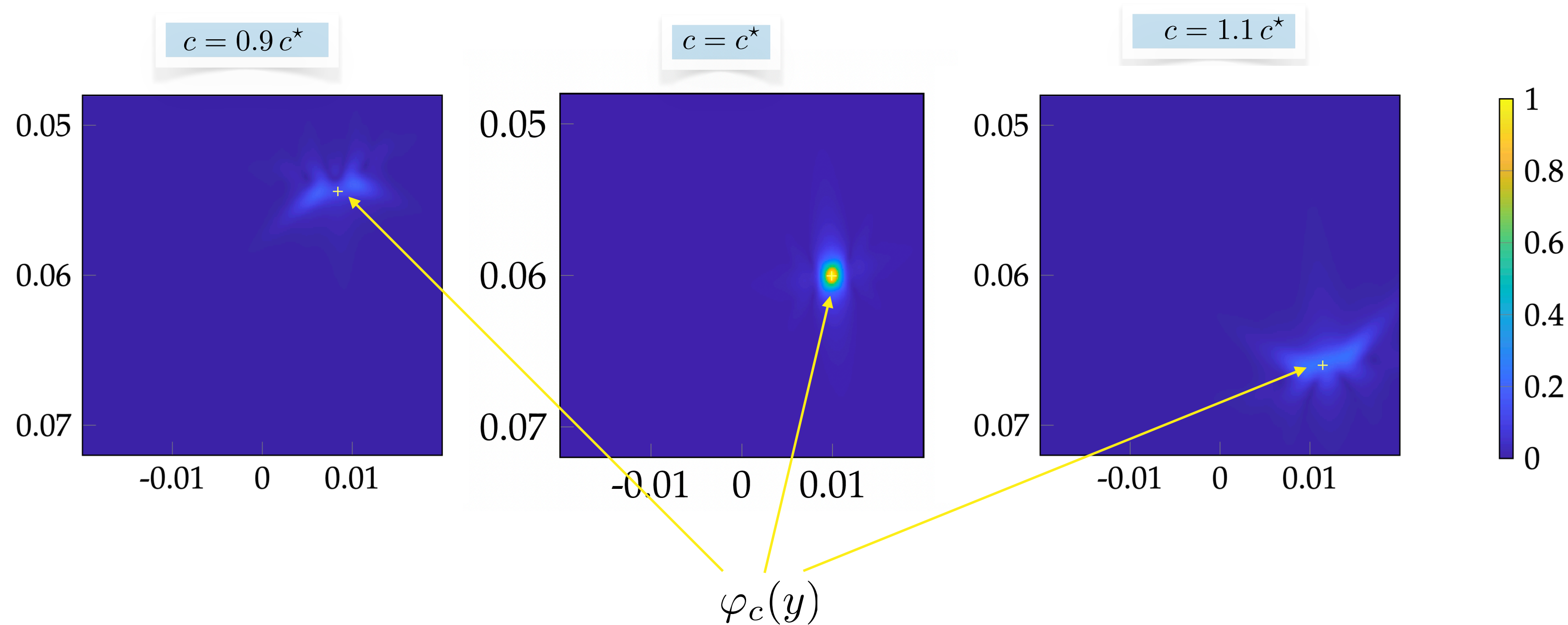
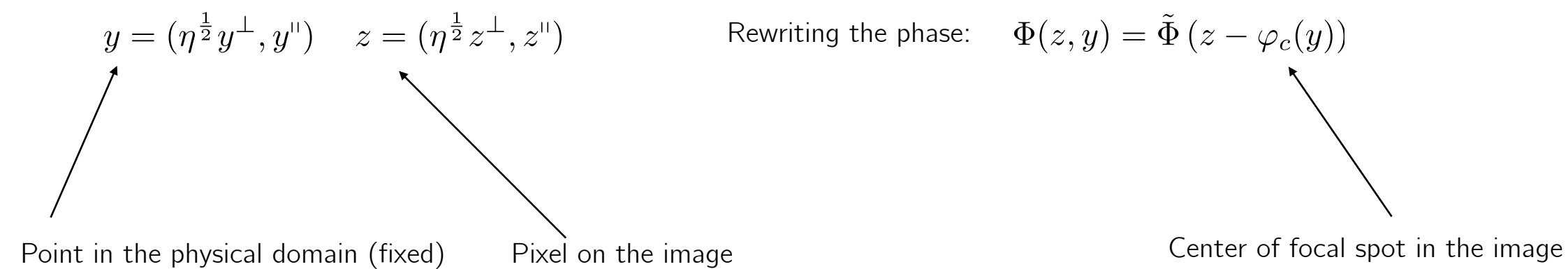
Center of the focal spot at a given speed c



Asymptotic expansion of travel times in the paraxial regime

$$\frac{|z - x_r|}{c} - \frac{|y - x_r|}{c^*} = \sum_k \eta^k f_k(z - \varphi_c(y))$$

Center of the focal spot at a given speed c



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Center of the focal spot

$$\varphi_c(y) = \left(\left(\frac{c}{c^*} \right)^2 \eta^{\frac{1}{2}} y^{\perp}, \frac{c}{c^*} y^{\parallel} \right)$$

Expansion of the PSF around the center of the focal spot

Analytic approximation of the PSF

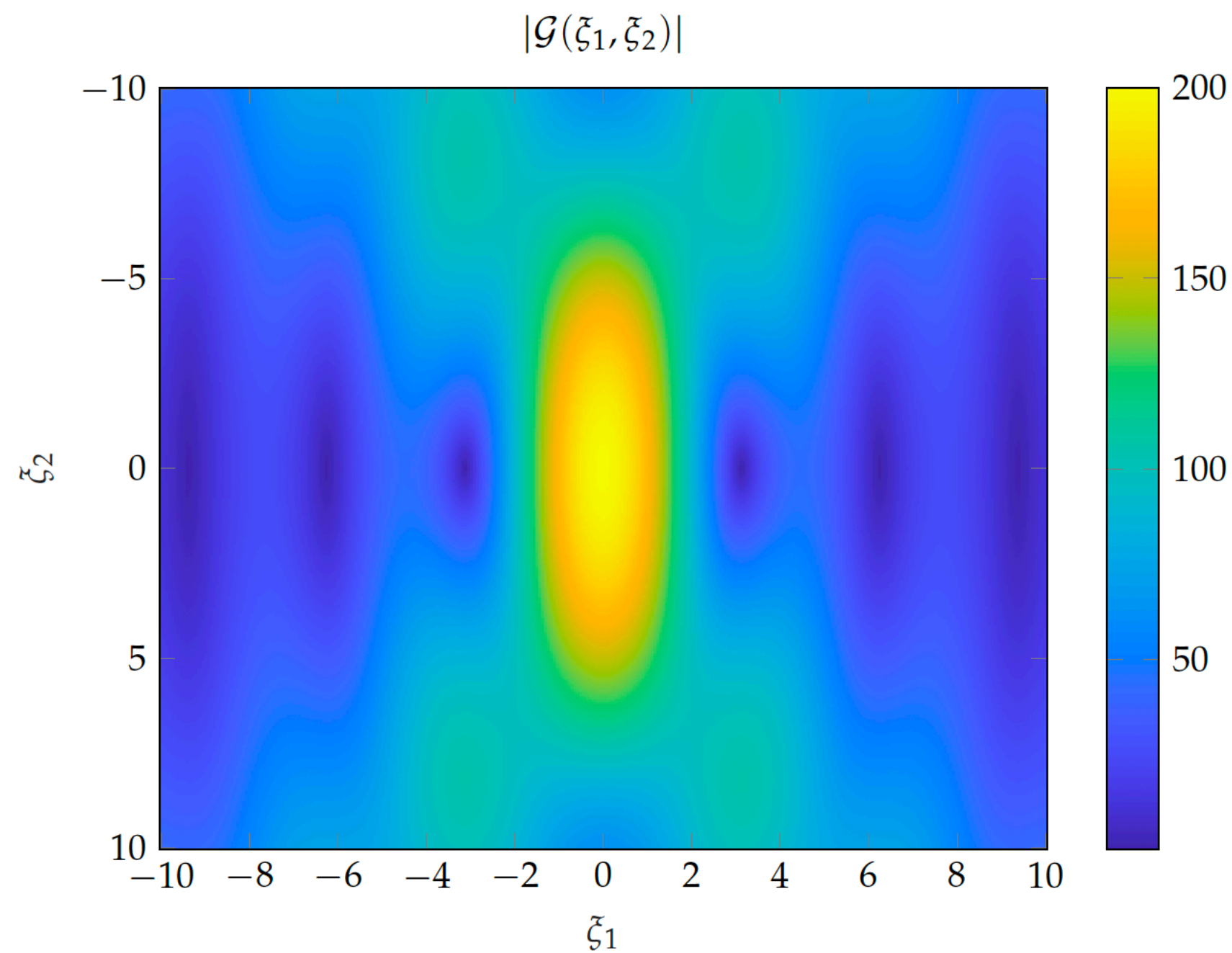
$$F^c(z, y) = \eta^{-1} \left(\frac{c}{c^\star} \right)^2 \frac{\ell_0^4}{(16\pi^2 |z| |\varphi_c(y)|)^2} \int_{\mathcal{B}_0} \omega^2 e^{i \frac{2\omega}{\eta c} (|z| - |\varphi_c(y)|)} e^{i \frac{\omega}{c} \left(1 - \left(\frac{c^\star}{c} \right)^2 \right) \frac{|\varphi_c(y)^\perp|^2}{|\varphi_c(y)|}} \\ \mathcal{G}^2 \left(\frac{\omega \ell_0}{c} \left(\frac{z^\perp}{|z|} - \frac{\varphi_c(y)^\perp}{|\varphi_c(y)|} \right), \frac{\omega \ell_0^2}{c} \left(\frac{1}{|z|} - \left(\frac{c}{c^\star} \right)^2 \frac{1}{|\varphi_c(y)|} \right) \right) d\omega + \mathcal{O}(1).$$

$$\mathcal{G}(\xi_1, \xi_2) := \int_{[-1,1]^2} e^{-ix_e^\perp \cdot \xi_1 + i \frac{|x_e^\perp|^2}{2} \xi_2} dx_e^\perp \\ \xi_1 \in \mathbb{R}^{d-1}, \xi_2 \in \mathbb{R}.$$

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PSF amplitude estimator

Definition : Confocal $\mathcal{F}$ trace at y_0

$$[c_{\min}, c_{\max}] \longrightarrow \mathbb{C}$$

$$c \longmapsto \mathcal{F}(c) := F^{\frac{c}{c^*}}(\phi_c(y_0), y_0)$$

with $y_0 \in D$

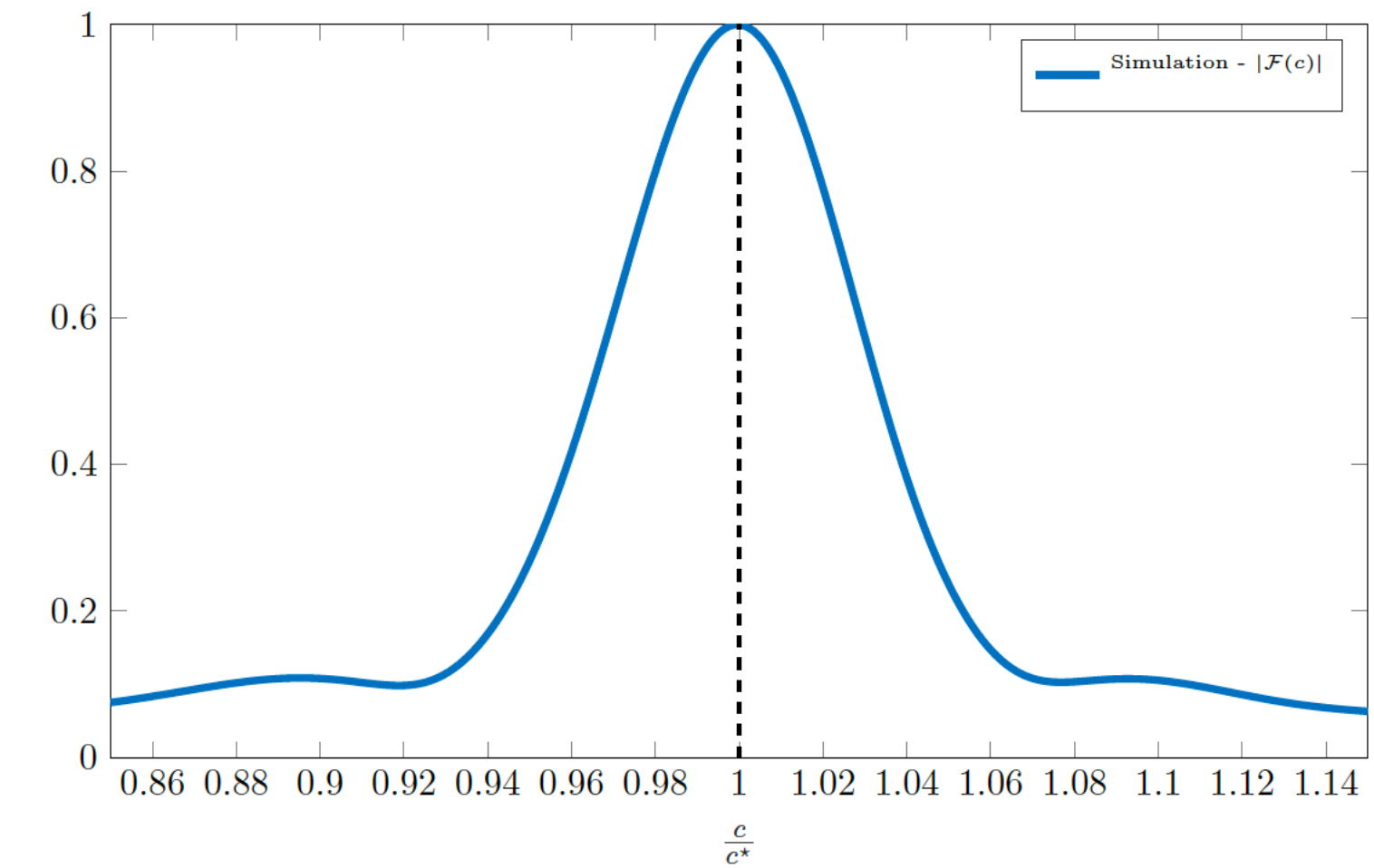
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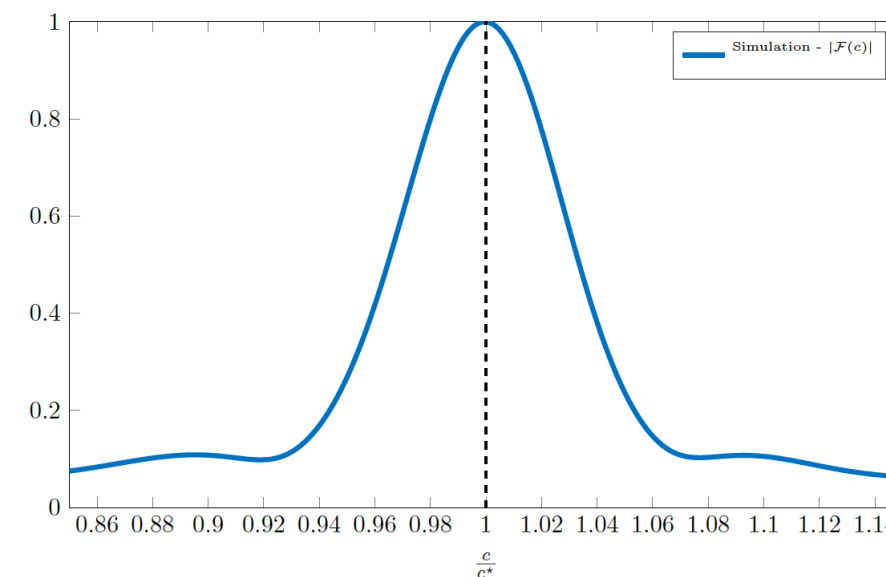


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Proposition : Amplitude Estimator

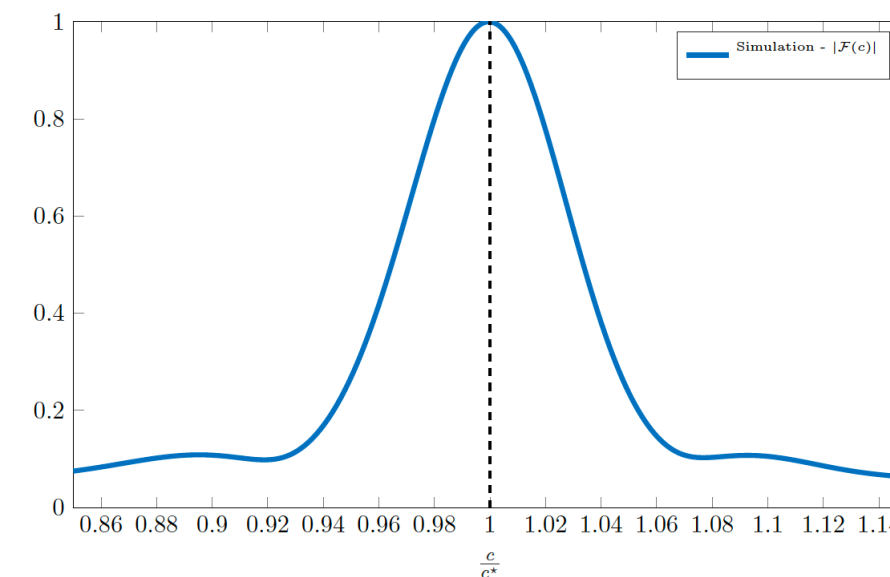
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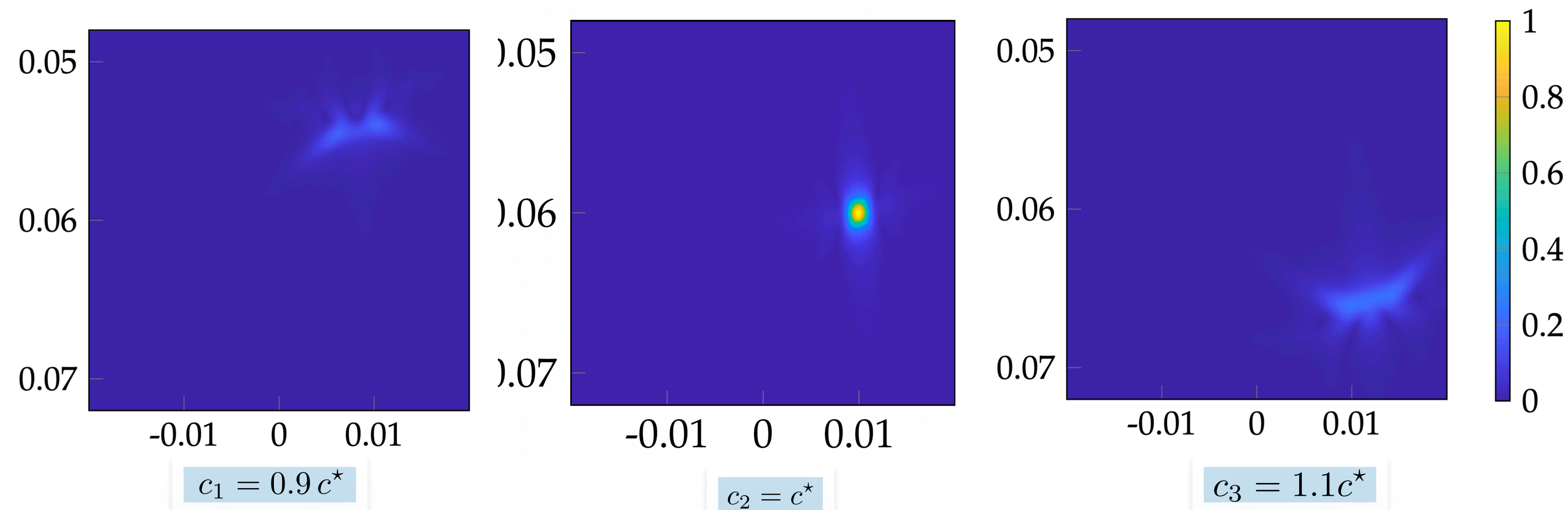
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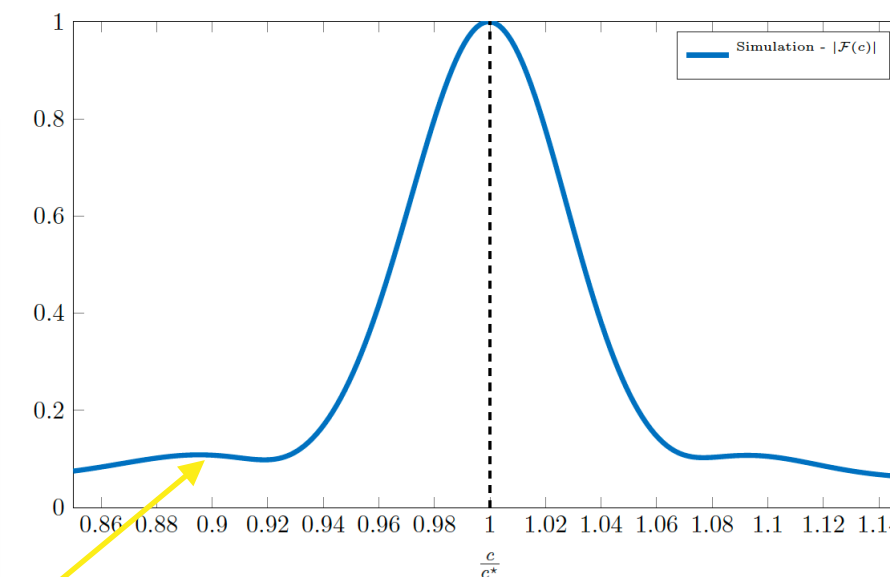
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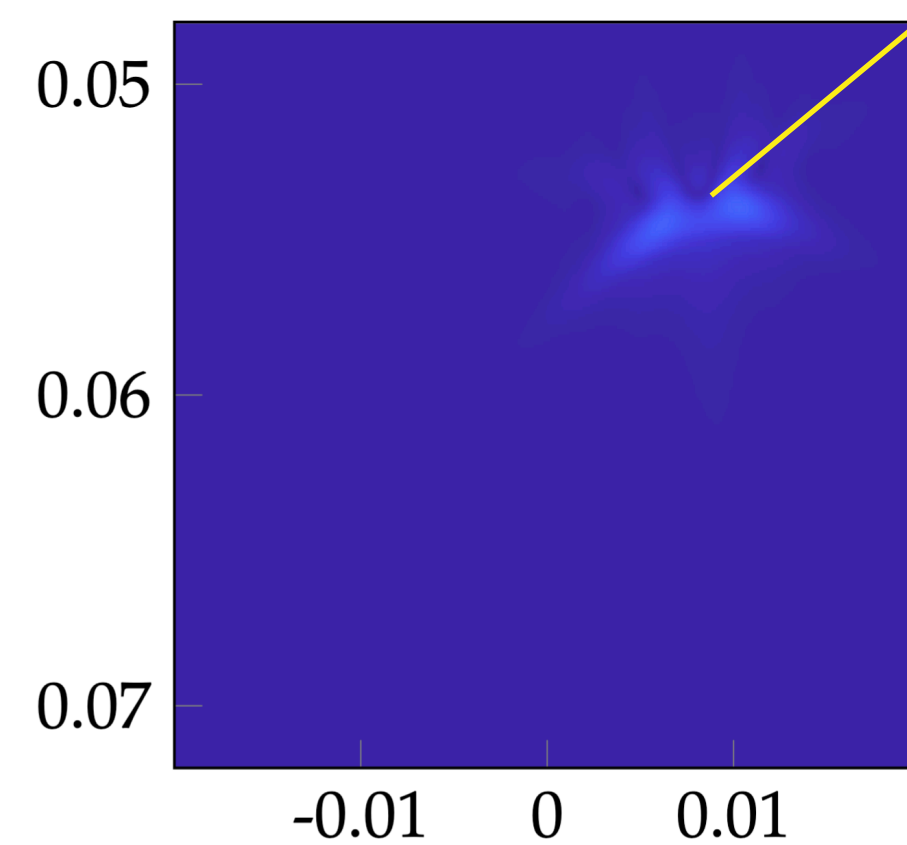
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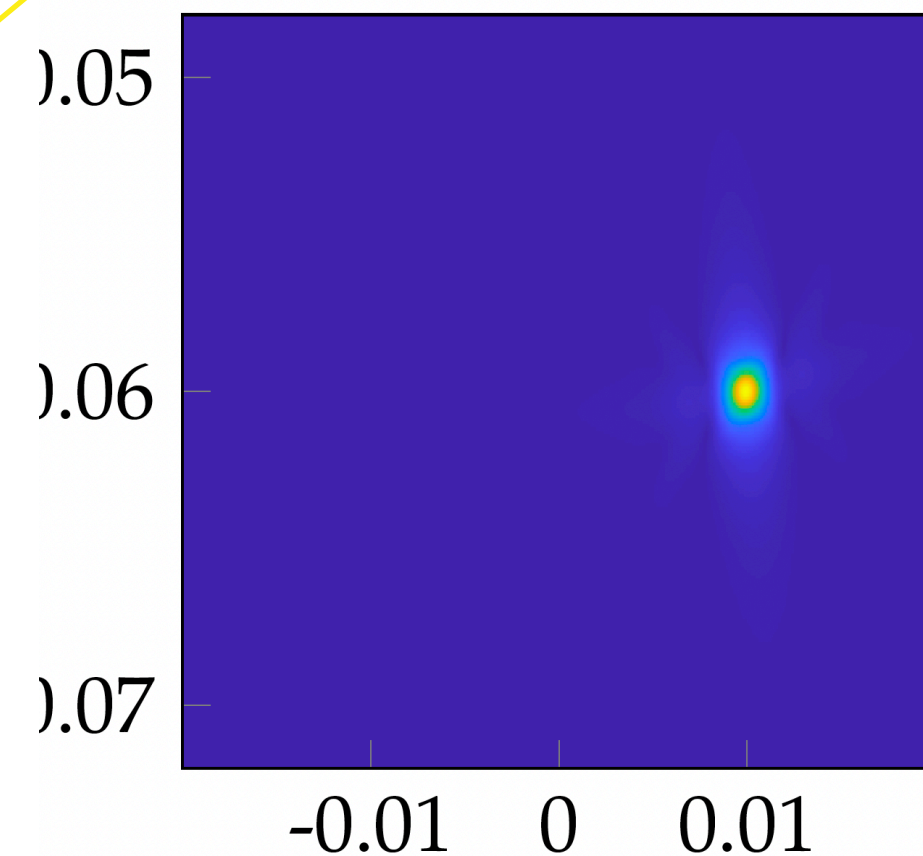
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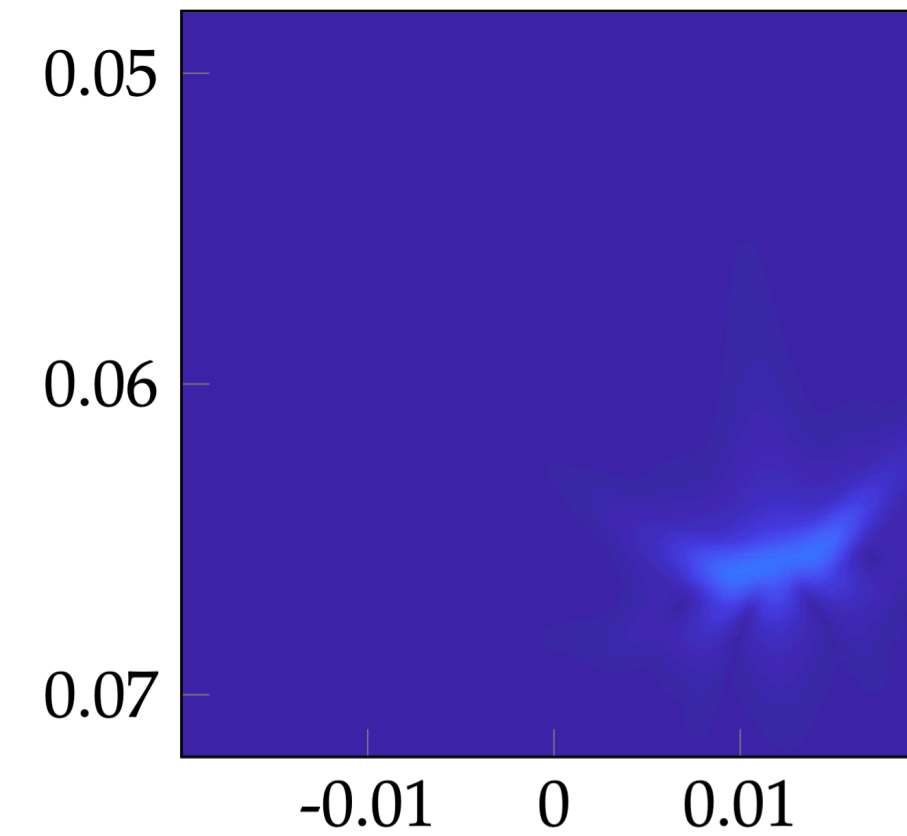
$\mathcal{F}(c_1)$



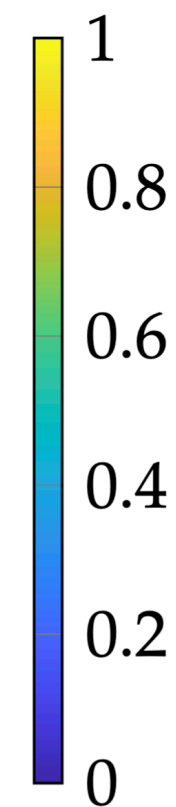
$$c_1 = 0.9 c^*$$



$$c_2 = c^*$$



$$c_3 = 1.1 c^*$$



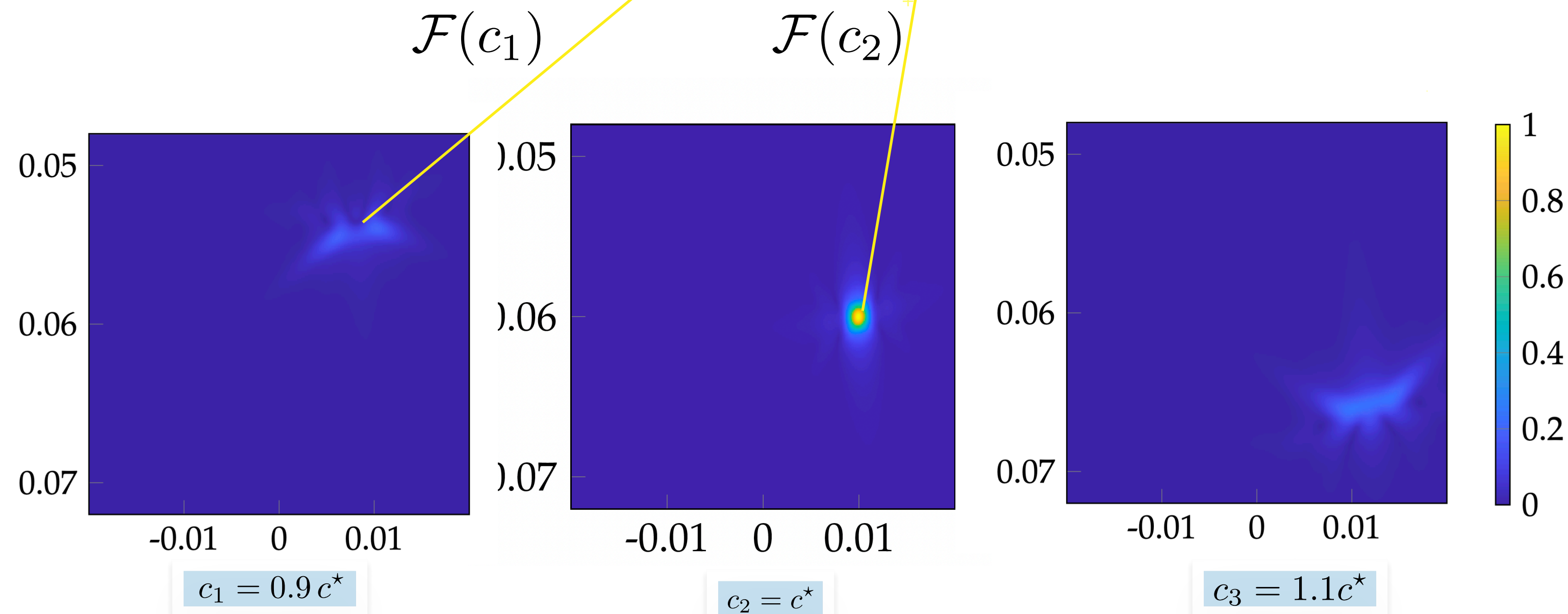
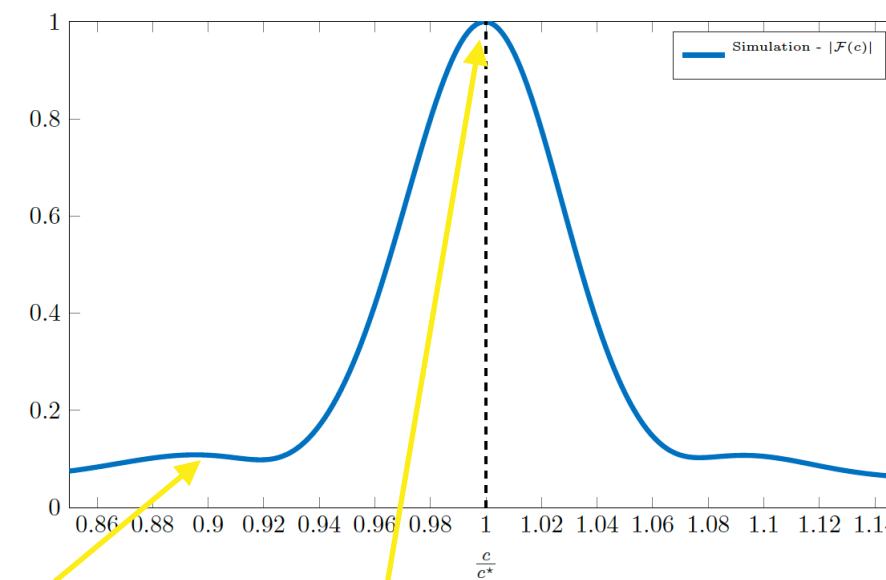
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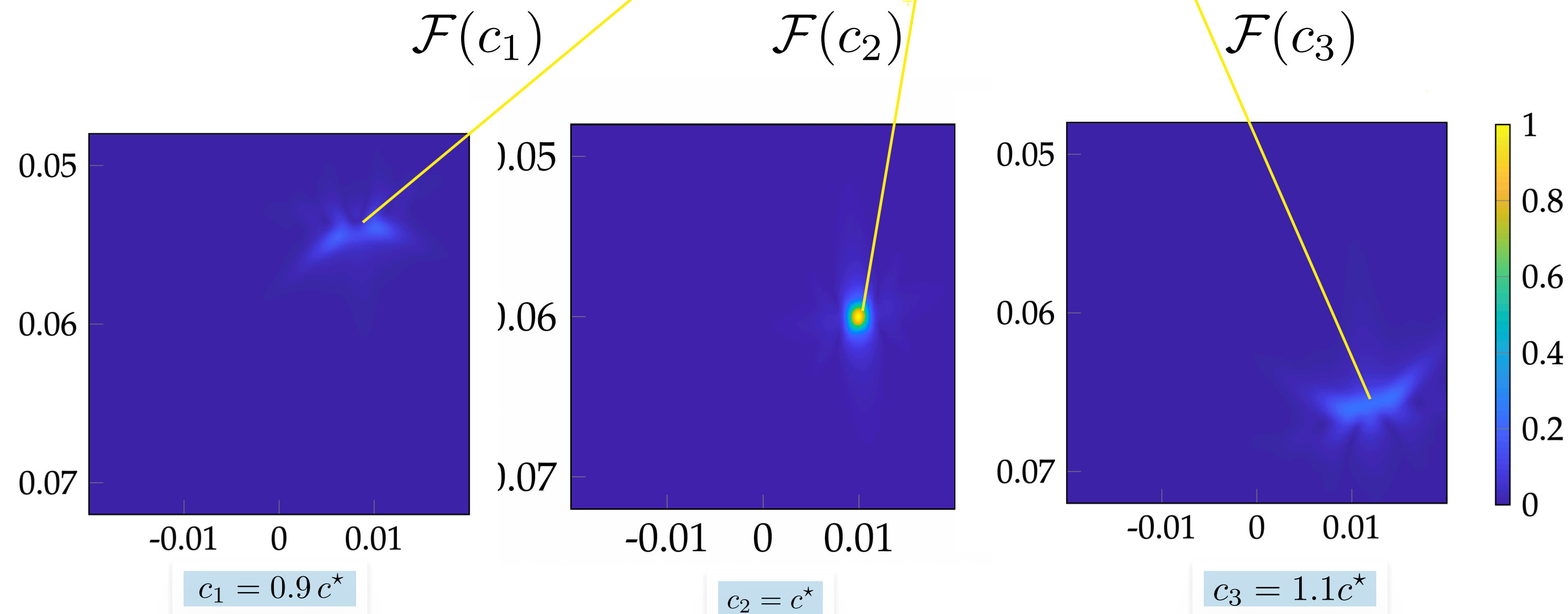
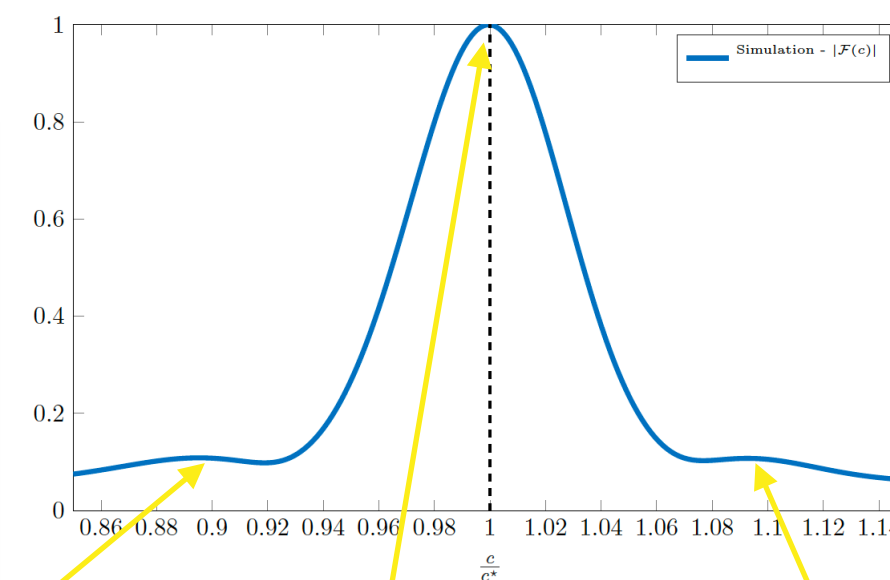
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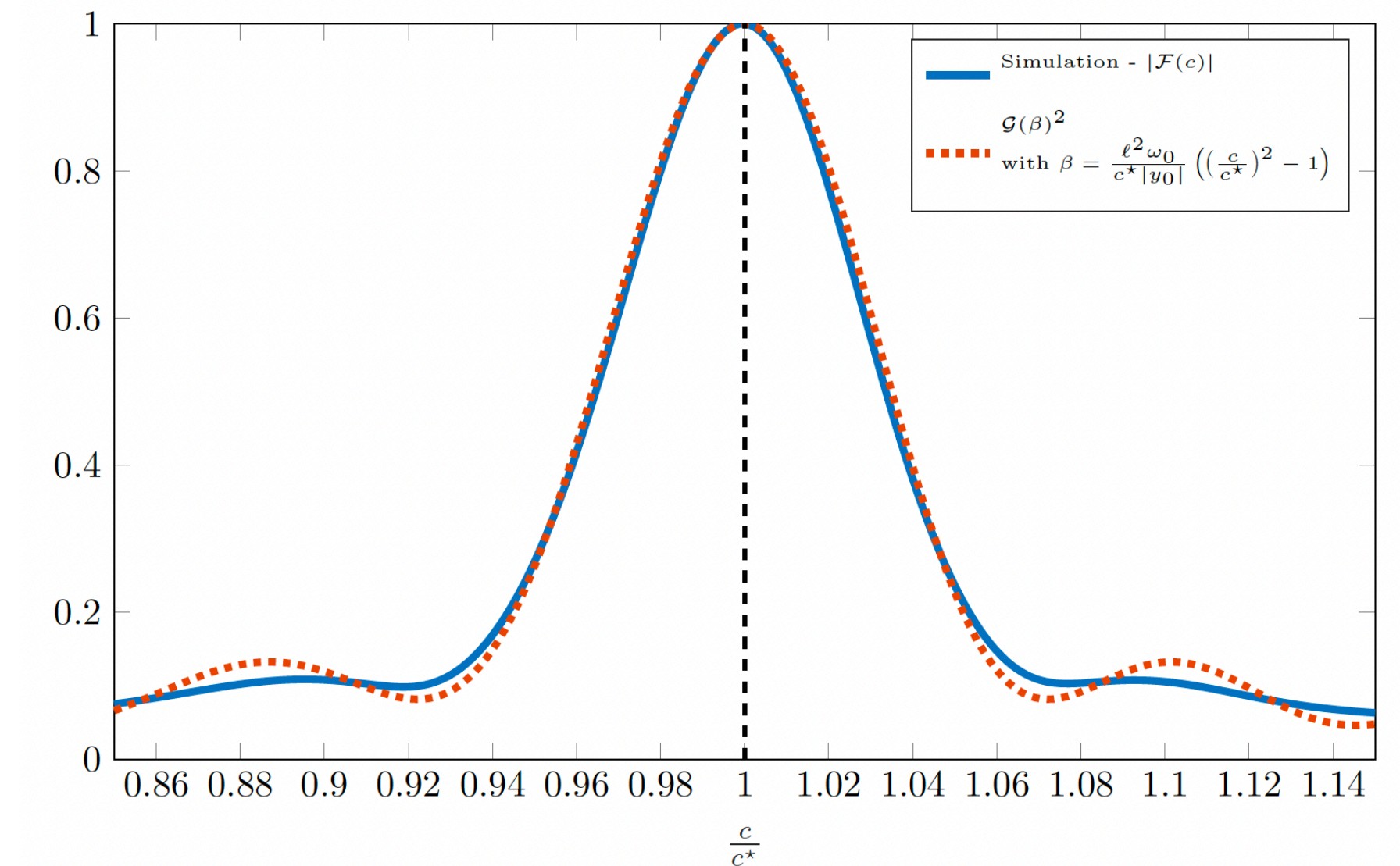
Asymptotic expression

Lemma : Asymptotic development (paraxial regime)

$$\mathcal{F}(c) \sim \mathcal{G}(\beta)^2 \quad \text{with} \quad \beta = \frac{\ell^2 \omega_0}{c^\star |y_0|} \left(\left(\frac{c}{c^\star} \right)^2 - 1 \right)$$

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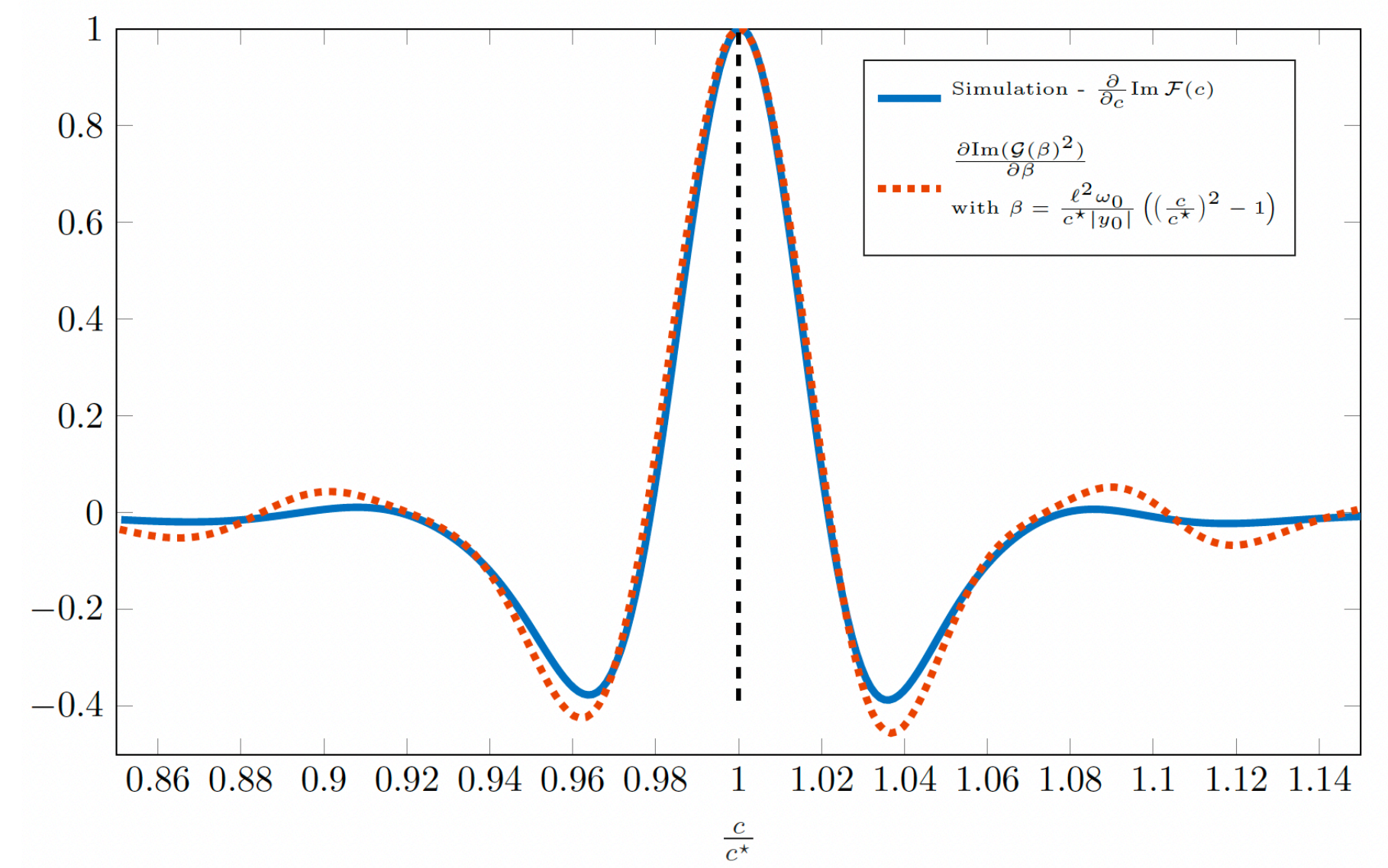
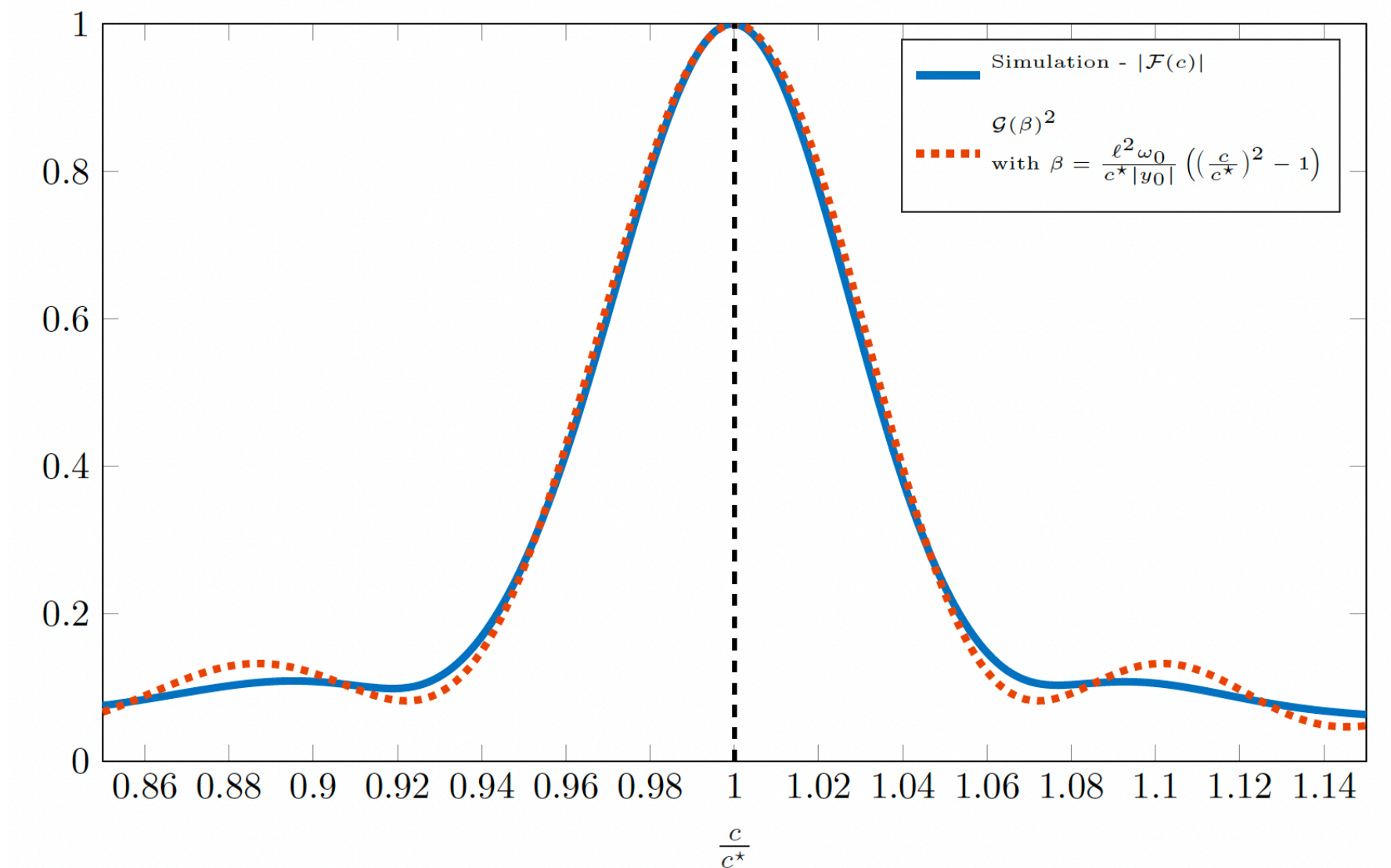
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Proposition : Phase jump estimator

$$c^\star = \operatorname{argmax}_c \frac{\partial}{\partial c} \operatorname{Im} \mathcal{F}(c).$$



The micro-structured medium problem

- The PSF can be used to build an estimator for the speed of sound

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Maximising brightness at center of focal spot

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How does one access the PSF in a microstructured medium

The dual focal spot

Image domain

$$\begin{aligned} D' &\longrightarrow D' \\ z &\longmapsto \left| F^{\frac{c}{c^*}}(z, y_0) \right| \end{aligned}$$



Exchanging the roles of c and c^*

Physical domain

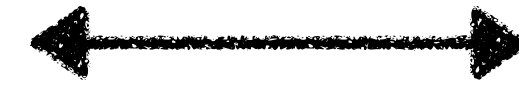
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centered around $z_0(c) = \varphi_c(y_0) \in D'$



Exchanging the roles of c and c^*

Physical domain

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The dual focal spot

Image domain

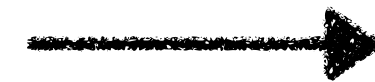
$$\begin{aligned} D' &\longrightarrow D' \\ z &\longmapsto \left| F^{\frac{c}{c^*}}(z, y_0) \right| \end{aligned}$$

Physical domain

$$\begin{aligned} D &\longrightarrow D \\ y &\longmapsto \left| F^{\frac{c}{c^*}}(z_0, y) \right| \end{aligned}$$

$\longleftrightarrow$
Exchanging the roles of c and c^*

Has a small « quasi-support »
centered around $z_0(c) = \varphi_c(y_0) \in D'$



The focal spot

The dual focal spot



Has a small « quasi-support »
centered around $y_0(c) = \varphi_c^{-1}(z_0) \in D$

The dual focal spot

Image domain

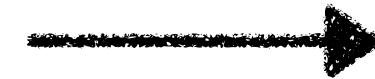
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$$D'_\delta(c, y_0)$$



$$D_\delta(c, z_0)$$

The part of the image affected by the
point $y_0 \in D$

The part of the domain probed by the
pixel $z_0 \in D'$

Virtual random reflector

$$I^c(z) = \int_D (n(y) - n^\star) F^{\frac{c}{c^\star}}(z, y) dy, \quad z \in D' \quad \longrightarrow \quad I^c(z) \approx \int_{D(c, z)} (n(y) - n^\star) F^{\frac{c}{c^\star}}(z, y) dy, \quad z \in D'$$

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Whole physical domain

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Whole physical domain

Small domain around $\varphi_c^{-1}(z)$

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Whole physical domain

Small domain around $\varphi_c^{-1}(z)$

$I^c(z)$ depends on the realization of $n(y) - n^\star$ in the small subdomain $D(c, z) \subset D$

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Proposition : Variance of I^c

$$\mathbb{E} \left[|I^c(z)|^2 \right] = \varepsilon^d C_n \int_{D(c,z)} |F^c(z, y)|^2 dy + o(\varepsilon^d)$$

C_n the integral of the covariance of n .

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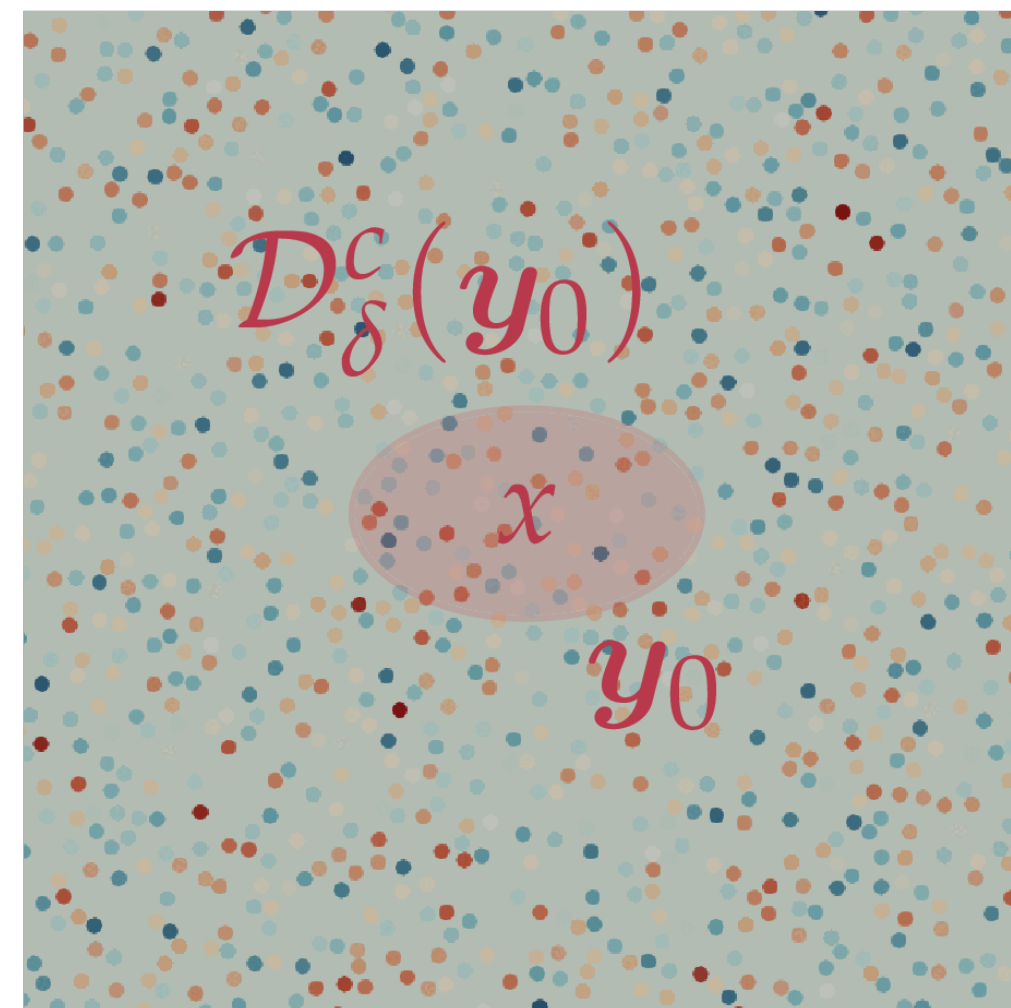
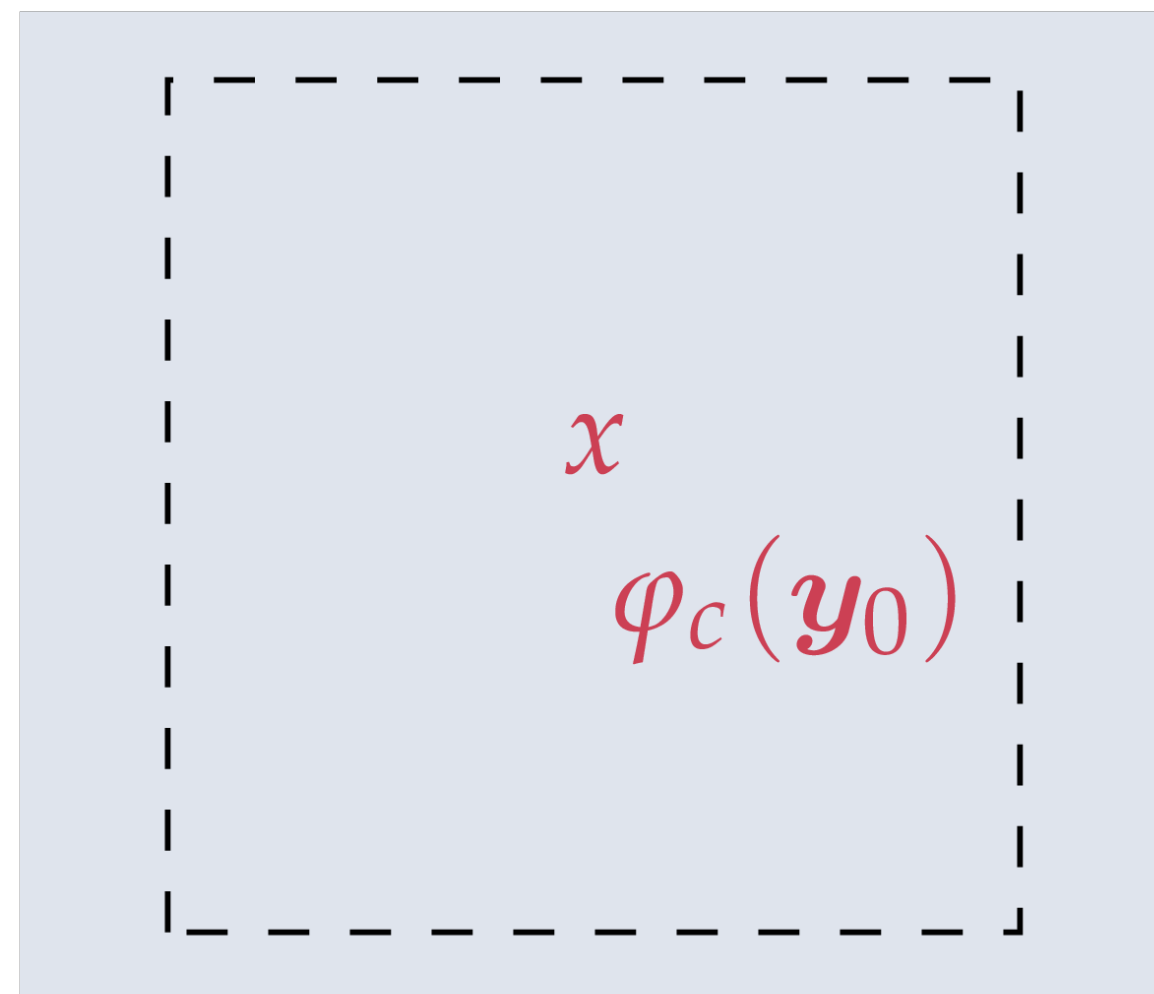
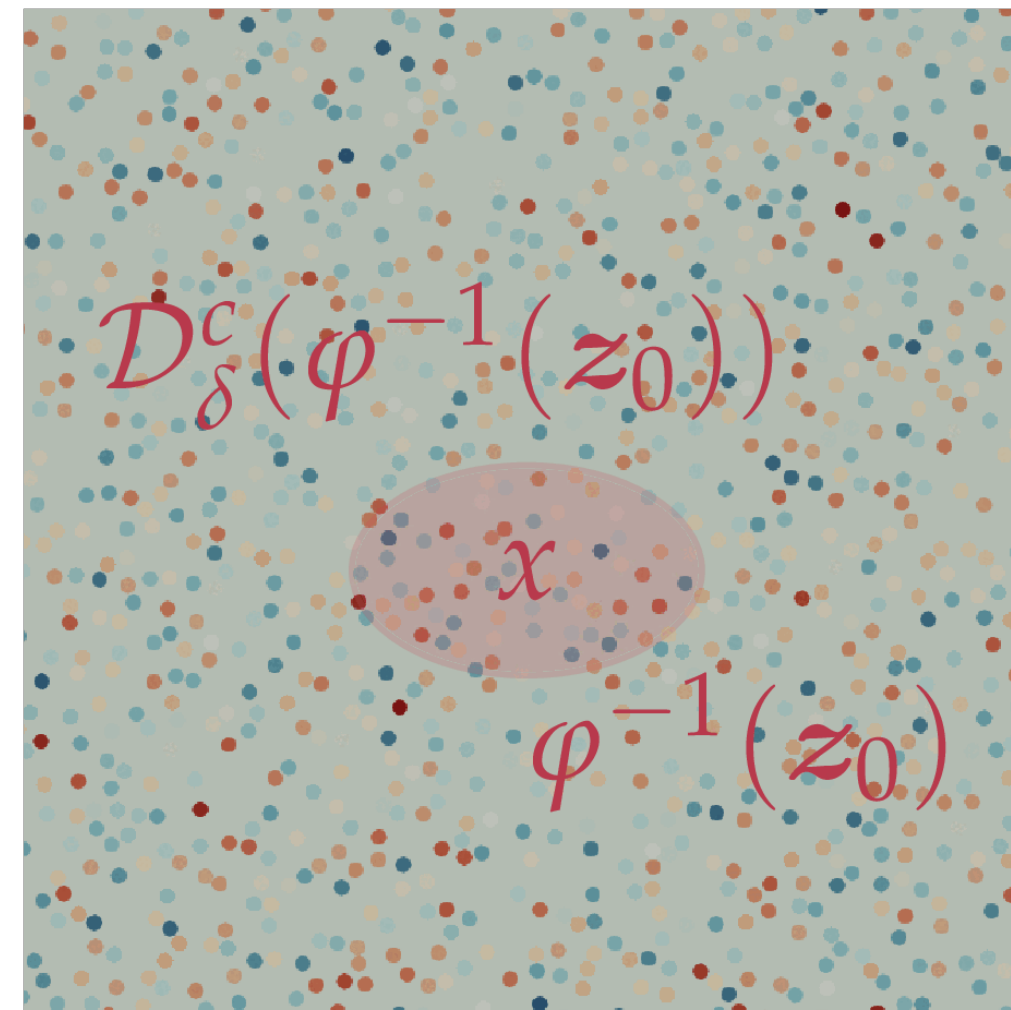
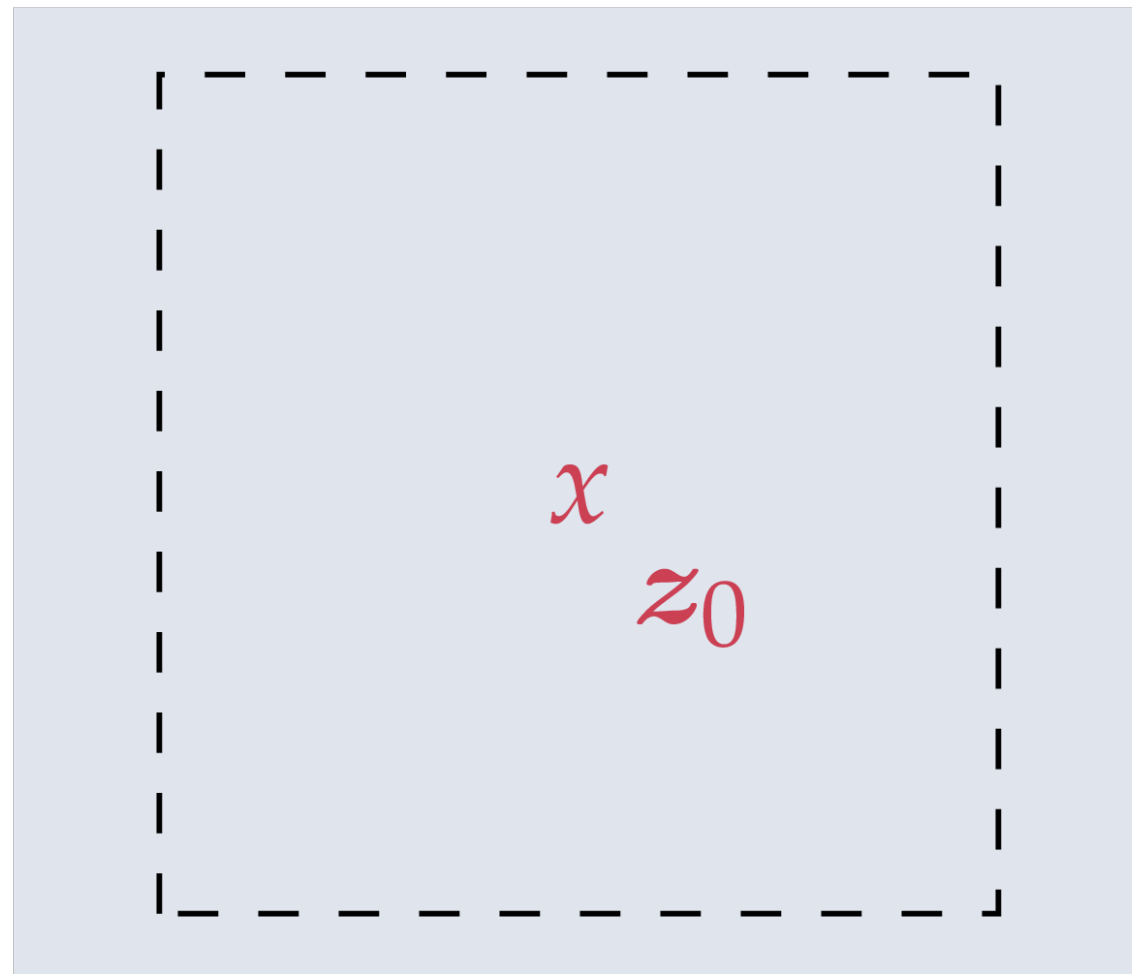
C_n the integral of the covariance of n .



$D(c,z)$ centered around $\varphi_c^{-1}(z)$ - moves with c

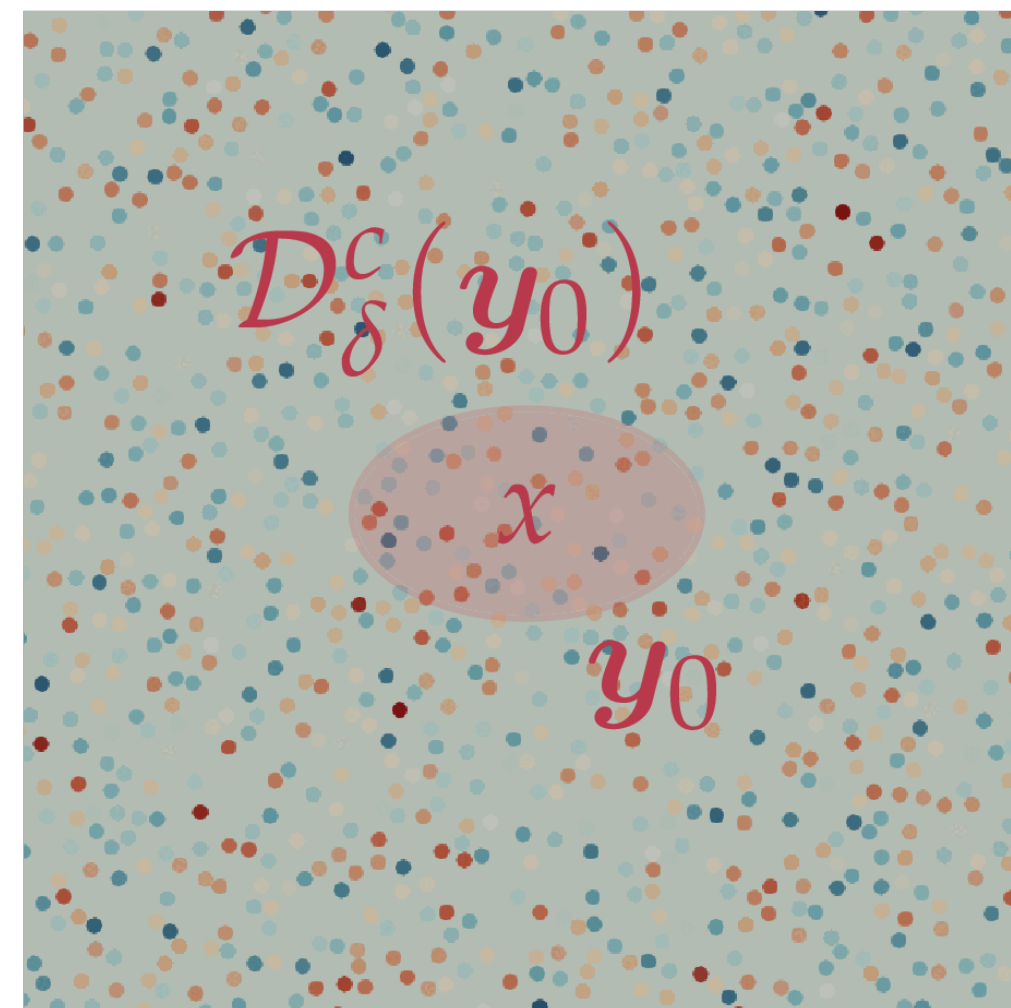
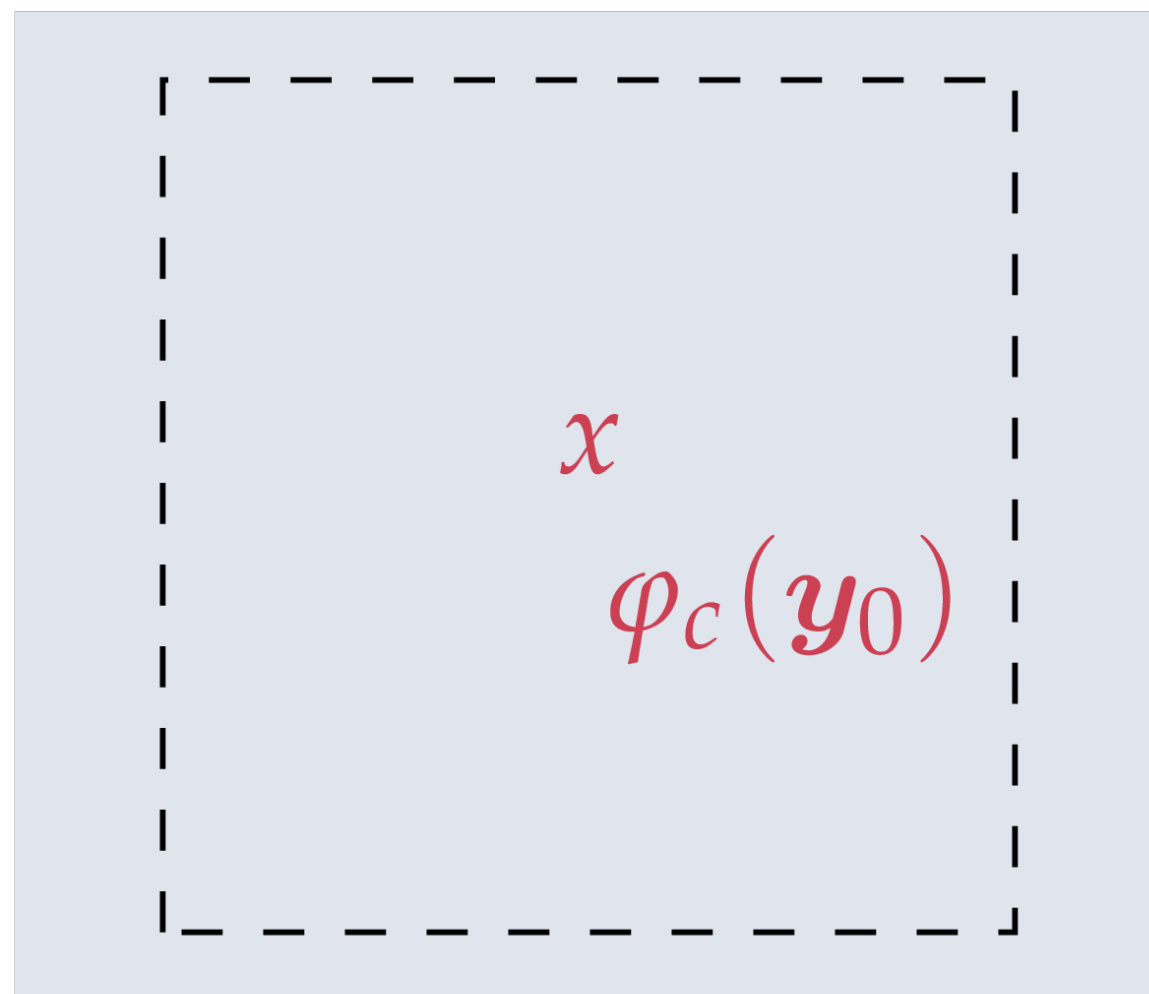
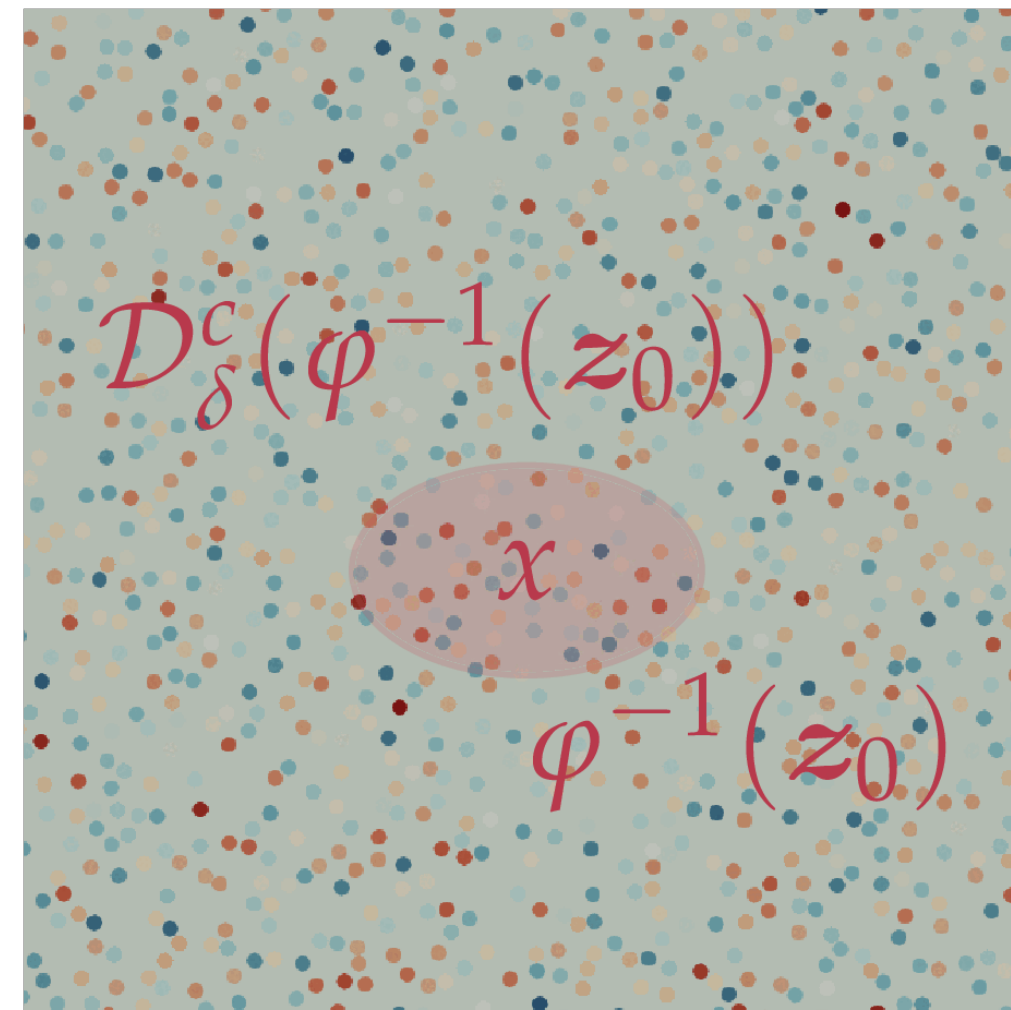
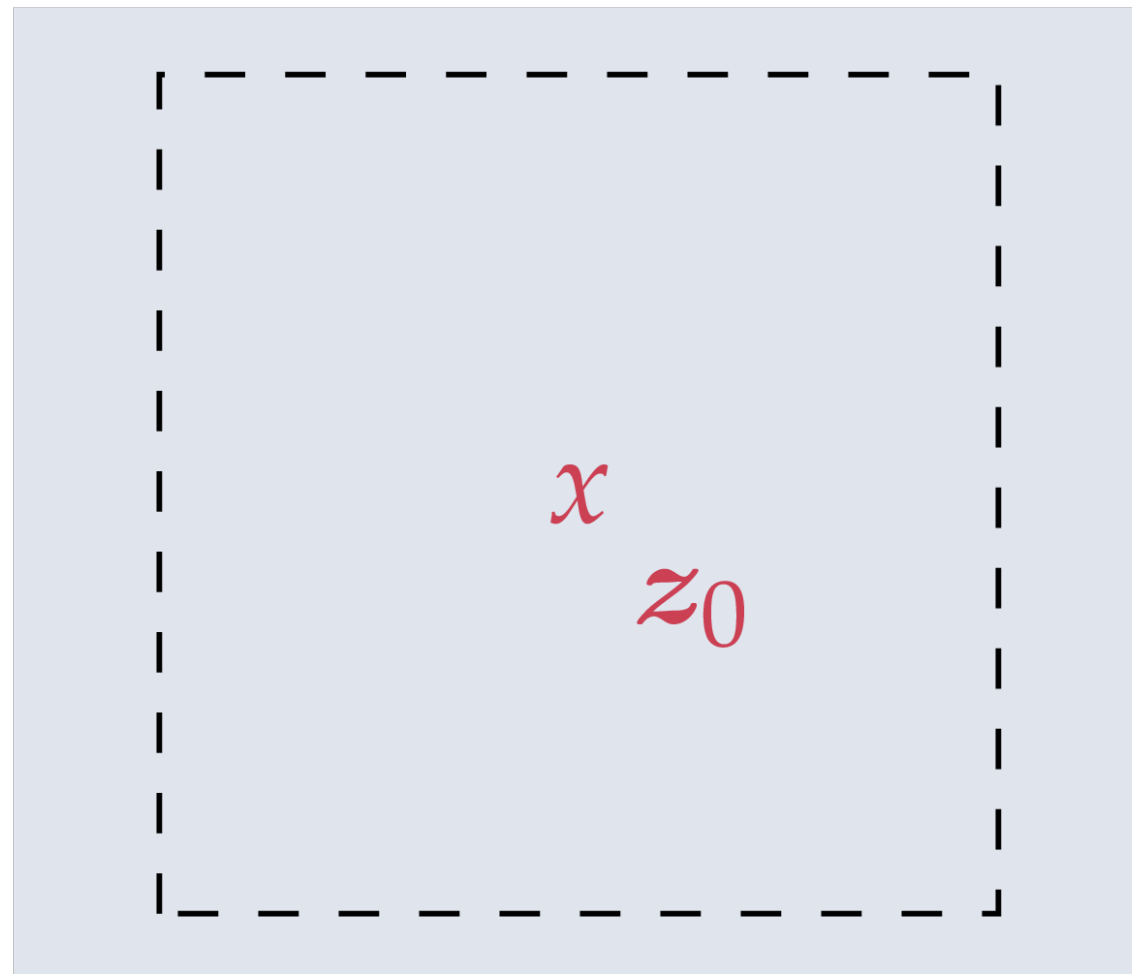
Moving focal spots

$$D' \text{ (Image)} \quad \textcolor{red}{c} = 1.2 * c^* \quad D \text{ (Physical domain)}$$



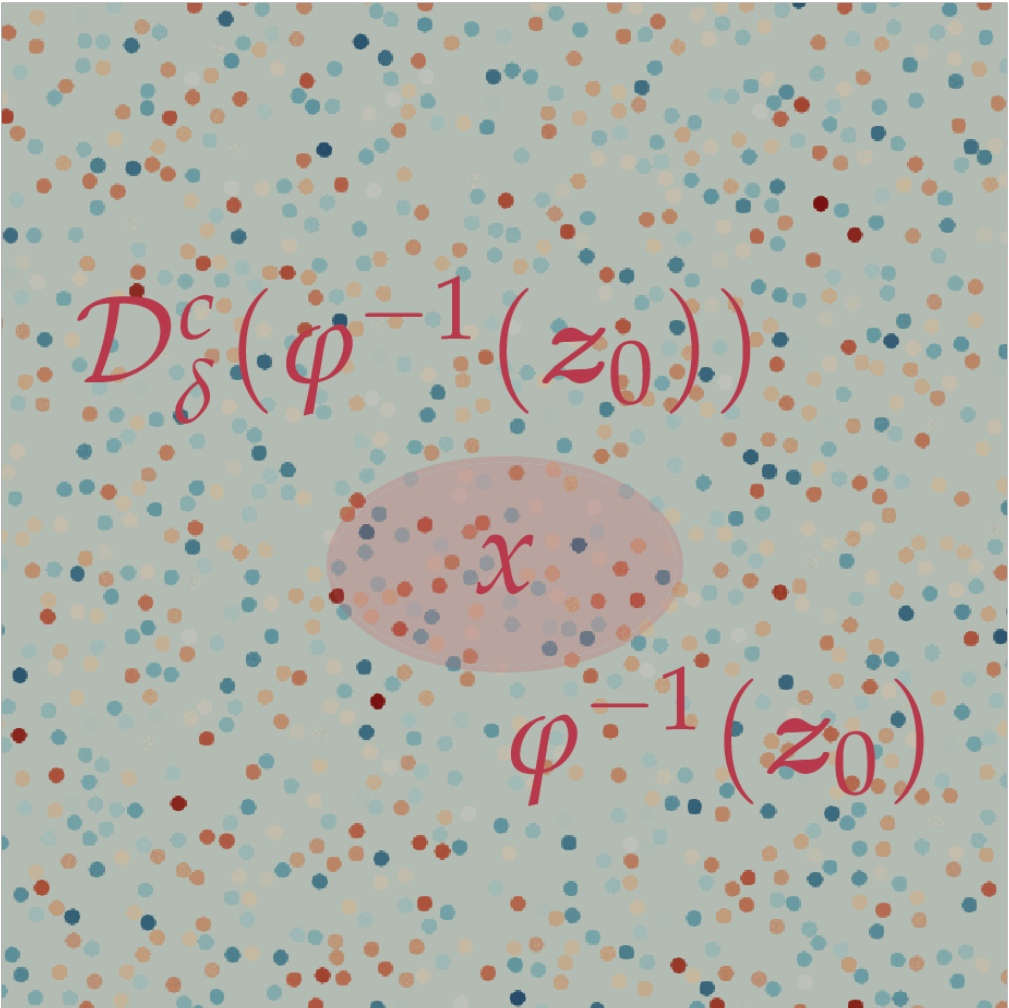
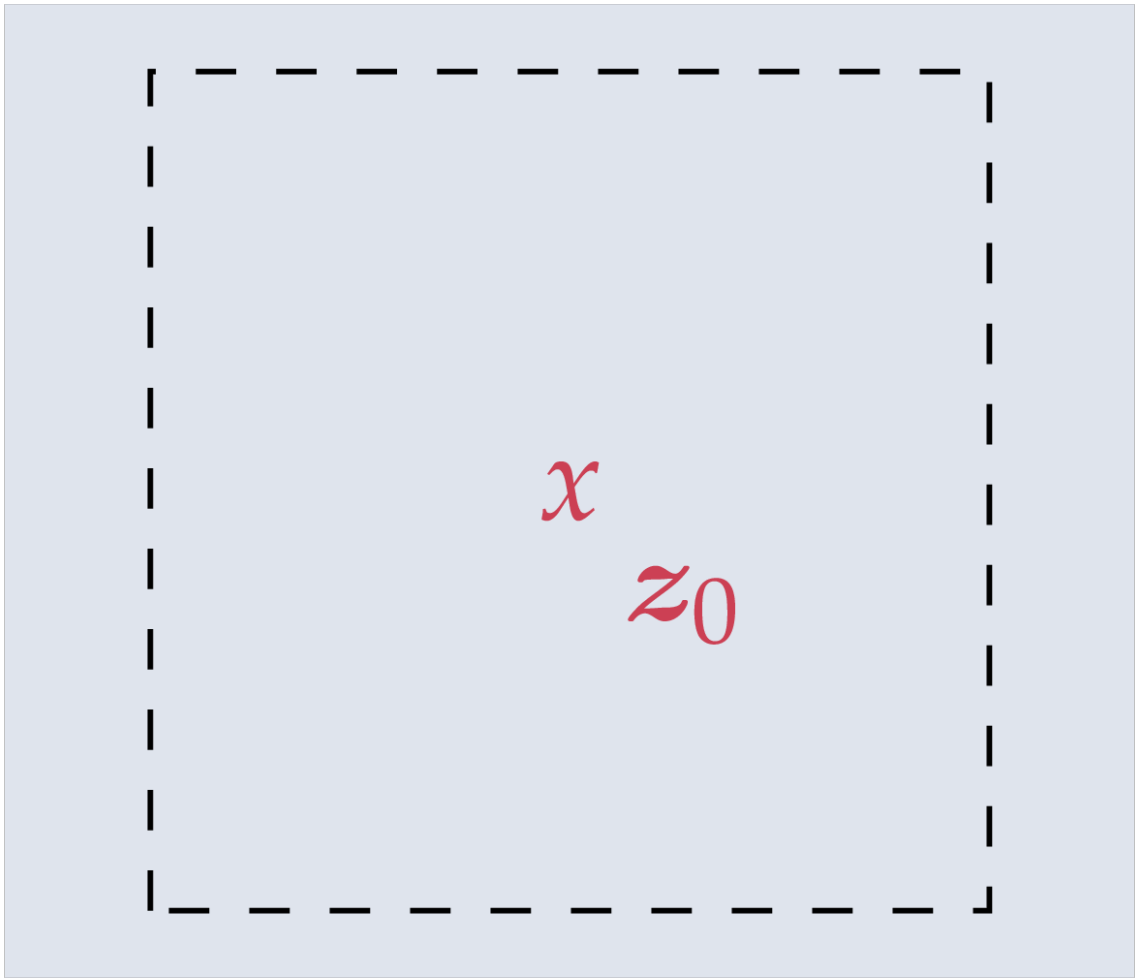
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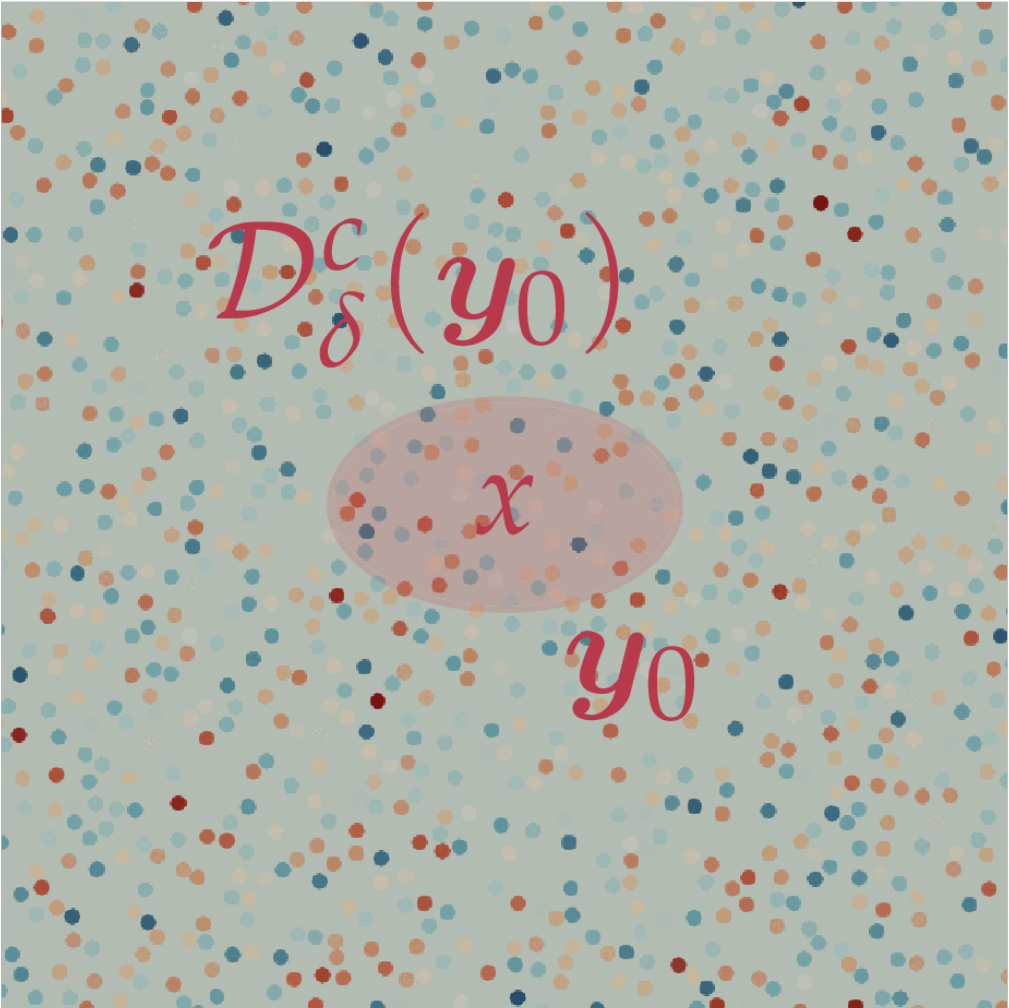
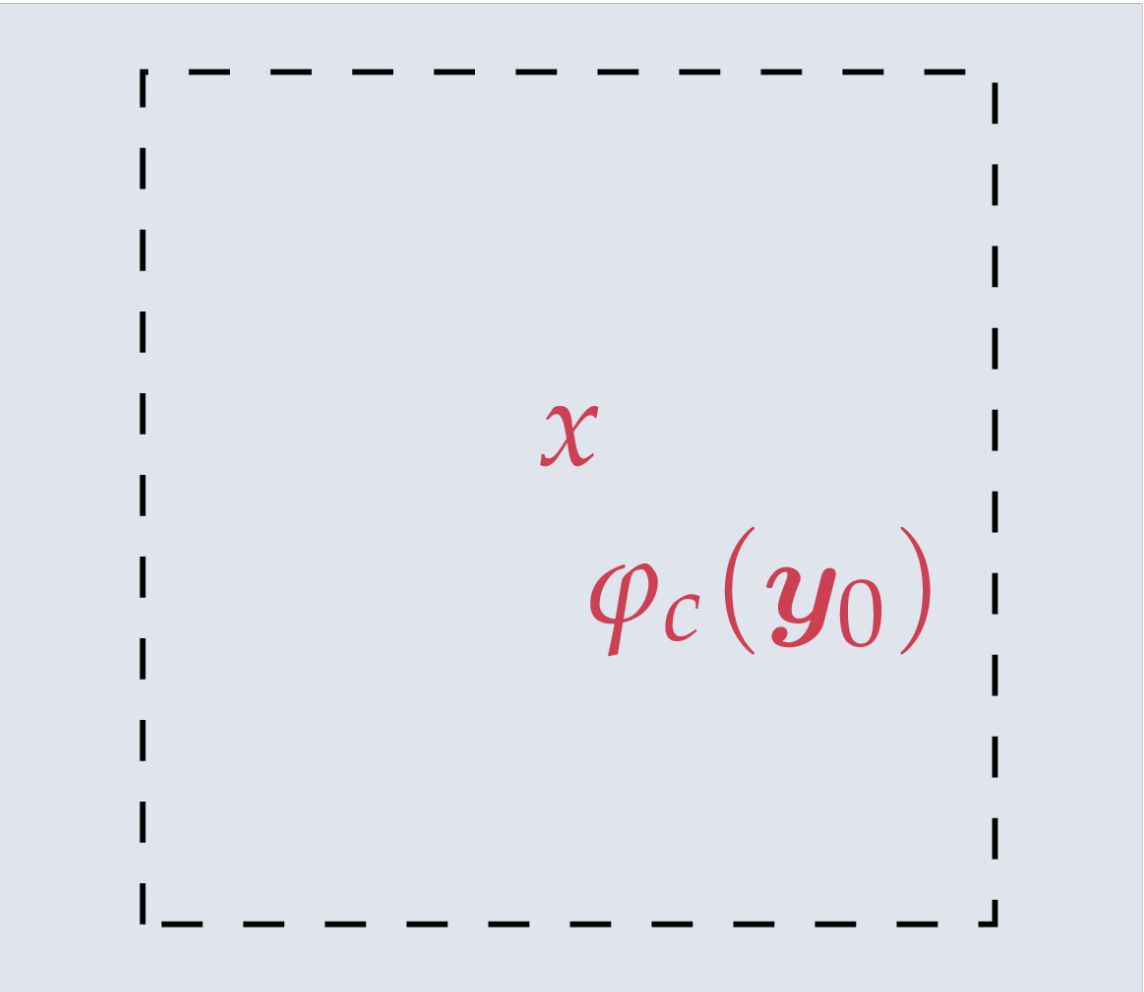
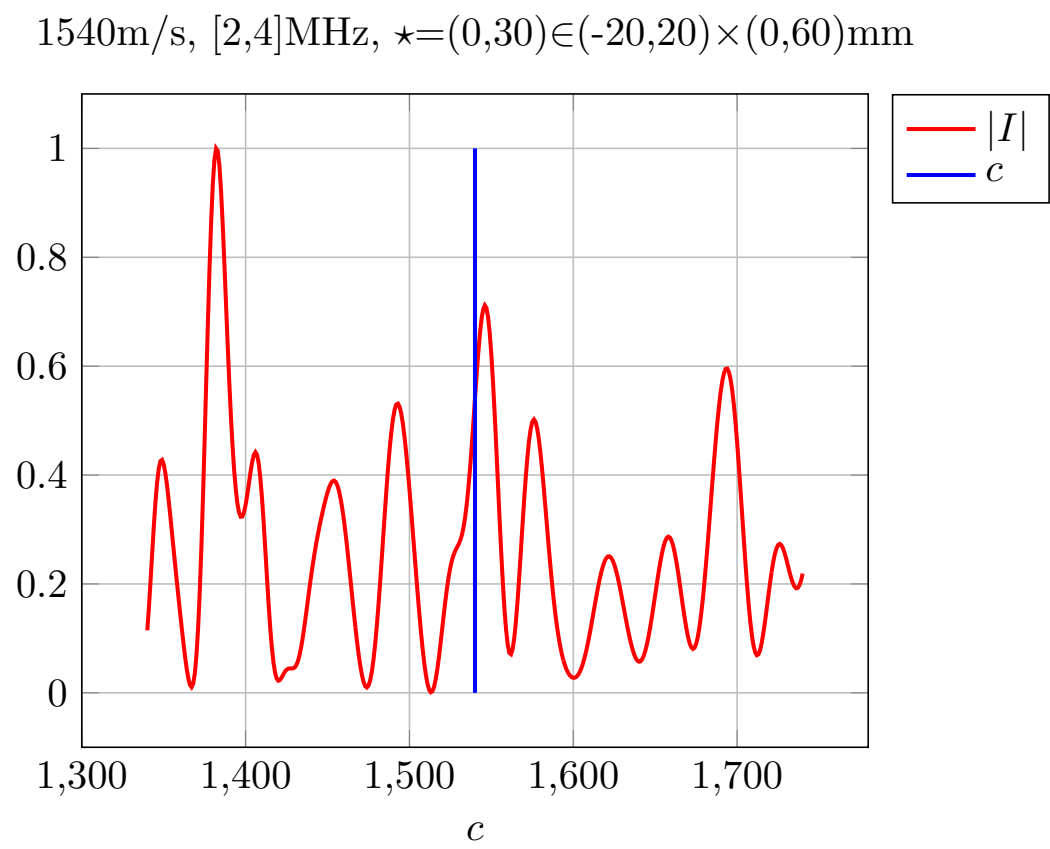


Moving focal spots

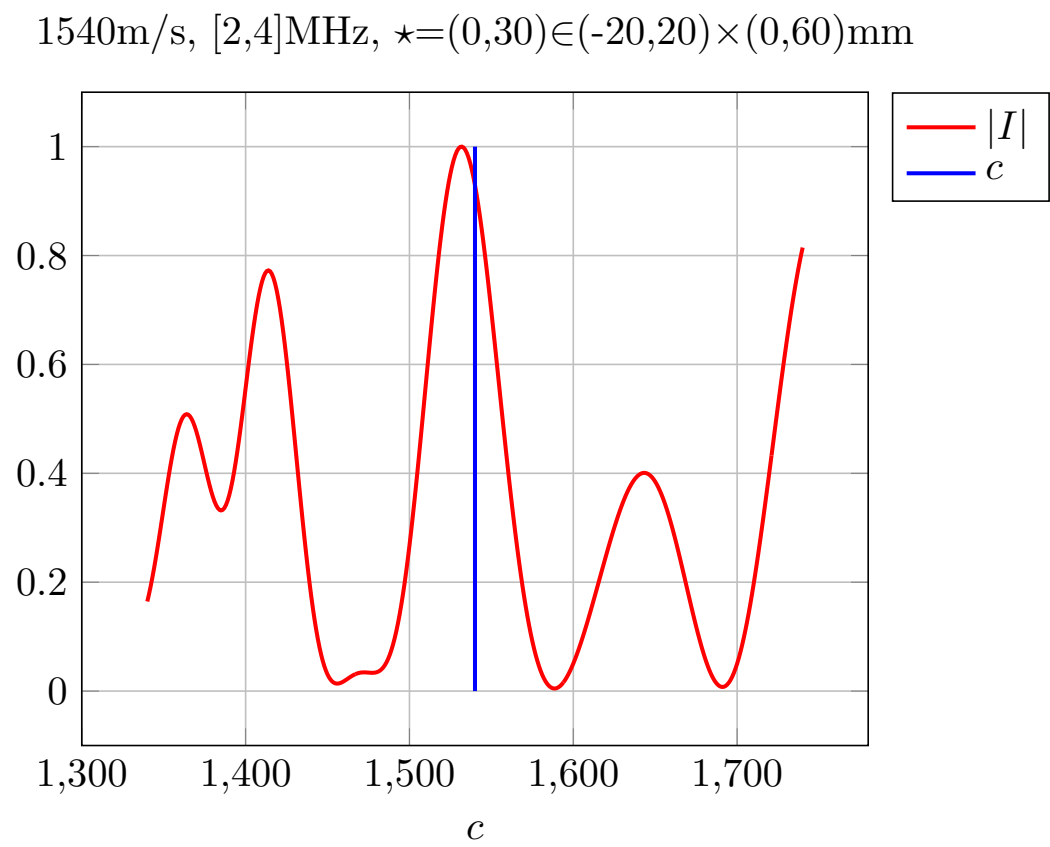
D' (Image)
 $c = 1.2 * c^{\star}$
 D (Physical domain)



$c \mapsto |I^c(z)|^2$



$c \mapsto |I^c(\varphi_c(y_0))|^2$



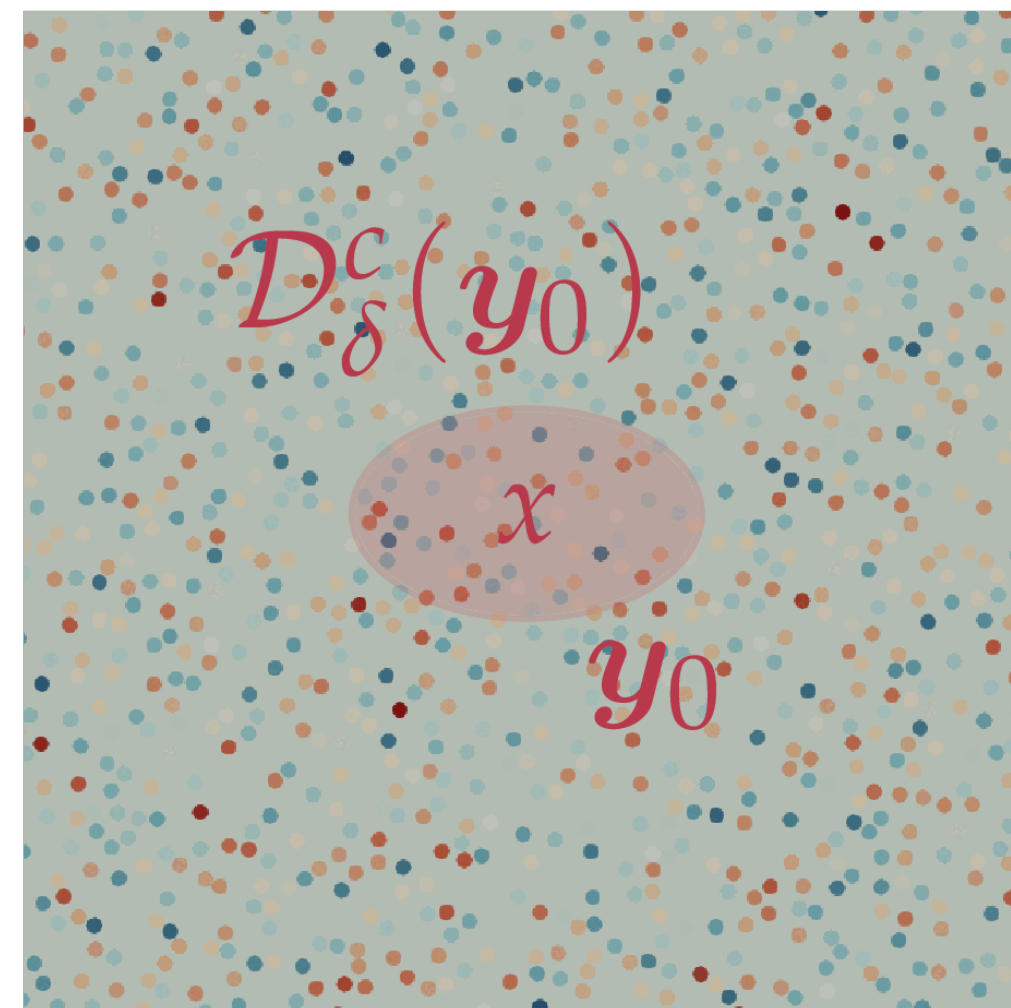
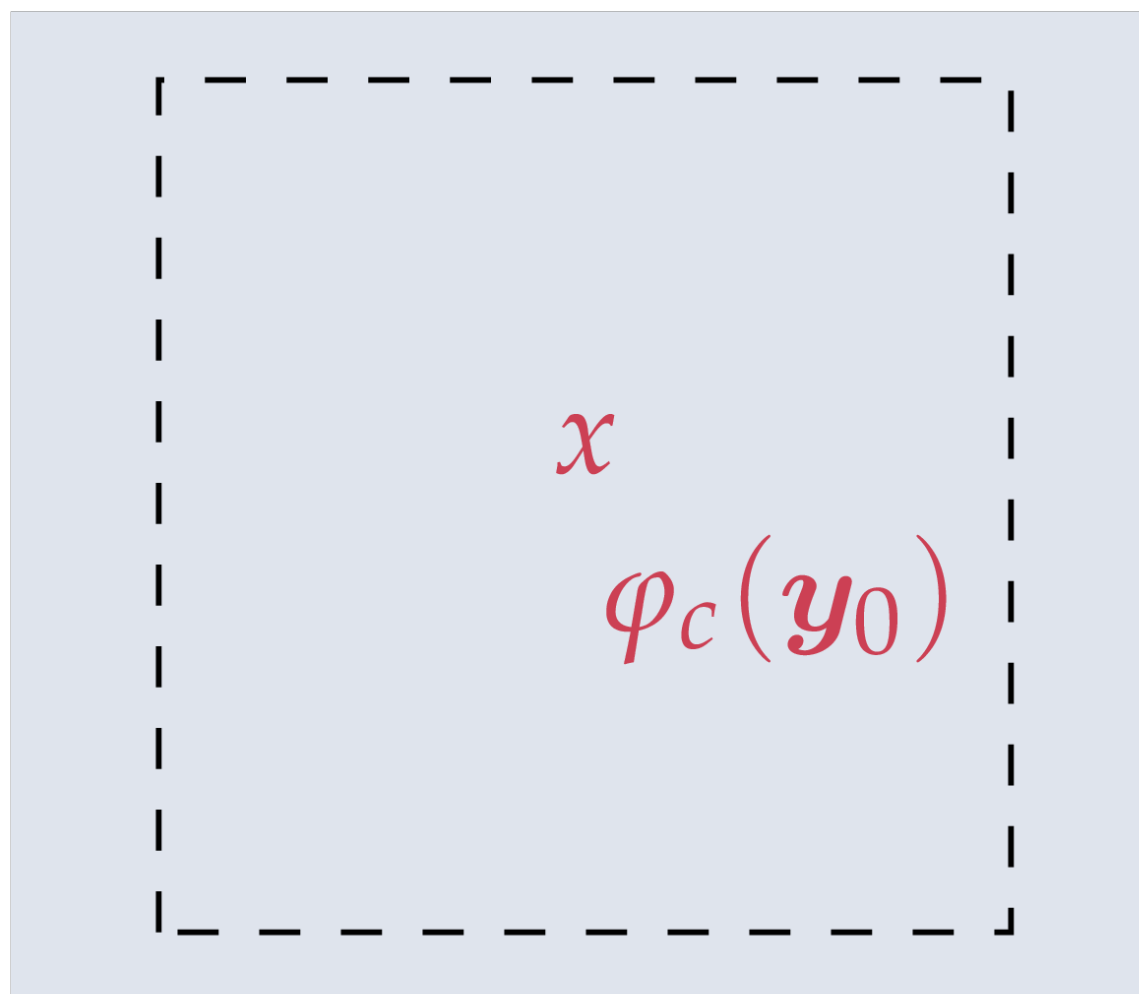
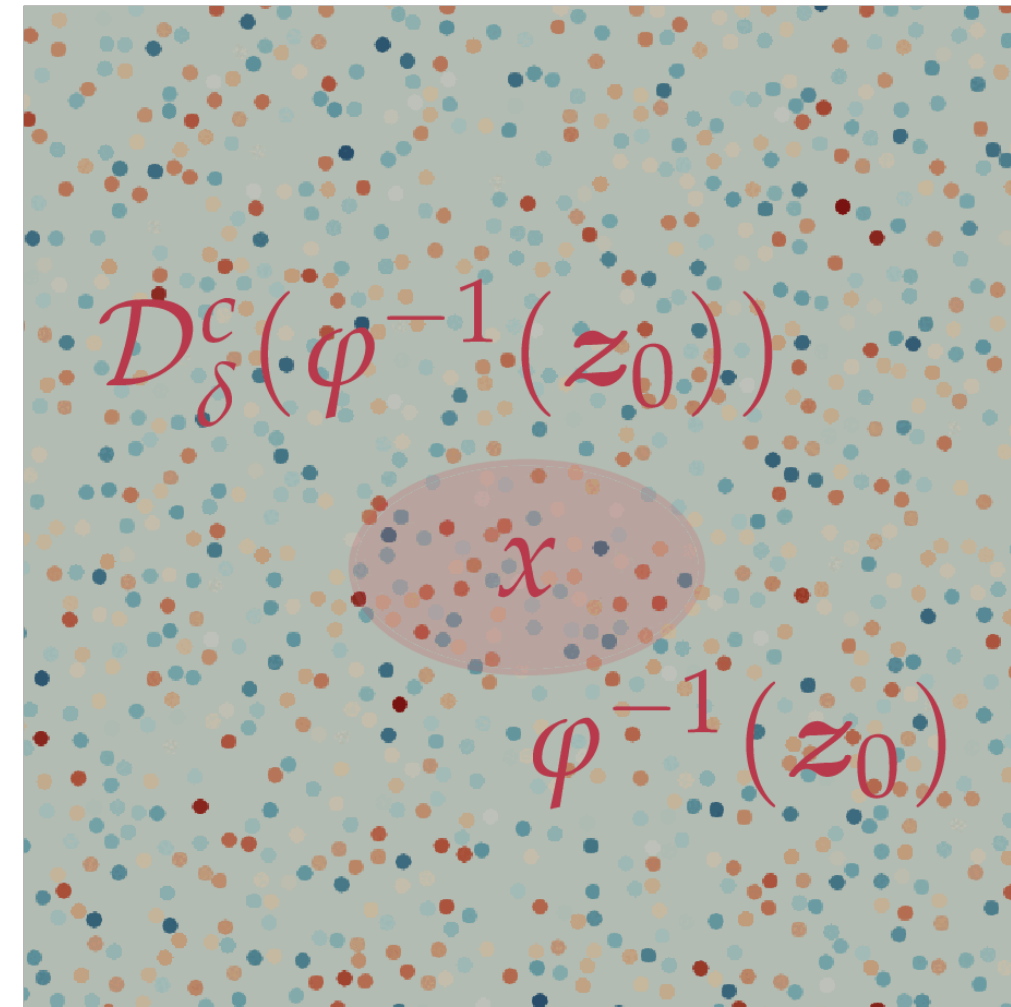
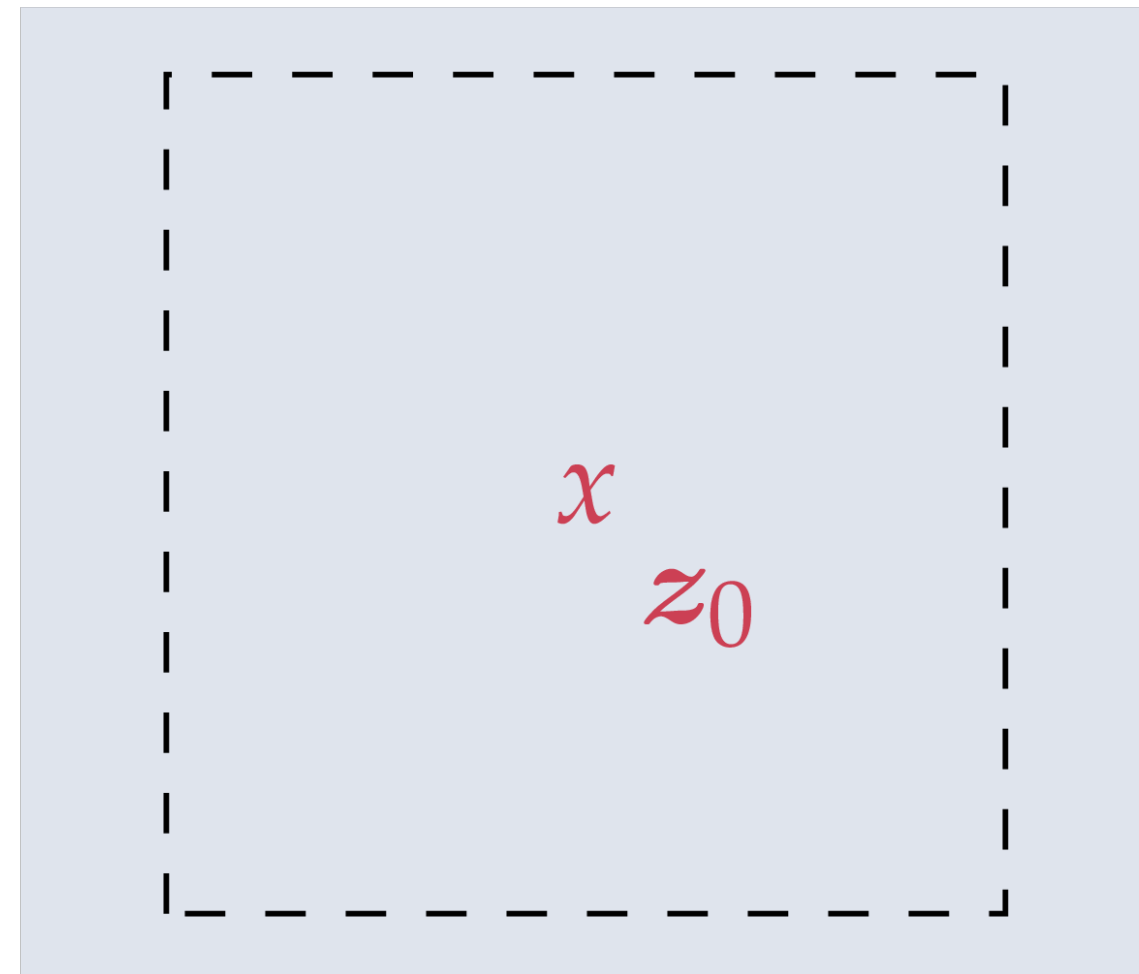
Moving focal spots

1 realization

20 realizations

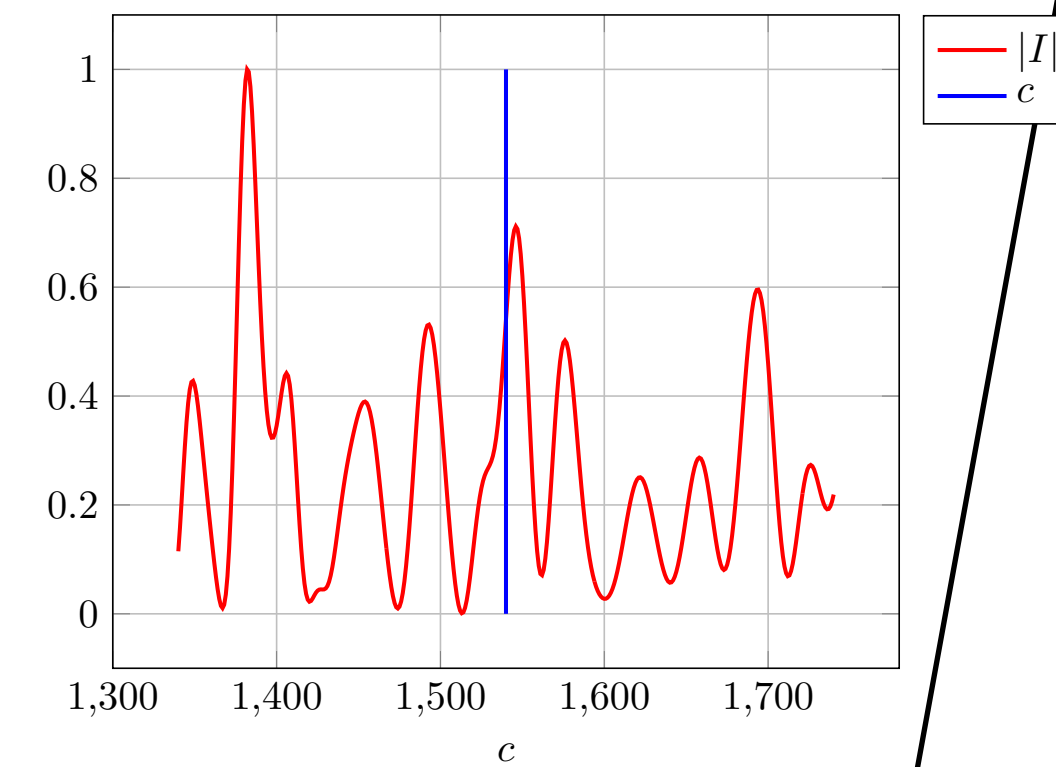
D' (Image)

$c = 1.2 * c^*$ D (Physical domain)



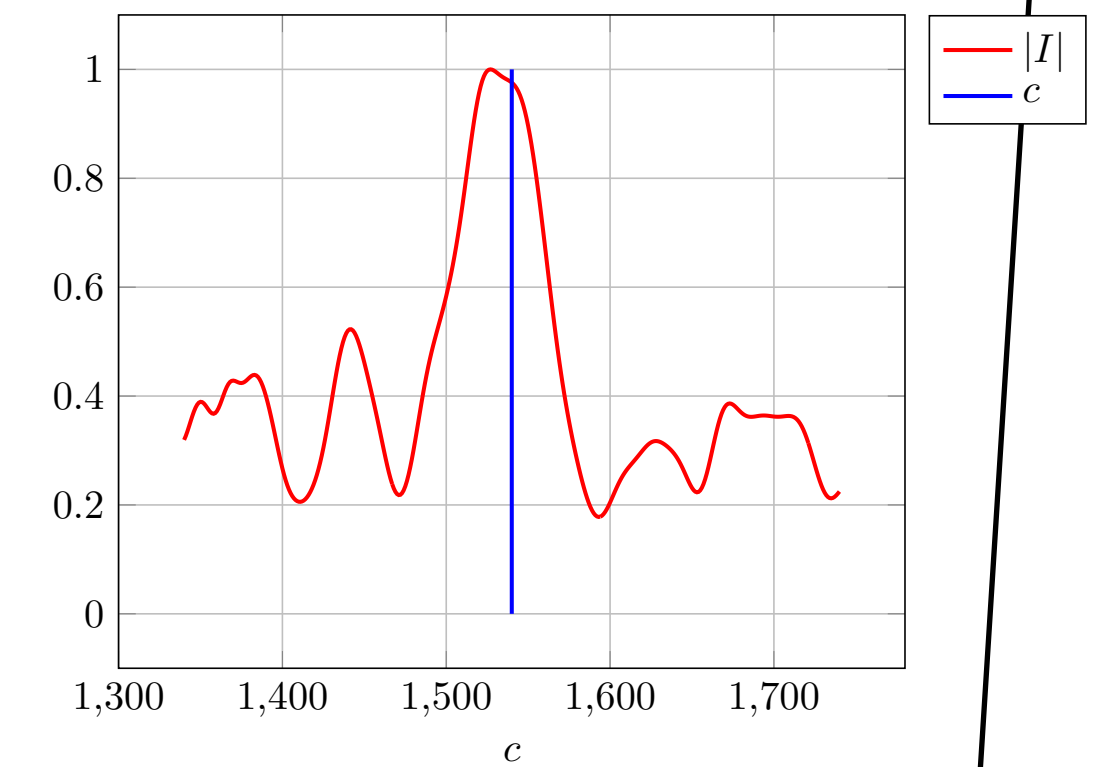
$c \mapsto |I^c(z)|^2$

1540m/s, [2,4]MHz, $\star=(0,30) \in (-20,20) \times (0,60)$ mm



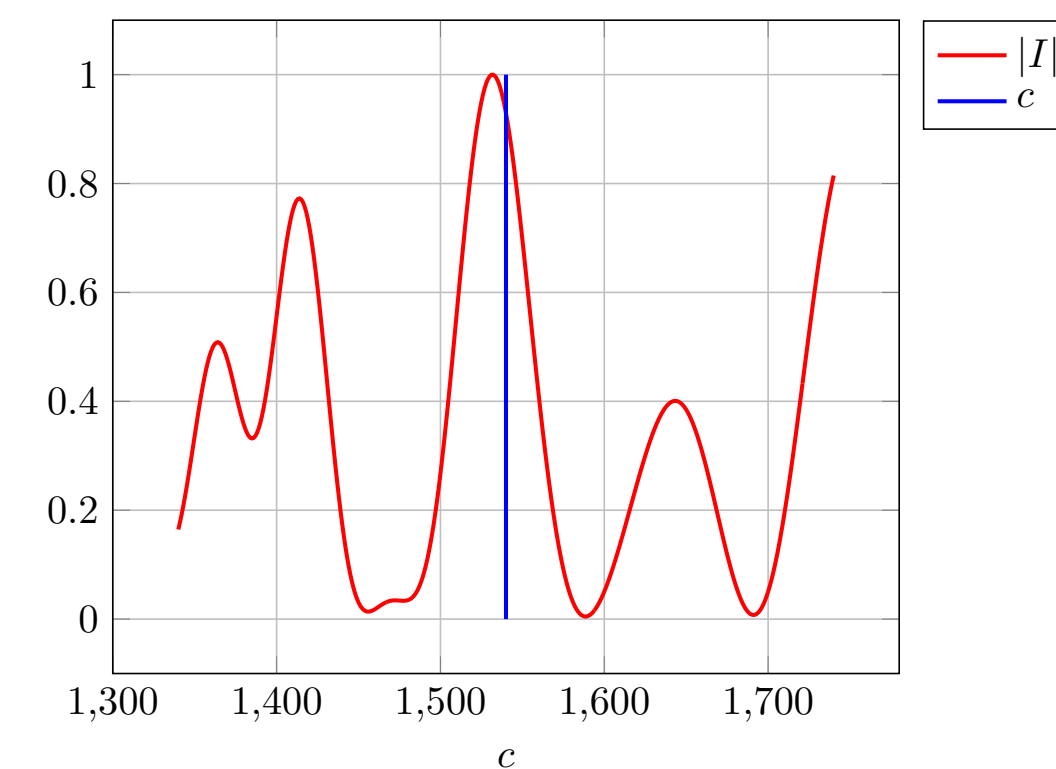
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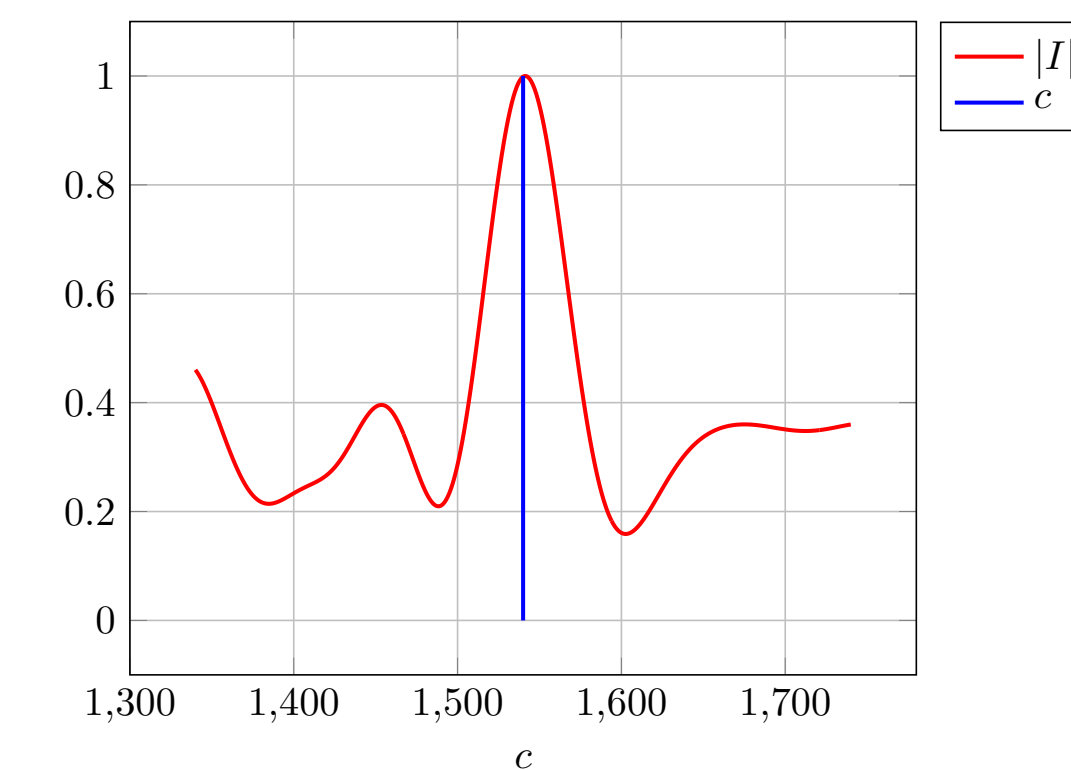
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Fixing the focal spot

Pick $t_0 \gg \omega_0^{-1}$ and consider $y_{t_0} := (0, c^* t_0)$  UNKNOWN point in the domain, only t_0 known

$\varphi_c(y_{t_0}) = (0, \frac{c}{c^*} y_{t_0}^{\parallel}) = (0, ct_0)$  Only depends on t_0 and c , KNOWN

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Theorem: Incoherent estimator

$$c^* = \operatorname{argmax}_c \mathbb{E} \left[I^c(z(c(t_0)))^2 \right] \quad \text{with} \quad z(c) = (0, ct_0)$$

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 Dual focal spot centered on y_{t_0}

 Point spread function

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Only one realization of the medium

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 Point spread function

Ensemble averaging via ergodicity

Denote by $n(\cdot, \gamma), \gamma \in \Omega$ the dependency on the randomness of the medium. Consider $\varepsilon \ll |\Delta z| \ll \frac{c}{\omega_0} \sim \frac{c^\star}{\omega_0}$.

Ensemble averaging via ergodicity

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Dual focal spot of z

Group action defining the ergodicity of the process

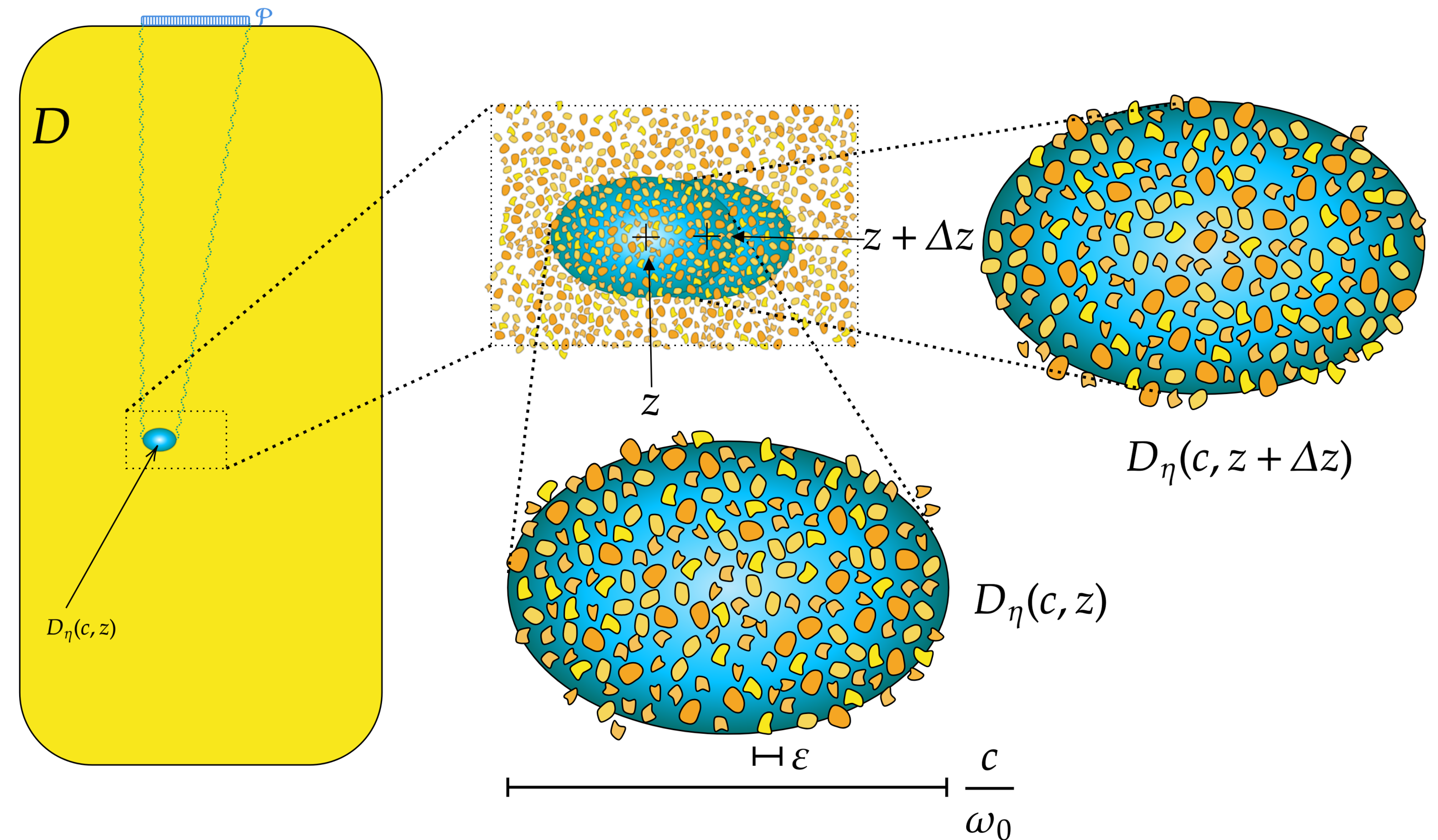
Slightly shifted dual focal spot of z

Ensemble averaging via ergodicity

Denote by $n(\cdot, \gamma), \gamma \in \Omega$ the dependency on the randomness of the medium. Consider $\varepsilon \ll |\Delta z| \ll \frac{c}{\omega_0} \sim \frac{c^*}{\omega_0}$.

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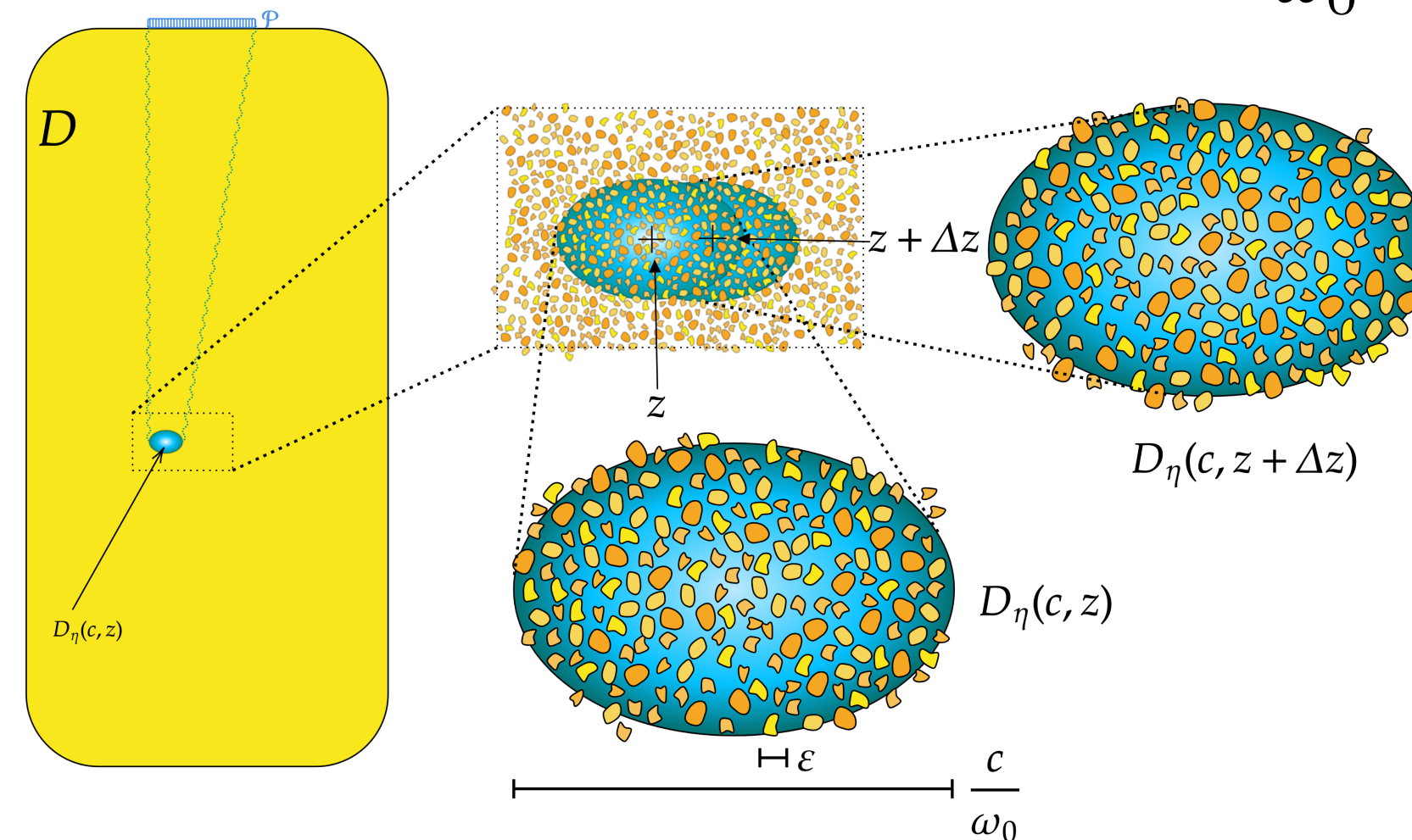


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For $\Delta z \in \mathbb{R}^d$ such that $\varepsilon \ll |\Delta z| \ll \frac{c^*}{\omega_0}$, there exists $\gamma' \in \Omega$ such that :

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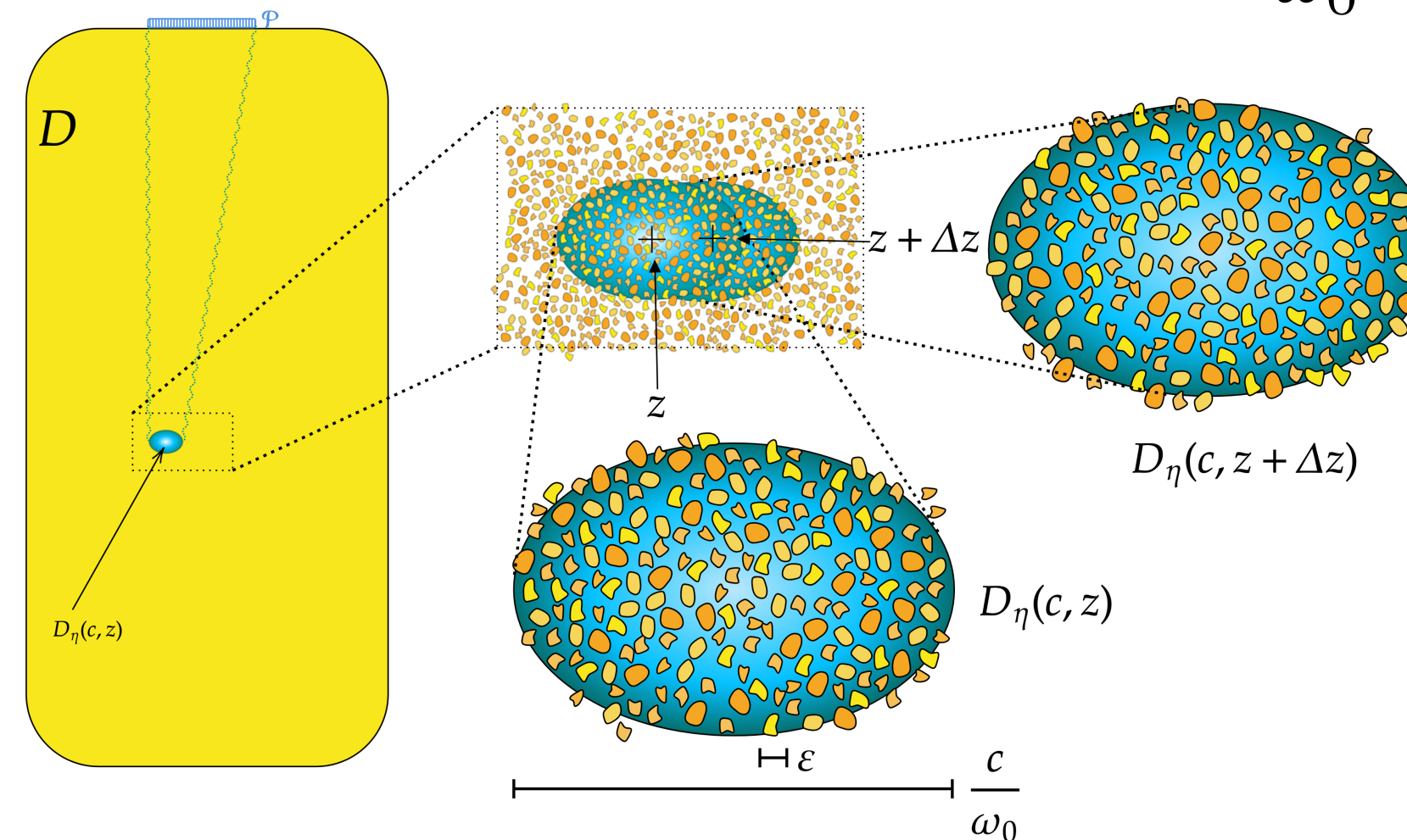
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Possible in practice to access statistics of I^c w/ one realization

Building the estimator in practice

Pick a travel time $t_0 \gg \omega_0^{-1}$.

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Define the set of possible values for c : $[c_{min}, c_{max}]$. Define the probing points $z(c) = (0, ct_0) \quad \forall c \in [c_{min}, c_{max}]$.

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Compute the matrix $\mathcal{K}_{ij} := |I^{c_j}(z(c_j) + (\Delta z)_i)|^2$

$\forall c_j \in [c_{min}, c_{max}]$

$\forall (\Delta z)_i \in \mathcal{S}$

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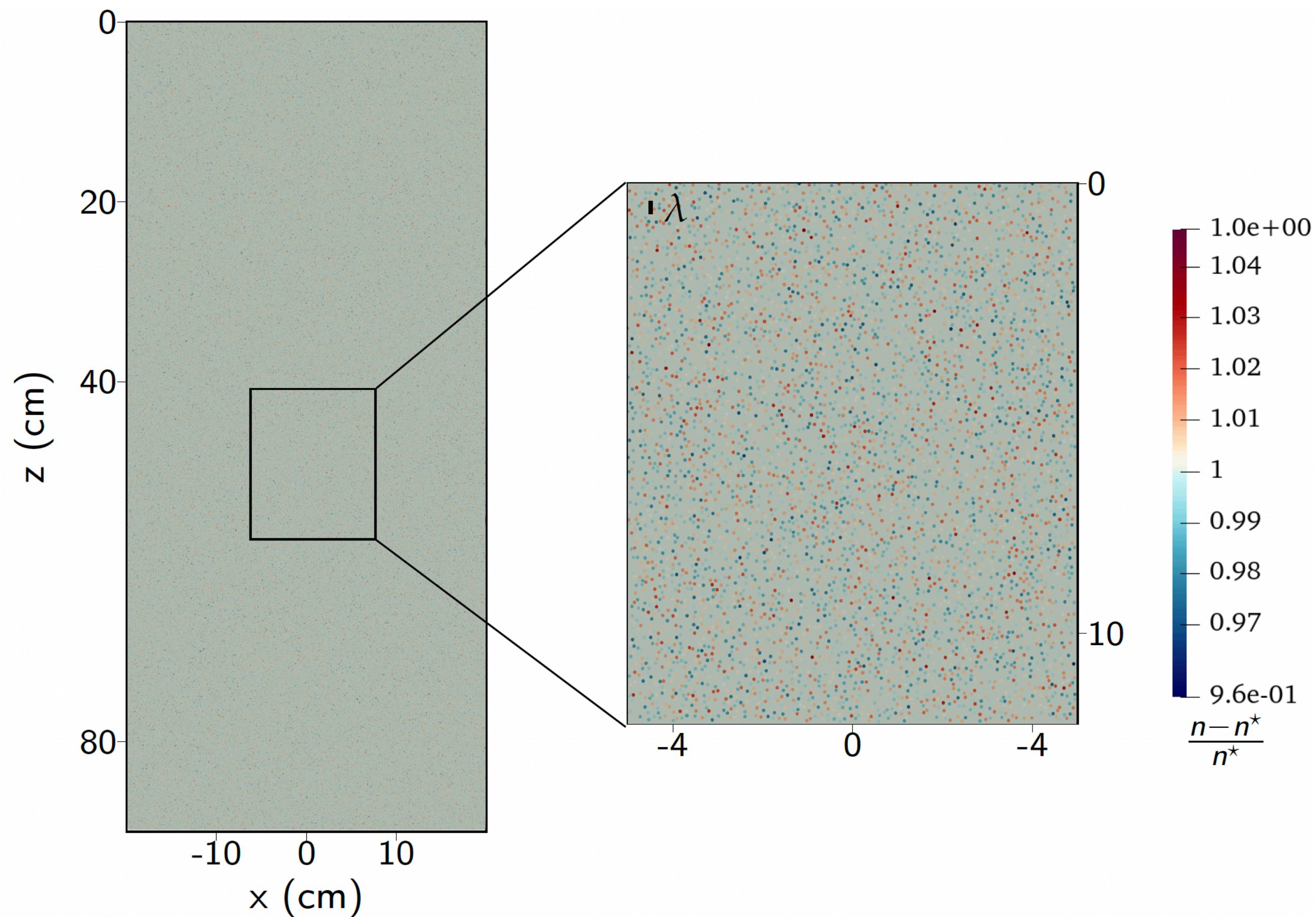
$\forall c_j \in [c_{min}, c_{max}]$

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Estimator

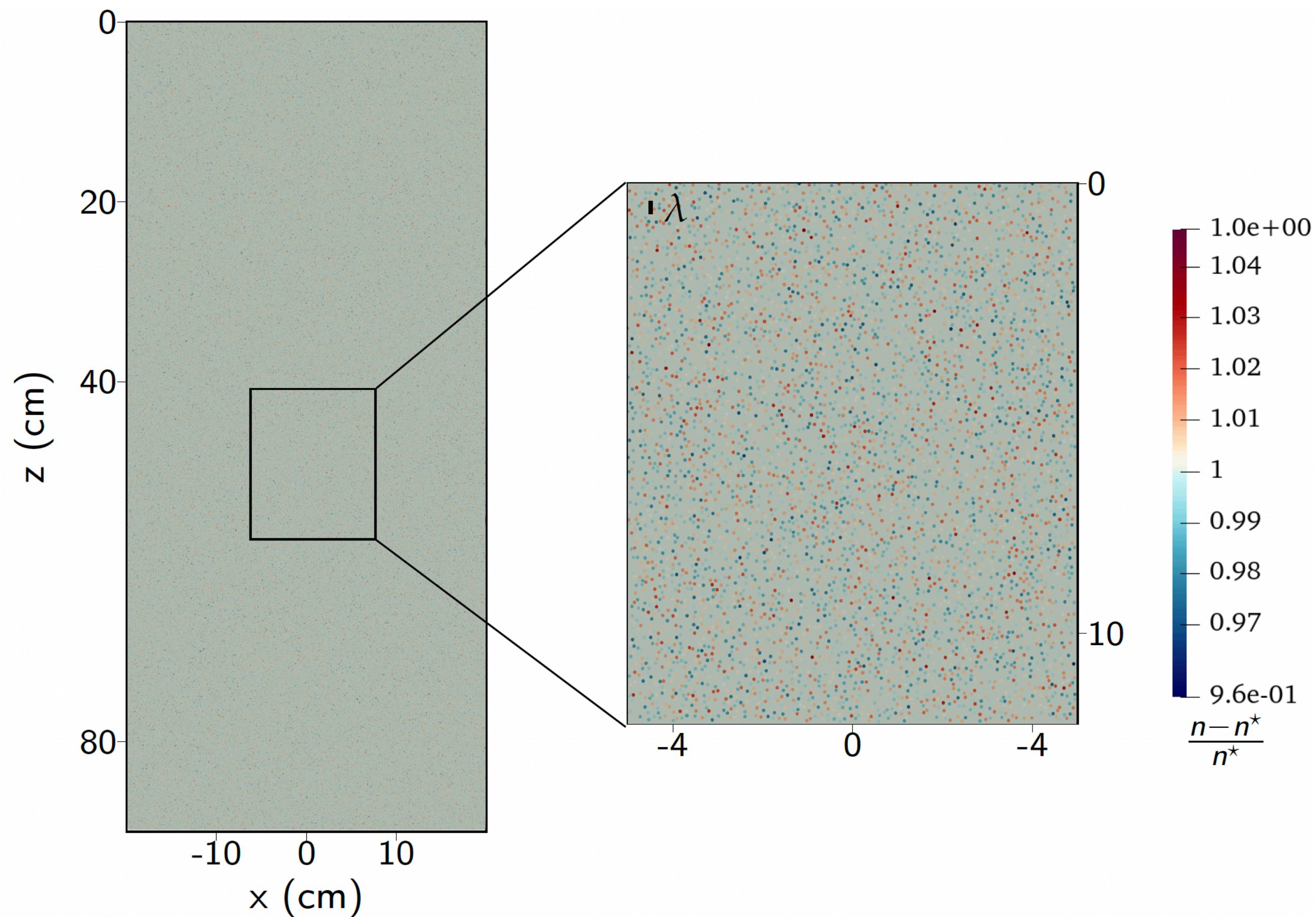
$$c^* = \operatorname{argmax}_j \sum_i \mathcal{K}_{i,j}$$

Numerical simulations (E. Parolin)



Simulations by E. Parolin (Alpines, INRIA)
166864 scatterers, $\varepsilon = 38.8\mu m$, $f = 4Mhz$.

Numerical simulations (E. Parolin)

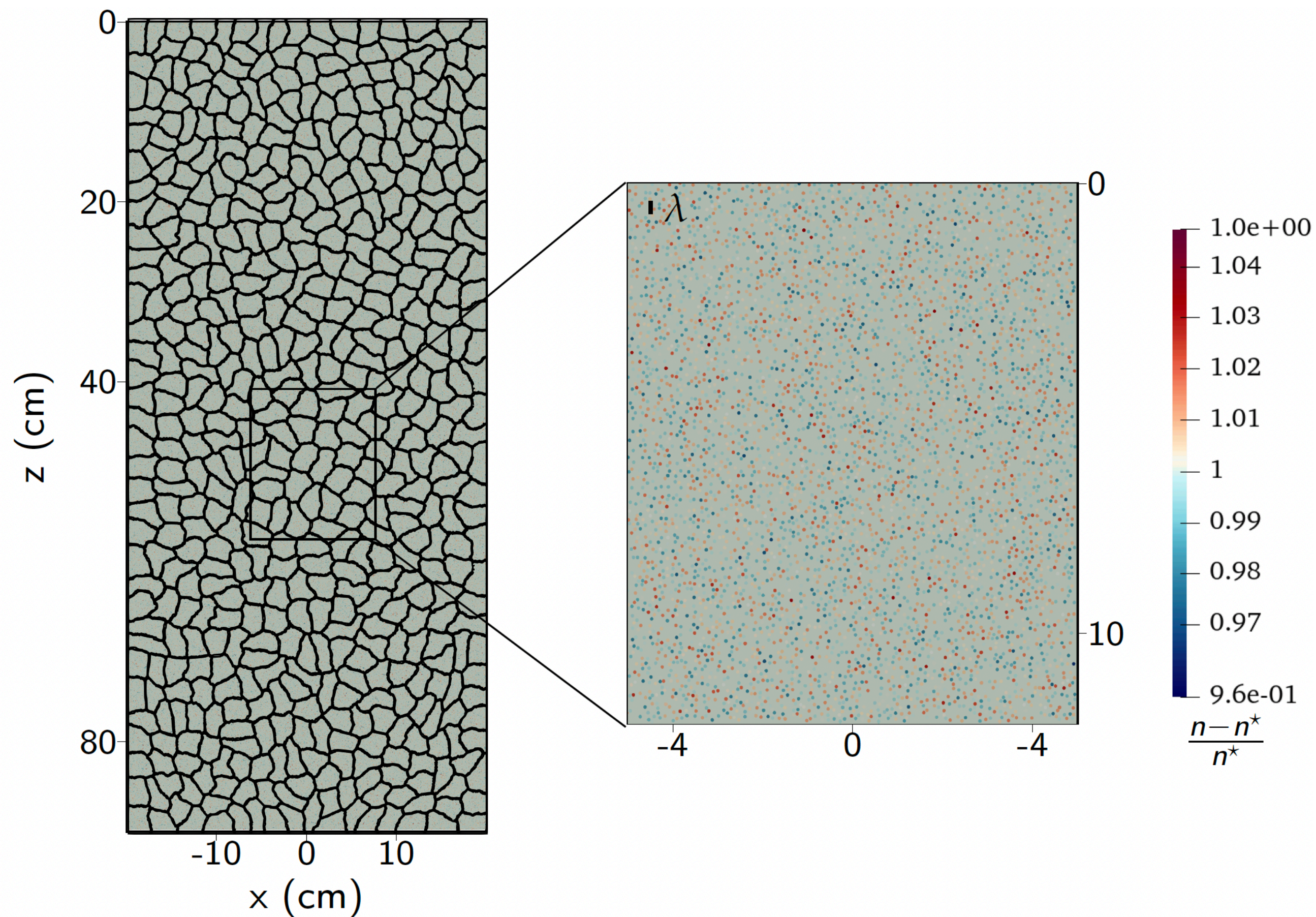


Parameters of the simulation

Discretisation: 108 DOFs (P3),
Preconditioner: one-level DD method (ORAS) with 512 subdomains,
Solver: 164 GMRES iterations for a 10^{-4} residual tolerance
Computation time: ~ 5 min on INRIA Paris' supercomputer.
implemented with Freefem++.

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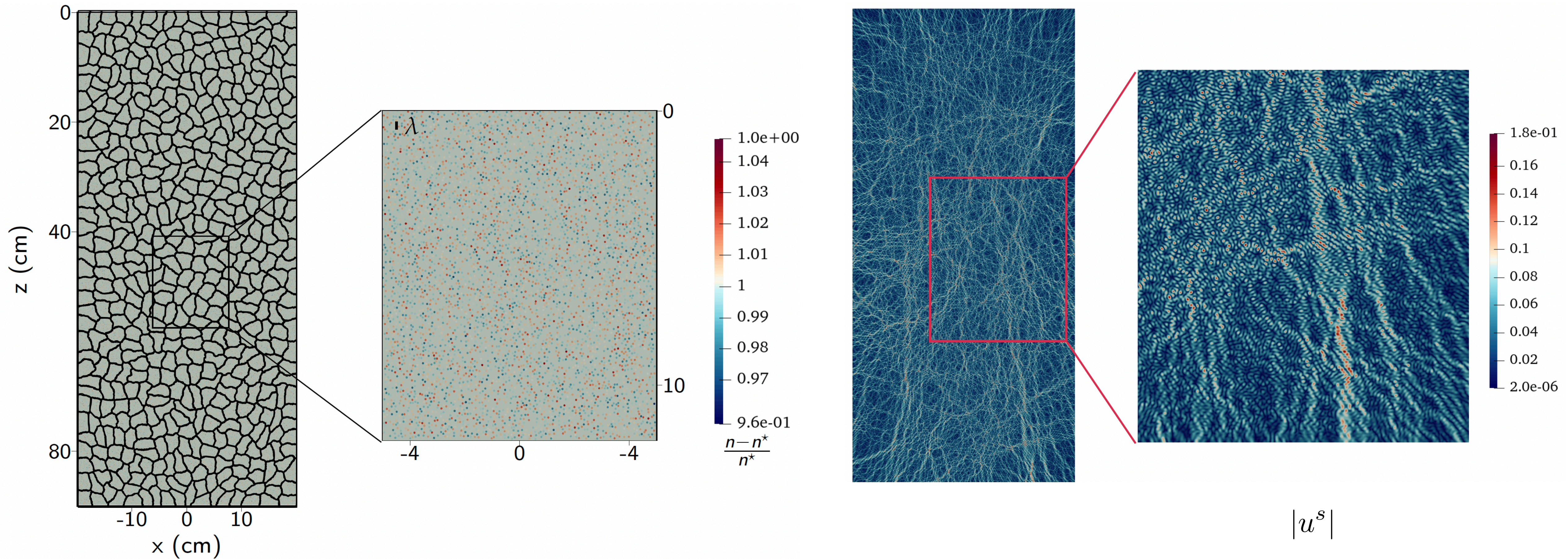


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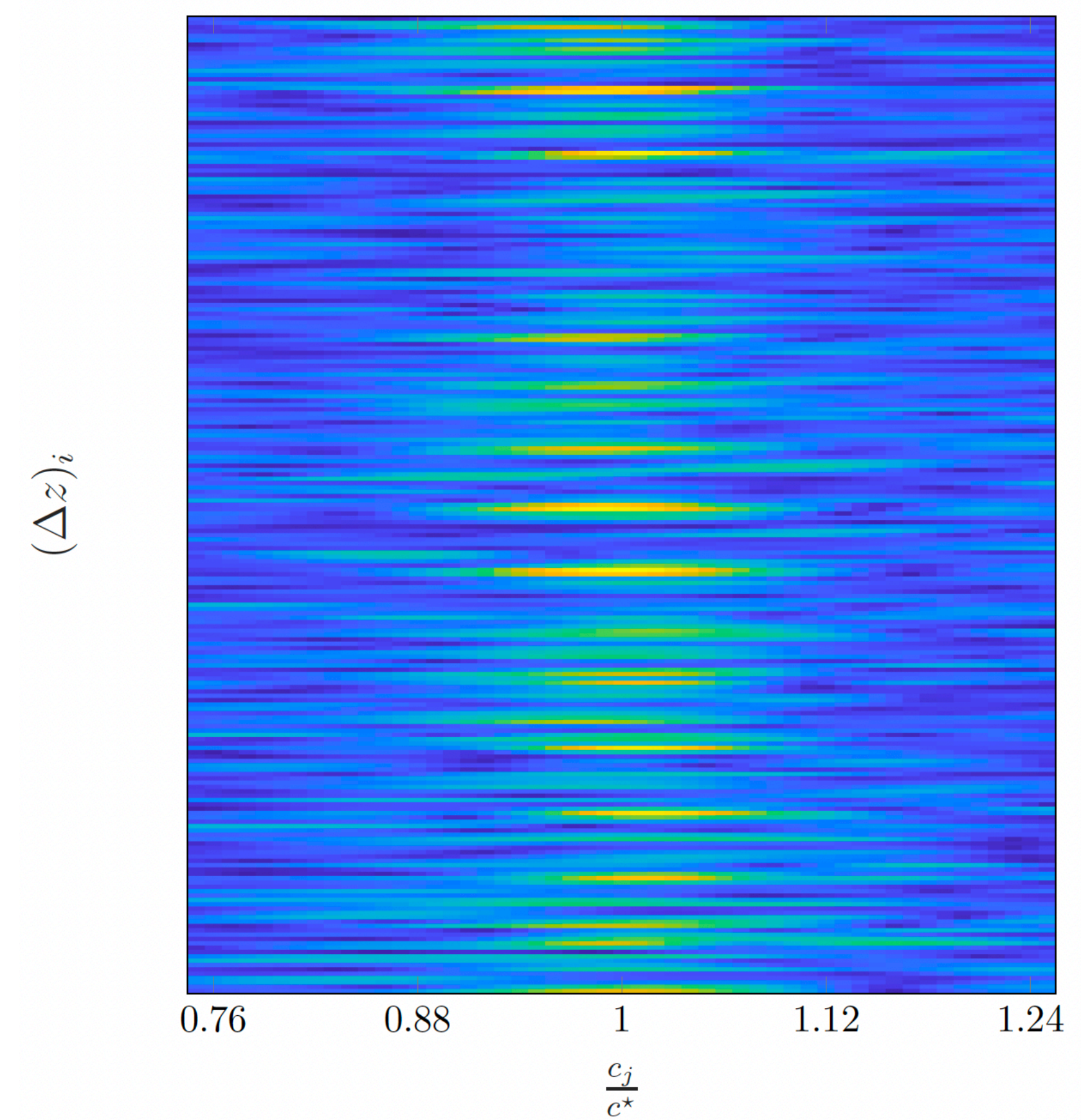
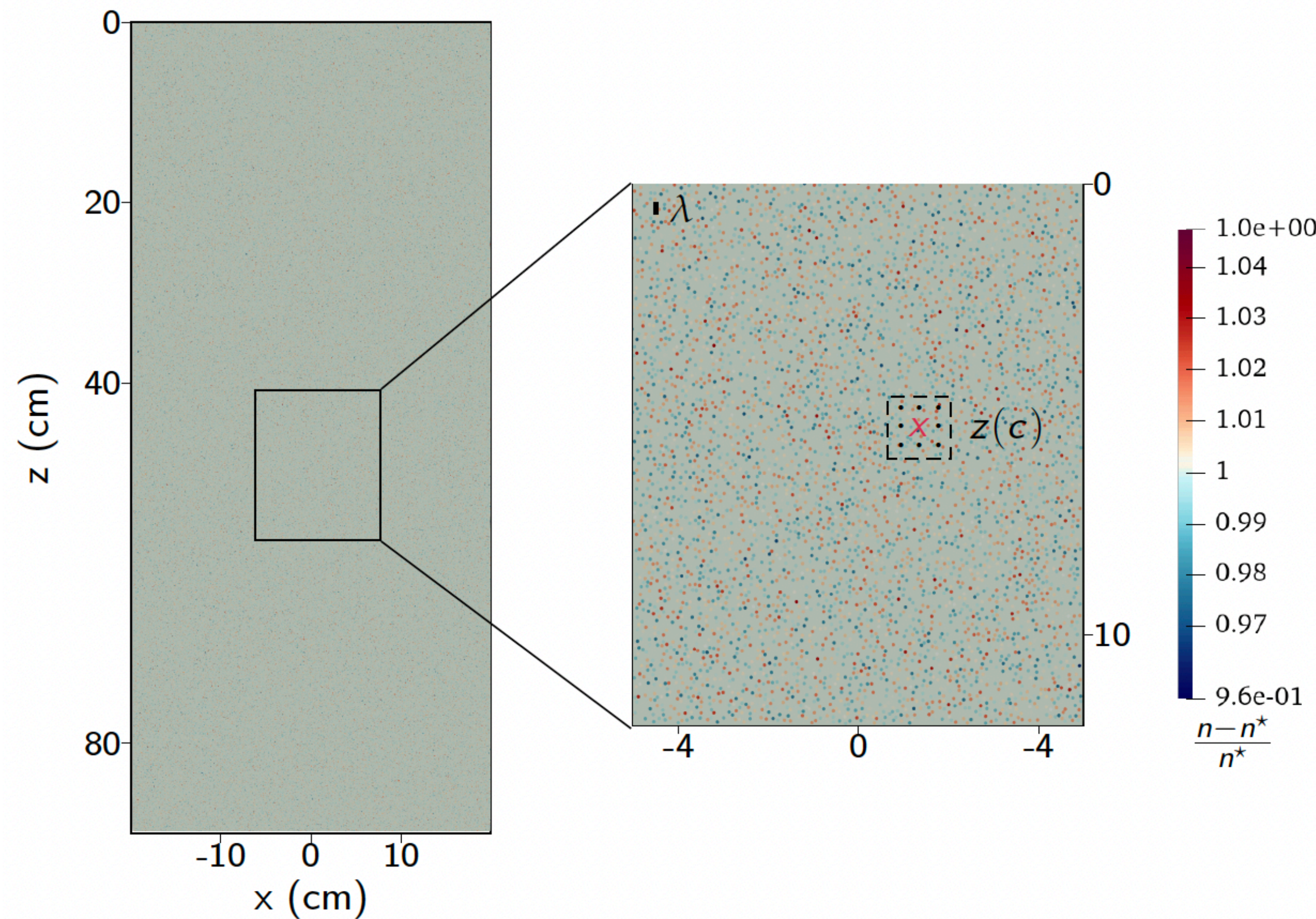
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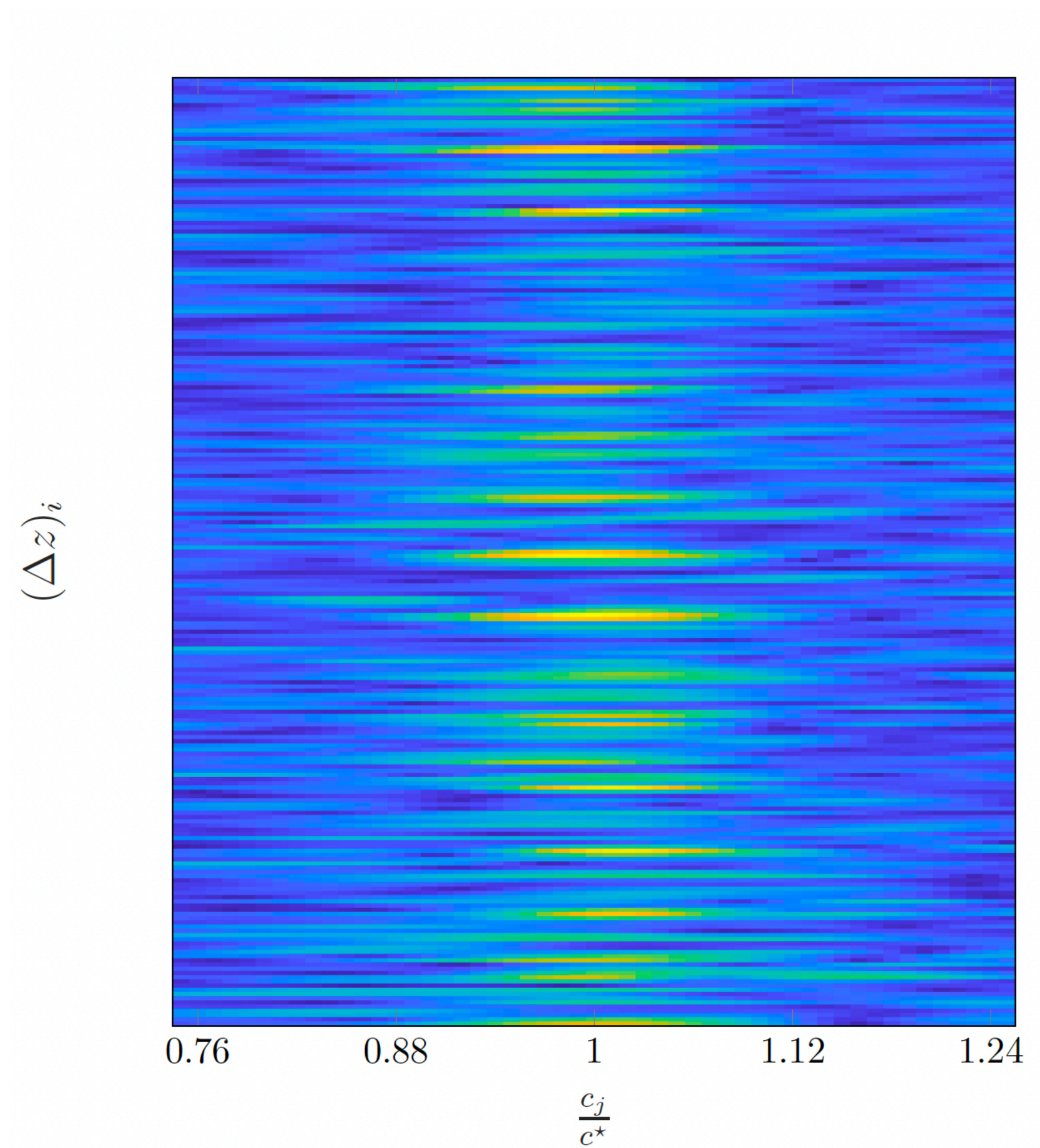
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Spatial averaging for a fixed realization



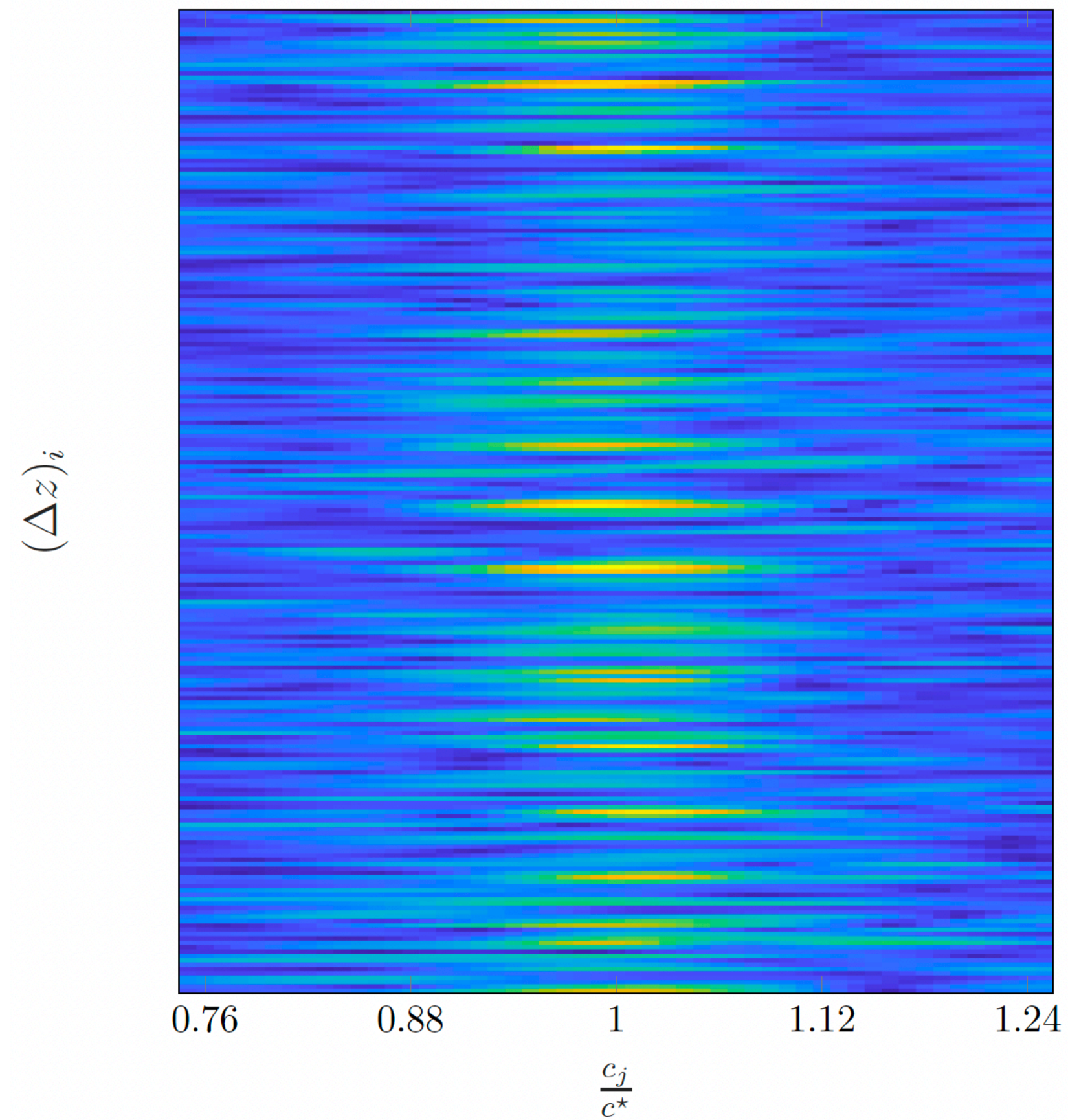
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Spatial averaging for a fixed realization

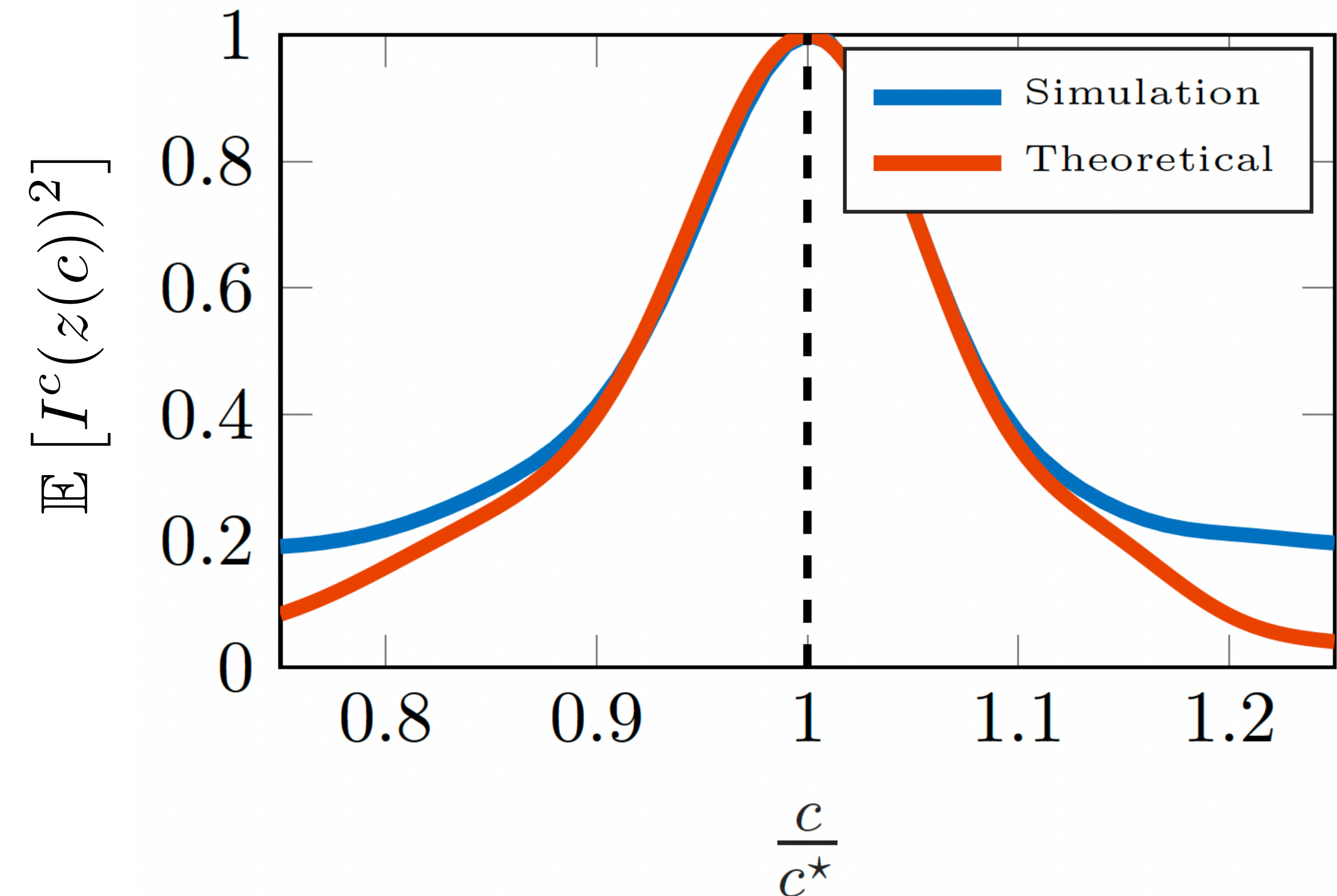


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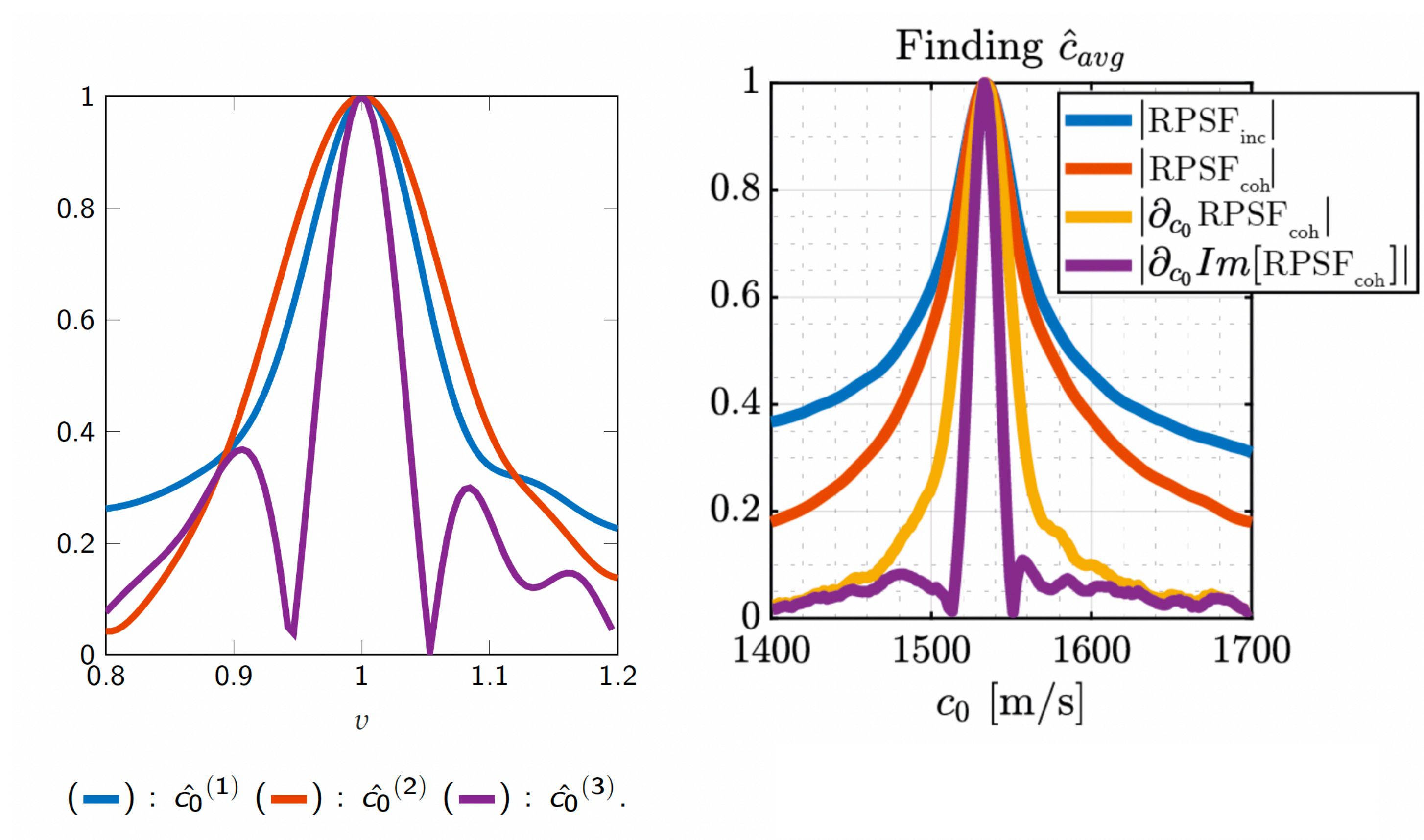
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Comparison with experiments



Comparison with experiments

Propagation of ultrasounds in random multi-scale media and effective speed of sound estimation

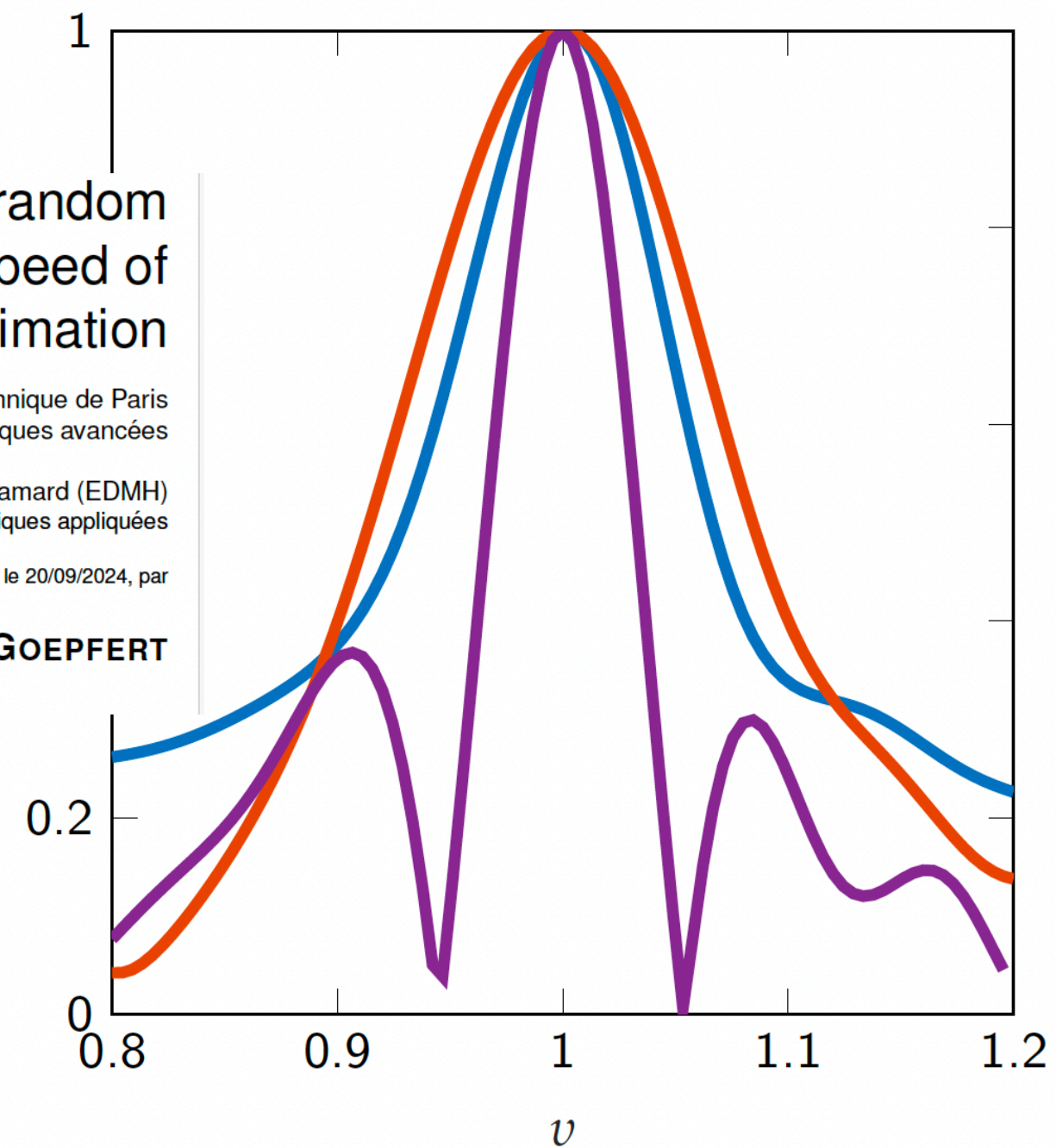
Thèse de doctorat de l'Institut Polytechnique de Paris
préparée à l'École nationale supérieure de techniques avancées

École doctorale n°574 École doctorale de mathématiques Hadamard (EDMH)
Spécialité de doctorat : Mathématiques appliquées

Thèse présentée et soutenue à Palaiseau, le 20/09/2024, par

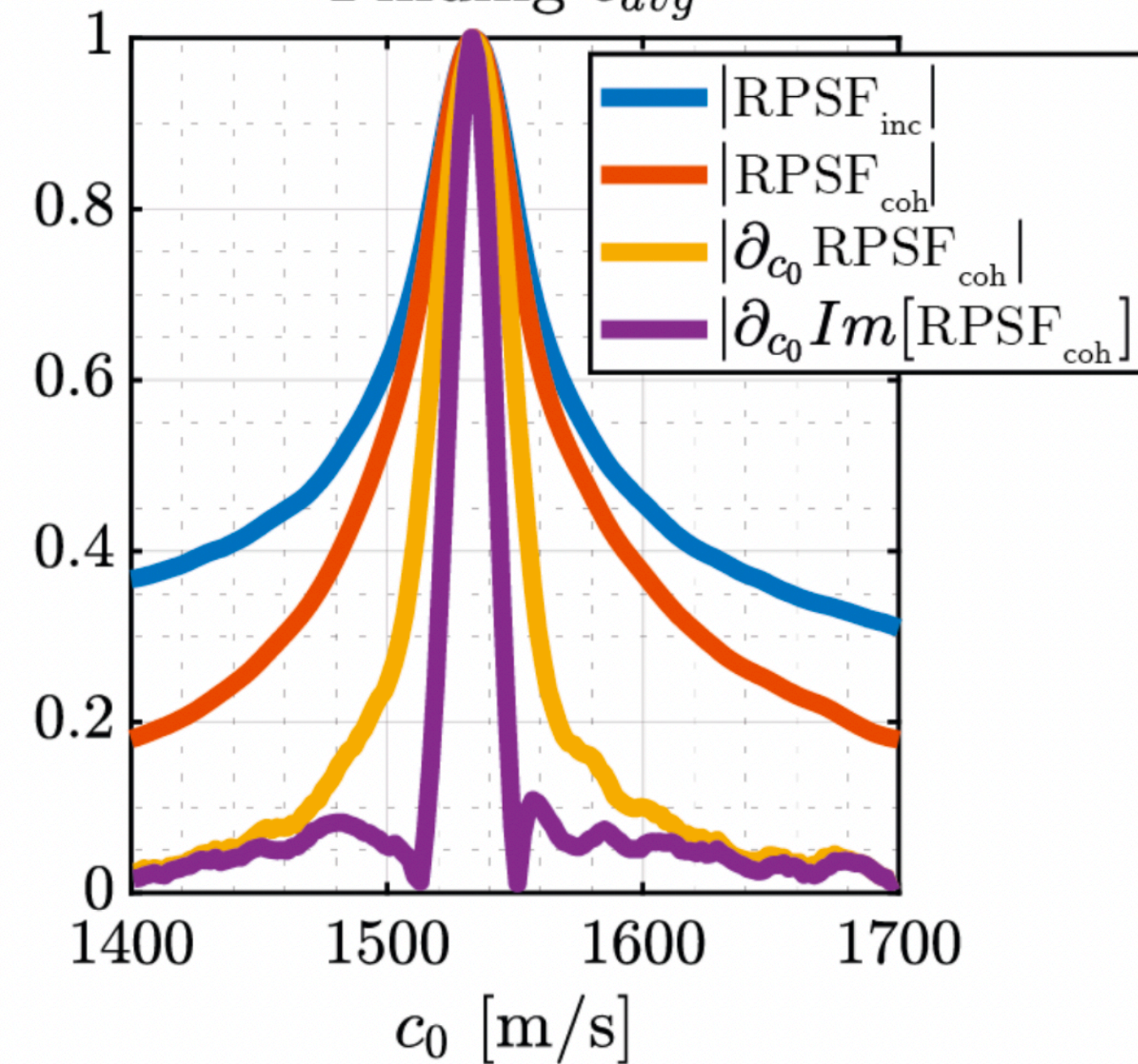
QUENTIN GOEPFERT

Numerical simulations



(—) : $\hat{c}_0^{(1)}$ (—) : $\hat{c}_0^{(2)}$ (—) : $\hat{c}_0^{(3)}$.

Finding $\hat{c}_{avg}$



Comparison with experiments

Propagation of ultrasounds in random multi-scale media and effective speed of sound estimation

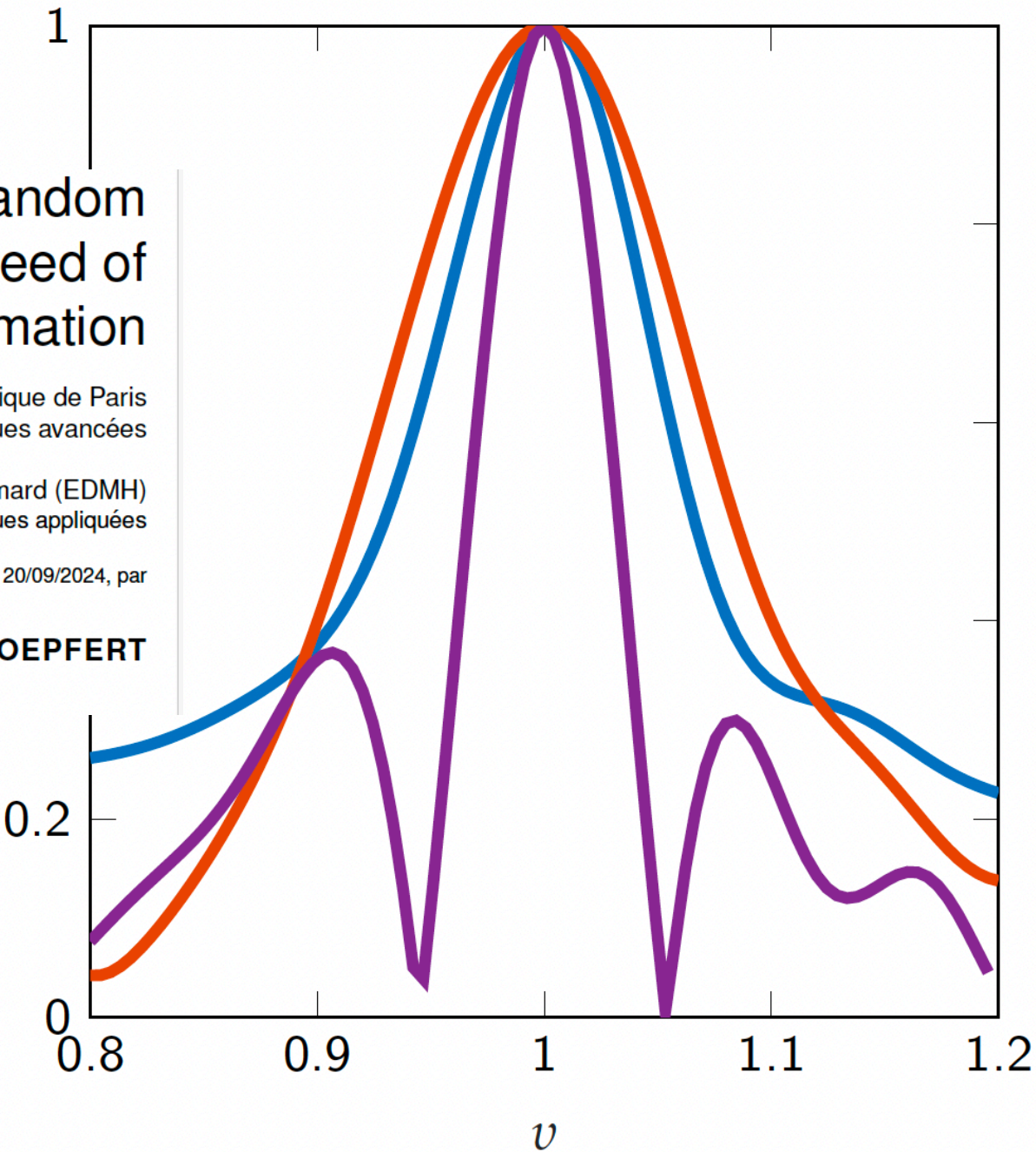
Thèse de doctorat de l'Institut Polytechnique de Paris
préparée à l'École nationale supérieure de techniques avancées

École doctorale n°574 École doctorale de mathématiques Hadamard (EDMH)
Spécialité de doctorat : Mathématiques appliquées

Thèse présentée et soutenue à Palaiseau, le 20/09/2024, par

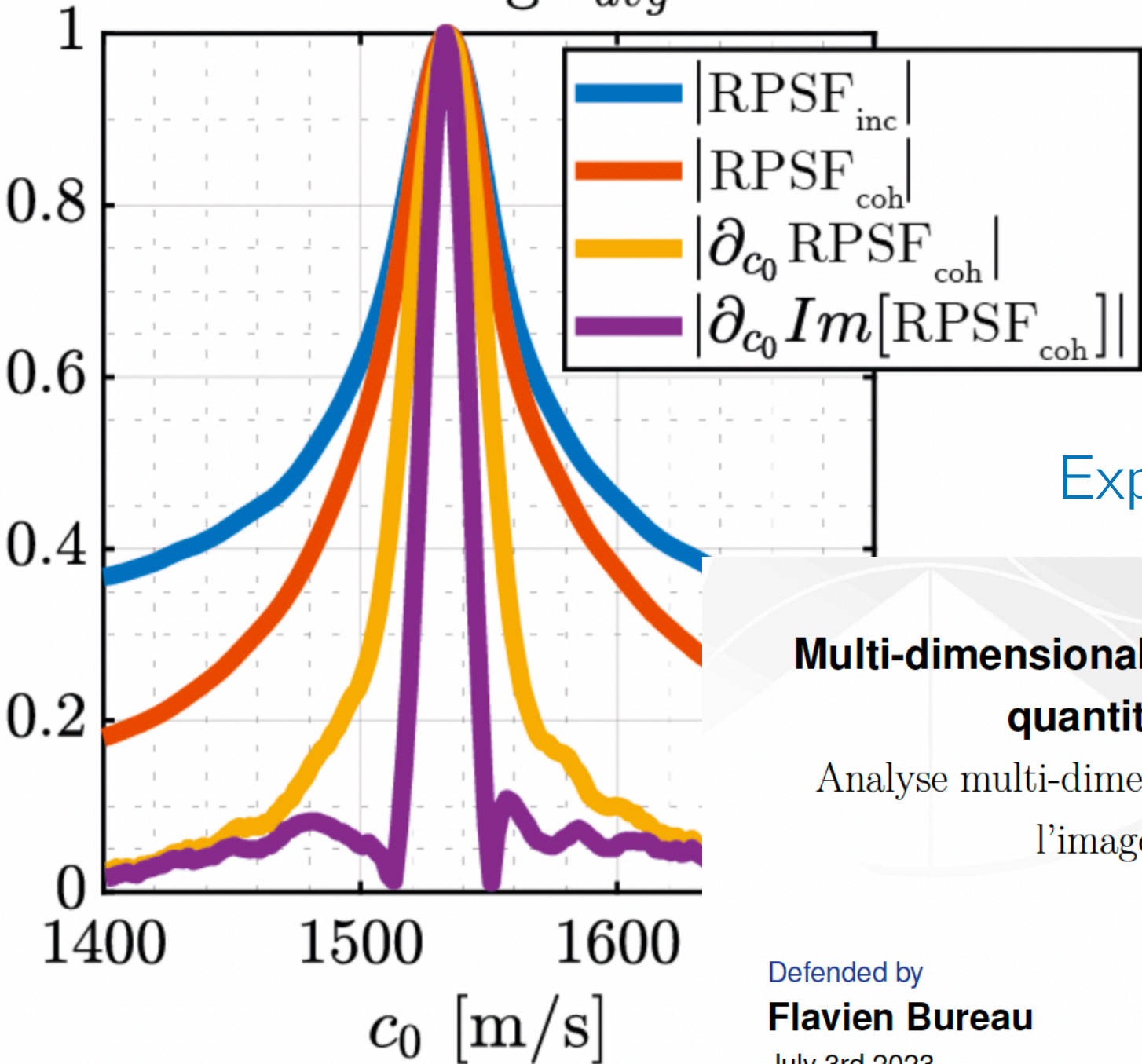
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Experimental curves

Multi-dimensional analysis of the reflection matrix for quantitative ultrasound imaging

Analyse multi-dimensionnelle de la matrice de réflexion pour l'imagerie ultrasonore quantitative

Defended by

Flavien Bureau

July 3rd 2023

Doctoral school n°564

Ecole Physique en Île-de-France

Speciality

Physics

Prepared at the

Institut Langevin (UMR 7587)

Composition of the jury:

Olivier COUTURE
Research director, CNRS

Chair of the jury
Examiner

Jeremy DAHL
Associate Professor, Stanford University

Reviewer

Jean PROVOST
Associate Professor, Polytechnique Montréal

Reviewer

Juliette PIERRE
Research scientist, CNRS

Examiner

Mathias FINK
Professor, ESPCI Paris

Thesis supervisor

Alexandre AUBRY
Research director, CNRS

Thesis supervisor

Summary

Modelisation

Provided a model for wave propagation (and back scattering) in a random micro-structured medium

Used this model to describe medical ultrasound imaging measurements

Inverse problem

Analysed the point-spread function when there is a mismatch modeled and actual speed of sound in the medium

Characterized the focal spot

Analysed the image quality indicator introduced by Aubry, Bureau, Fink & Al.

Proved that it is possible to access *in situ* the effective speed of sound in a micro-structured medium from backscattering measurements

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Take Home messages

It is possible to re introduce sparsity by focusing in the medium

The amplitude of the PSF is enough to control *a posteriori* the quality of the focusing (at least the geometrical component)

Perspectives

Speed of sound mapping

Extend the method to more complex speed of sound model

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Layered mediums - refraction effects (ongoing work w. C. Prada)

Local variation of speed of sound (on going work w. A. Aubry's team)

Perspectives

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Microstructure analysis

Add some contrast in the divergence (density)

Possible effective anisotropy

Effects of multiple scattering

Extension to propagation in solids (ongoing work w. C. Prada)